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(71) Applicant (for all designated States except US): ELAN PHARMA INTERNATIONAL LIMITED [IE/IE]; Lincoln House, Lincoln Place, Dublin 2 (IE).			
(72) Inventors; and (75) Inventors/Applicants (for US only): LAVI, Gilad [IL/IL]; Harav Bazov David 6, 58497 Holon (IL). YIGAL, Gil [IL/IL]; Shlom Zion 5/7, Gan-Yavne 60800 (IL). TSALS, Izrail [US/US]; 17 Rose Way, Sudbury, MA 01776 (US). GROSS, Yossi [IL/IL]; Moshav Mazor 20502 (IL).			
(74) Agents: HOOVER, Thomas, O. et al.; Hamilton, Brook, Smith & Reynolds, P.C., Two Militia Drive, Lexington, MA 02421 (US).			

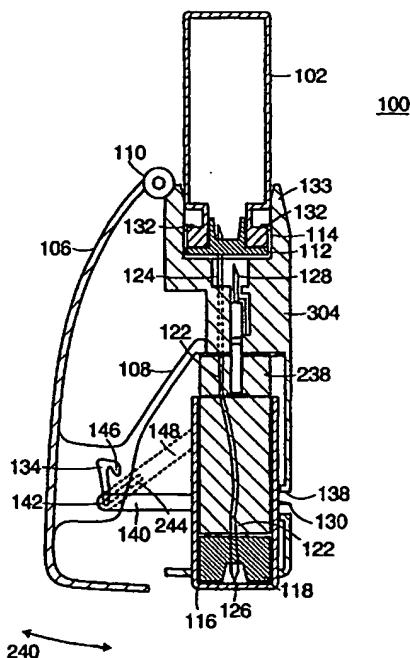
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(57) Abstract

The present invention relates to a drug delivery device for mixing and delivering a drug by injection. The device includes a housing having a first port or opening therein that receives a first container that contains a fluid or powdered drug, for example, a lyophilized drug. The housing can also include a second port or opening that receives a second container that contains a fluid to be mixed with the drug to form an injectable fluid. The device includes a manifold having a channel that fluidly connects the first and second containers. A penetrating membrane such as a needle is used to inject the drug into a patient which is in fluid communication with the first container. The needle is movable from a storage position in the housing to an injection position extending through the housing.



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## DRUG DELIVERY SYSTEMS AND METHODS

## RELATED APPLICATIONS

This application claims priority to U.S. Provisional Application No. 60/108,382 filed November 13, 1998 and U.S. Provisional Application No. 60/131,644 filed April 29, 1999, the entire teachings of both of these applications being incorporated herein by reference.

## BACKGROUND OF THE INVENTION

The present invention relates to the preparation and administration of a product and, more particularly, to the injection of the same into a living organism, for example, a human body.

Previously, various devices have been developed for the percutaneous delivery of medications into living organisms including syringes in which a liquid is delivered from a chamber using pressure asserted by a manual plunger through a needle inserted under the skin.

Additionally, it is well known in the art that the storage life of certain injectable substances such as glucagon, used to dissolve blood clots, is increased when the substance is stored in a powdered or lyophilized state, for example. These lyophilized substances (i.e., drugs or compounds) are presently used for injection of materials that would otherwise be unstable. Lyophilization, for example, is the rapid freezing of a material at a very low temperature followed by rapid dehydration by sublimation in a high vacuum. The resulting lyophilized compound is typically stored in a glass vial or cartridge which is closed by a cap, such as a rubber stopper or septum.

It is necessary to reconstitute the powdered or solid material, such as a lyophilized compound, prior to administration. This is accomplished by mixing the solid compound with a suitable diluent or liquid. Reconstitution typically involves the use of a syringe with a needle to withdraw the diluent from a separate vial and inject it into the vial containing the compound. The compound is then thoroughly mixed, typically by shaking the vial by hand, and a separate syringe with a needle withdraws the desired amount to be injected into the patient. Because two separate containers are used, the person reconstituting the compound must be certain to mix the correct amounts such that a proper concentration of the mixture results. When a syringe is used to mix the diluent and drug, the exact volume of diluent to drug ratio

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is difficult to obtain. Thus, precise concentration levels of administered drug may be compromised.

Moreover, because the diluent and compound are in separate, sterilized containers, the manual withdrawal of diluent via a syringe and reinjection of the  
5 same into the container containing the solid material such as a powdered or lyophilized drug may compromise sterility, and safety due to the use of a syringe.

Because of increased use of powdered compounds or lyophilized drugs, for example, it is desirable to provide both professional and non-professional personnel with a reconstituted drug delivery system. It is desirable to have a simple, reliable  
10 system that facilitates preparation and safe delivery of an accurate dosage of a reconstituted compound. In addition, it is desirable to provide a system that reconstitutes a lyophilized drug while maintaining sterility throughout the process. Also, it is desirable to provide improvements in the percutaneous delivery of medication generally, which provide for safe, effective administration by the user.

## 15 SUMMARY OF THE INVENTION

The present invention relates to systems and methods for delivering liquid drugs to a user. The drug delivery system can include delivery of reconstituted powdered drugs such as, for example, lyophilized drugs, or more generally for the transfer and delivery of liquid drugs. Powdered or lyophilized drug delivery further  
20 includes a system to reconstitute the powdered drug. The drug delivery systems may further include a pressurization system which pressurizes the drug for transfer to a delivery system or for direct subcutaneous delivery. Further, the drug delivery system in accordance with the present invention includes an injector system which contacts the tissue and delivers the drug to the patient or user. In the alternative, the  
25 drug delivery system in accordance with the present invention includes filling of detachable delivery devices, for example, a standard syringe, a needleless injector, an infusion device or different types of pumps. Another example uses a pen injector which aspirates the liquid drug from the system and in turn delivers the drug subcutaneously.

30 The methods for delivering a powdered drug such as a lyophilized drug include the steps of pressurizing a diluent solution in a diluent vial. The

pressurizing systems may include, but are not limited to, a compressed air supply, a chemical gas generator, a collapsible volume supply, a bellow canister, a standard syringe or a cylinder, for example. The methods further include the step of delivering the pressurized diluent solution to the powdered drug vial. The next step  
5 in the method includes the reconstitution of the drug to form a liquid drug by mixing the powdered drug with the diluent solution. The methods further include the steps of providing the liquid drug to an injector system or transferring the liquid drug to detachable delivery devices. The following step includes the injection of the liquid drug into the tissue of the patient or user. The methods further include the steps of  
10 moving the injection needle from a delivery or injection position to a retracted or storage position once delivery is complete. It should be noted that, depending on the application or delivery of different medicaments, the features of the drug delivery systems may vary. For example, the pressurization level can vary depending upon the viscosity level of the medicament, and the needle type or length can vary  
15 depending upon subcutaneous injection or intermuscular injection. For example, for subcutaneous injections, the needle length ranges from 5 to 12 mm while the needle length may vary up to about 3 cm for intermuscular injections.

The methods for delivering a liquid medicament to a patient include the steps of pressurizing the liquid drug solution in the vial with a pressurizing system. The  
20 subsequent steps are similar to the steps described with respect to the methods for delivering a powdered medicament.

A preferred embodiment of the present invention features an injector system having an angled or u-shaped needle. Another preferred embodiment of the present invention features an injector system having a straight needle. Yet another preferred  
25 embodiment of the present invention employs a transfer system for transferring the drug to delivery devices such as, for example, a standard syringe with a needle or a needleless pen injector. The devices receive the liquid drug from a container, such as a vial containing the liquid drug. The delivery devices subsequently deliver the medication to the user's tissue as described herein.

30 Another preferred embodiment of the present invention features a combination system having the ability to reconstitute drug into solution and subsequently inject it into a user. In accordance with this embodiment the

reconstituted drug delivery system has a housing having a first opening or port that receives a first container that contains a solid substance, such as a powdered lyophilized drug, for injection. It should be noted that the container is a rigid container, such as, for example, a vial or a cartridge containing the powdered drug.

- 5 The housing can also include a second opening or port that receives a second container that contains a fluid to be mixed with material in the first container, to form an injectable fluid. The drug delivery system may include a manifold having a first channel that provides fluid communication between the first and second containers. The manifold further includes a second channel between the first  
10 container and a delivery or transfer device. The manifold can also include a communication channel to a pressurization system which provides the driving pressure to deliver the liquid drug. In a preferred embodiment, the penetrating member is a needle, in fluid communication with the first container after the needle moves between a storage position in the housing to an injection position extending  
15 outside the housing and into the user.

A preferred embodiment of the invention provides for concealment of the injection needle within the main housing of the drug delivery device except during the injection of the drug to the user. This embodiment can include a needle retraction device for withdrawing the needle into the housing after injection to  
20 minimize the risk of exposure to a contaminated needle.

In accordance with other aspects of the present invention, the length of the delivery path from the container with the injectable fluid to the injection needle is reduced to minimize loss of residual amount of liquid drug. According to another aspect of the invention, the injection needle first pierces the skin of the person being  
25 injected and is concurrently placed in fluid communication with the first container that contains the injectable fluid. According to yet another aspect of the invention, the container that contains the injectable fluid is substantially visible during reconstitution and injection such that the user can visually observe the process. A compressed fluid, such as a gas in the container with the injectable fluid, is used to  
30 force the injectable liquid through the injection needle and into the tissue being injected. In an alternative embodiment, the device has a single port with a compression element such that a container with a liquid medication, such as a

previously reconstituted material, can be inserted into the housing and simultaneously pressurized to the needed pressure to deliver the correct dose over a predetermined time period.

In a preferred embodiment of the system, the device is used with the injectable fluid container being vertically oriented during injection. To reduce the risk of injecting any gas into the injection site, a gas impermeable membrane such as a hydrophilic membrane is disposed in the fluid path, which in a wetted state minimizes or preferably prevents gas flow while allowing liquid to flow through the membrane. The rigid containers need to be in a vertical orientation during reconstitution for appropriate pressurization. In an embodiment including a cartridge having diluent and air, a vertical orientation is not required for reconstitution. According to a further aspect of the present invention, the axis of the injection needle is perpendicular to the longitudinal axis of the container with the injectable fluid. In a preferred embodiment, the containers containing a powdered or lyophilized drug and diluent are inserted in the housing in the same direction along parallel axes. In another embodiment, the containers are inserted along a common axis or parallel axes in the opposite direction. The system can have housing apertures, ports, or openings that have a size compatible with standard vial and cartridge sizes such that existing vials and/or cartridges can be used. The container contents do not have to be mixed until immediately prior to injection. Because the contents of the containers are only in contact with other sterile parts, sterility prior to and during the reconstitution process is maintained.

According to another aspect of the present invention a further improvement to reduce and preferably prevent the risk of injecting gas into the injection site, includes the use of a drug which is gas impermeable once wetted. Further, since the gas impermeable membrane can sustain pressure, the delivery time for the liquid drugs is shortened as a higher driving force is generated using pressurization systems. By disposing such a membrane such as a hydrophilic membrane in the drug delivery path that is gas impermeable in a wetted state, gas needed to control injection pressure and duration can be added in the system as the membrane checks the delivery of gas to the user. The container containing the fluid can be a changeable volume container which contains a controllable volume of a gas, for

example, air. This controllable volume of air and/or fluid are forced into the drug container, resulting in a drug under pressure to deliver the correct dose over a selected time period. According to a further aspect of the invention, the device includes a manifold system to minimize the drug delivery path and simplify  
5 assembly costs, and increase system reliability. The simplicity and flexibility of the manifold system facilitates the use of standard prefilled cartridges and syringes. In a preferred embodiment, the manifold is a two-piece polycarbonate molding in which the two molded elements are ultrasonically welded together. The gas impermeable membrane is attached or welded to one piece of the polycarbonate molding.

10 According to another aspect of the present invention, a further improvement to deliver an accurate predicted volume of a drug includes adjustable height penetrating members, such as, for example, outlet spikes. In the alternative, delivery of an accurate predicted volume, for example 50% or 80% etc., can be gauged from the residual drug volume or the use of detachable delivery devices, for example, a  
15 standard syringe or a pen-type pump injector.

According to another aspect of the present invention, a further improvement to the drug delivery systems includes interlocks and indicators which ensure the safe and accurate delivery of the drugs. The interlocks include, but are not limited to latches which provide for a desired sequence of operation such as pressurization of  
20 containers to follow the step of insertion of the containers, or prevention of displacement of the needle to an injection position after a first injection use. The indicators include a vertical orientation indicator and end of delivery indicators.

According to another aspect of the present invention, the housing of the drug  
25 delivery device is shaped and designed to function appropriately to enable single handed operation. For example, the bottom surface of the housing is flat in shape to allow table top placement to accommodate single handed operation by the user. Further, the device is sized to enable the insertion of vials and subsequent activation of the device using one hand.

30 In a preferred embodiment, the system housing is lightweight and compact, having a weight of less than 30 grams and a volume of less than 100cm<sup>3</sup>. This provides a portable disposable device that can be discarded or recycled after a single



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use and that is readily transported by the user. In addition, the present invention is self-contained and maintains sterility throughout the reconstitution and injection of a fluid such as a lyophilized drug. It should be noted, the weight and volume of the system housing can vary depending upon the different embodiments and the volume of drug being delivered to a user.

#### BRIEF DESCRIPTION OF THE DRAWINGS

Figures 1A-1F illustrate the operation of a preferred embodiment of a drug delivery device in accordance with the present invention.

Figures 2A and 2B illustrate cutaway views of the drug delivery device shown in Figures 1A-1F, along line 2A, 2B - 2A, 2B in Figure 1F.

Figures 3A-3D illustrate the sectional views of the internal components of the drug delivery device of Figures 1A-1E and Figure 2 during administration of the reconstituted drug.

Figures 4A-4O illustrate the operation of a preferred embodiment of a drug delivery device in accordance with the present invention.

Figures 5A-5C are perspective views of a preferred embodiment of a drug delivery device in accordance with the present invention.

Figures 6A-6C illustrate the operation of a drug delivery device substantially similar to the device shown in Figures 5A-5C.

Figures 7A-7C are partial perspective views of the drug delivery device of Figures 5A-5C and 6A-6C illustrating the injection of the drug.

Figures 8A-8F illustrate the operation of a drug delivery device substantially similar to the device shown in Figures 5A-5C.

Figures 9A-9F illustrate the operation of a preferred embodiment of a drug delivery device in accordance with the present invention.

Figures 10A and 10B are graphical illustrations of the pressure, weight, and delivery characteristics of a preferred embodiment of the invention.

Figures 11A-11D illustrate cutaway views of an alternative embodiment including a drug container subassembly of the drug delivery device in accordance with the present invention.

Figures 12A-12B illustrate perspective views of a preferred embodiment of the diluent container subassembly shown in Figures 11A-11D.

Figures 13A and 13B illustrate cutaway views of an alternate embodiment of the drug delivery device in accordance with the present invention.

5        Figure 14 illustrates a cutaway view of another preferred embodiment of the drug delivery device in accordance with the present invention.

Figures 15A and 15B illustrate cutaway views of an alternate embodiment of the drug delivery device in accordance with the present invention.

10       Figure 16 illustrates a cutaway view of an injection device in accordance with the present invention.

Figures 17A-17C illustrate cutaway views of an alternate embodiment of the drug delivery device in accordance with the present invention.

Figures 18A-18C illustrate cutaway views of an alternate embodiment of the injector system of the drug delivery system in accordance with the present invention.

15       Figures 19A-19F illustrate alternate embodiments of pressurization systems included in the drug transfer system in accordance with the present transfer invention.

Figures 20A-20C illustrate views of an alternate embodiment of the drug delivery system in accordance with the present invention which uses standard vials  
20       containing a liquid medicament.

Figure 21 illustrates a view of another preferred embodiment of the drug delivery system in accordance with the present invention which uses standard vials containing a liquid medicament.

Figures 22A-22E illustrate cutaway and perspective views of an alternate  
25       embodiment of the drug delivery system in accordance with the present invention.

Figures 23A and 23B illustrate alternate preferred embodiments to control the dose of drugs in accordance with the present invention.

Figures 24A-24C illustrate cutaway views of an alternate embodiment of the drug delivery system in accordance with the present invention incorporating filling  
30       devices, for example a syringe, to inject the drug system.

Figure 25 illustrates a cutaway view of an alternate embodiment of the drug transfer system in accordance with the present invention incorporating filling devices, for example a pen type pump to inject the liquid medicament.

Figures 26A-26D illustrate perspective views of a preferred embodiment of a  
5 drug transfer system in accordance with the present invention.

Figures 27A-27C illustrate cutaway views of a preferred embodiment of a drug delivery system in accordance with the present invention.

Figures 28A-28C illustrate cutaway views of the operation of a preferred embodiment of a drug delivery system in accordance with the present invention.

10 Figure 28D illustrates an enlarged cutaway view of a preferred embodiment of the spike which brings the liquid drug in communication with the delivery system in Figures 28A-28C.

Figures 29A and 29B illustrate partial cutaway views of a preferred embodiment of the drug transfer delivery system in accordance with the present  
15 invention.

Figures 30A and 30B are views showing the two piece construction of the manifold in accordance with the drug delivery system of the present invention.

Figures 31A-31G are perspective views of a preferred embodiment of a drug delivery system in accordance with the present invention.

20 Figures 32A - 32E are perspective views of another preferred embodiment of a drug delivery system in accordance with the present invention.

Figures 33A - 33I are cutaway views illustrating the interlocks built into the drug delivery system in accordance with the present invention.

Figures 34A - 34D are views of a preferred embodiment illustrating an end  
25 of delivery indicator of the drug delivery system in accordance with the present invention.

Figure 35 is a graphical illustration of a delivery profile of a preferred embodiment of the drug delivery system with no additional volume of air in the liquid vial in accordance with the present invention.

30 Figure 36 is a graphical illustration of the delivery duration and delivery pressure of a preferred embodiment of the drug delivery system in accordance with the present invention.

Figure 37 is a graphical illustration of delivery parameters of injecting a drug with no additional volume of air in accordance with the present invention.

Figure 38 is a graphical illustration of the air pressure gradient on a hydrophilic membrane in the drug delivery system in accordance with the present invention.

Figure 39 is a graphical illustration of the delivery profile with respect to time for a vial system containing about 7.5 ml of air in accordance with the present invention.

Figure 40 is a flowchart describing the method of delivery of a reconstituted drug in accordance with the present invention.

Figure 41 is a flowchart describing the method of delivery of a liquid drug in accordance with the present invention.

The foregoing and other objects, features, and advantages of the drug delivery systems and methods will be apparent from the following more particular description of preferred embodiments of the invention, as illustrated in the accompanying drawings in which like reference characters refer to the same parts throughout the different views. The drawings are not necessarily to scale, emphasis instead being placed upon illustrating the principles of the invention.

#### DETAILED DESCRIPTION OF THE INVENTION

The present invention is directed to drug delivery systems and methods. The drug delivery system provides generally for the delivery of a drug in solution under pressure, and more particularly to the injection of powdered or lyophilized drugs that require reconstitution. The drug delivery system includes a reconstitution system, a pressurization system to facilitate drug delivery, a transfer system and an injector system. Different embodiments of the present invention may use only one of the systems described and other embodiments can employ combination of these systems, depending on the requirements of different applications. For example, a preferred embodiment can deliver a liquid drug and not require reconstitution. Therefore the drug delivery systems and methods are a combination of some or all of the systems or processes described below.

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With reference to Figures 1A-1E, the general operation of a preferred embodiment of a drug delivery device 100 is illustrated. Figures 2A-2B, and 3A-3D provide sectional views of the same embodiment for clarity. As specifically illustrated in Figure 1A, drug delivery device 100 comprises a first member or housing 304 and a pivotally connected second member or handle 106. The device 100 is used to mix, within a sterilized environment, a first liquid such as a diluent 166 (for example, a fluid such as sterilized water) with a second powdered drug such as a lyophilized drug or compound concentrate 164, e.g., interferon, and to inject the resulting reconstituted lyophilized drug into a living organism, which in the preferred embodiment is a human being. Advantageously, the device 100 utilizes a standard vial or first storage container 102, which contains the lyophilized drug or compound 164, and a standard cartridge or second storage container 116, which contains the diluent 166. The device 100 may be formed from inexpensive materials, such as plastic or the like, such that it is economically feasible to dispose of the device after a single injection.

In preparation for the administration of the drug, the user removes protective packaging which envelops the device 100. This packaging maintains sterility of the device 100 prior to use. In the preferred embodiment of the invention, cartridge 116 containing diluent 166 comes preassembled, being locked into the bottom of housing 304 by the arms 133 as shown in Figures 2A and 2B.

The sterility protector of the vial 102 is removed and then locked into the top of housing 304 as shown in Figure 2A with a needle 124 from the housing penetrating a stopper 112 of the vial. At this stage, vial 102 is filled with air at ambient pressure. The cartridge 116 is pushed upward, i.e., toward vial 102. The cartridge 116 is punctured and the diluent 166 is delivered to the vial 102 as shown in part in Figure 1C. At this stage, as will be explained below, there is a fluid such as gas in vial 102 which is compressed by transfer of diluent 166 into vial 102. The user swills the device 100 to ensure the lyophilized drug is appropriately reconstituted. The reconstituted lyophilized drug, or injectable fluid, is identified as reference number 160.

Now, drug in solution with the diluent is ready for injection. The device 100 is pressed against the skin of the person to be injected with the vial 102 in a vertical

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orientation to ensure that the compressed gas, for example, air is used to inject the reconstituted drug and that the gas or air is not injected into the injection site. The user presses the handle 106 which causes the injection needle 130 to move between a first position, or storage position, within the housing 304 as shown in Figure 3A, and a second position, or injection position, outside the housing as shown in Figure 3C. It is preferred that the needle extend out of the housing 304 in the range of 5 to 12 millimeters. The second extended position of the injection needle 130 is also illustrated in Figure 1D. At this point, the injection needle 130 is fluidly connected to vial 102 such that the reconstituted lyophilized drug 160, under pressure from the compressed gas in vial 102, is delivered to the injection site. The delivery of the reconstituted lyophilized drug 160 can be completed in a time period in the range of 10 -30 seconds.

Upon release of handle 106, a biasing mechanism 108 (to be detailed below) returns the handle to the original position. Simultaneously, a needle retraction mechanism (also to be described below) locks the injection needle 130 within the housing 304, thereby reducing and preferably preventing exposure of the contaminated needle. The final stage of operation is illustrated in Figure 1E, wherein the device 100 may be safely discarded.

Figure 1F is a view taken along line 1F-1F of Figure 1E and illustrates the relative positions of vial 102 and cartridge 116 in housing 304. As shown, the longitudinal axes of vial 102 and cartridge 116 are parallel but offset relative to the positioning within the housing 304. This allows for both vial 102 and cartridge 116 to be inserted into the housing 304 without interfering with the internal components of the device 100, for example, the needle retraction mechanism described below.

Figures 2A and 2B illustrate cutaway views along lines 2A, 2B - 2A, 2B of Figure 1F of the device 100 including vial 102 and cartridge 116. More particularly, vial 102 is preferably a standard vial, for example, a 2 milliliter vial, which typically comprises glass and includes a puncturable rubber stopper 112 held in place by an aluminum band or other sealing mechanism 114. The upper end of housing 304 includes a grooved portion 132 which locks the vial 102 to the housing by passing the lip of the aluminum band 114 under a pair of spaced apart arms that hook up into the housing. A first needle 124, or other suitable means, is mounted to the housing

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304 and is configured to pierce the rubber stopper 112 of vial 102 upon insertion of the vial into the locking position provided by arms 133. First needle 124 is fluidly connected to a first channel or tube 122 for receiving the diluent from cartridge 116 as illustrated in Figure 2B. Cartridge 116, similar to vial 102, preferably comprises

5 a standard cartridge (for example, a 2 milliliter cartridge with about 1 milliliter diluent) and includes a rubber stopper 118 which is pierced by a second needle 126, or other suitable means. Second needle 126 is fixedly mounted on an extending member or compression element 238 of housing 304 such that the cartridge is pierced upon insertion of the cartridge. First tube 122 is fluidly connected to the

10 second needle 126. Upon insertion of the cartridge 116, extending member 238 or compression element of housing 304 contacts and pushes rubber stopper 118 toward the bottom of cartridge 116. In this manner, the diluent 166 is forced up tube 122 into vial 102 to mix with the drug 164 contained therein. In the preferred embodiment of the present invention, cartridge 116 contains approximately 1

15 milliliter of diluent which is forced into vial 102, resulting in a pressure inside vial 102 of approximately 2.25 bars. This pressure can be adjusted, for example, by decreasing the amount of diluent or air in cartridge 116. A higher pressure inside vial 102 injects the reconstituted drug 160 more quickly.

Thus, a sterilized solution is provided wherein the diluent 166 is mixed with

20 the lyophilized drug 164 with minimal exposure to outside contaminants. It is preferable that vial 102 containing the reconstituted lyophilized drug 160 be visible during reconstitution and injection such that the user can properly visually verify that the lyophilized drug 160 is thoroughly mixed with diluent 166 and that the vial 102 is vertical during injection to ensure the compressed gas is not being injected

25 into the injection site.

Handle member 106 is pivotally connected to the housing 304 at a first end by a pivoting mechanism 110 which can include a rivet or other suitable means such that the handle member rotates in the direction of arrow 240. Handle member 106 includes biasing mechanism 108 which resiliently biases handle member such that

30 the end opposite the pivotally connected end is forced away from housing 304. Biasing mechanism 108 includes an extending member from handle member 106 which contacts housing 304, thereby providing a resilient biasing force away from

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the housing when the handle member is forced toward the housing. Alternatively, or additionally the biasing mechanism 108 can comprise a conventional spring, or other suitable means, interposed between housing 304 and handle member 106 which provides the biasing force.

5        Also shown in Figure 2A is a needle injection and retraction mechanism for injecting the reconstituted drug 160 into the person and retracting the injection needle 130 within the housing 304. The mechanism includes a first bar member 140, which is pivotally connected at a first end by member 136, and guidably mounted at a second end to the handle member 106 by a first coupling device 142, 10 such as a pin, rivet, bolt, or other suitable means. Member 136 fixedly supports injection needle 130 and is guided by an opening 138, or needle aperture, in the housing 304. In the preferred embodiment of the invention, injection needle 130 is in the range of a 24-28 gauge needle. The movement of first coupling device 142 is controlled by a J-shaped slot 134 which can comprise a slot or groove in handle 15 member 106. A second bar member 148 is pivotally connected at a first end to first coupling device 142 and pivotally connected at a second end to a third bar member 152 by a third coupling device 150. Third bar member 152 fixedly supports a third needle 128 and may be guided by internal bore in housing 304. A second channel or tube 120 fluidly connects the third needle 128 and injection needle 130. It is 20 preferable to minimize the length of tube 120 such that the residual volume of drug remaining in the tube after injection is reduced to increase the accuracy of the dosage.

The operation of drug delivery device 100 shown in Figures 2A and 2B is illustrated in Figures 3A-3D. Figure 3A illustrates the stage at which the cartridge 25 116 is inserted forcing diluent 166 up tube 122 into vial 102. It will be recalled that the rubber stopper of 118 of cartridge 116 is forced to the bottom of the cartridge by member 238 as shown in Figures 2A and 2B. This causes the diluent 166 to be forced up tube 122 which results in the reconstituted drug 160 being under pressure, which in the preferred embodiment is approximately 2.25 bars. The device 100 is 30 preferably vigorously shaken to ensure the lyophilized drug is properly mixed with diluent 166.



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In Figure 3B, the device 100 is placed against the skin of the person being injected. The user presses handle member 106 toward the housing 304 in a direction shown by arrow 240A, thereby displacing injection needle 130 from the first position within the housing to a second position outside the housing such that the  
5 needle penetrates the skin of the body being injected.

As shown in Figure 3C, continued pressure of the handle 106 towards the housing 304 causes the first bar member 140 to ride up the J-shaped slot 134. Simultaneously, second bar member 148, which includes a linear slot 244, is rotated such that first coupling device 142 rides up to the top of slot 244.

10 Figure 3D illustrates the continued pressing motion of the handle member 106 toward the housing 304. As the handle member 106 continues to pivot, the second bar member 148 forces third bar member 152 and hence third needle 128 upward such that third needle penetrates the rubber stopper 112 of vial 102. Because the reconstituted lyophilized drug 160 is under pressure, it is forced through  
15 tube 120 and thus into the person being injected. At this point, biasing mechanism 108 is compressed. As the handle member 106 is released, biasing mechanism 108 forces the handle member away from the housing 304 as indicated by arrow 240B and thus withdraws injection needle within the housing. This is illustrated in Figure 3D. J-shaped slot 134 is beneficially provided with an end locking portion 146  
20 which catches coupling device 142 such that the injection needle 130 is "locked" within the housing 304 after a single injection. Now, the device 100 can be safely discarded.

Figures 4A-4K illustrate a drug delivery device 100-1 in accordance with a preferred embodiment of the present invention wherein the same reference numbers  
25 refer to the same or similar elements. More particularly, Figure 4A illustrates the device 100-1 which includes a housing 304-1 having a first port or opening 176 for receiving a diluent cartridge 116 and a second port or opening 262 for receiving vial 102. In this embodiment, it is preferred that cartridge 116 containing diluent 166 be preassembled such that the cartridge is partially penetrated by needle 126-1 and such  
30 that the device 100-1 (without vial 102) is wrapped by a packaging material to maintain sterility prior to use. Again, it is preferable to use a standard 2 milliliter vial and cartridge that contains 1 milliliter of diluent. Thus, the user unwraps the

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packaging material and places vial 102 containing the lyophilized drug 164 into the opening 262. Alternatively, vial 102 and cartridge 116 are packaged separately from the device 100-1 as shown in Figure 4A. The user removes the sterility protector and presses the vial 102 firmly into the opening until needle 124-1 penetrates the rubber stopper 112. The user then forces cartridge 116 into the housing 304-1. As cartridge 116 is forced into the housing 304-1, the rubber stopper 118 is first penetrated by needle 126-1 such that the needle extends into the diluent 166. This stage is illustrated in Figure 4B.

Continuing to insert the cartridge 116 into the housing 304-1 forces the rubber stopper 118 to the bottom of the cartridge, as shown in Figure 4C. That is to say, the first opening 176 of housing 304-1 is preferably circular, thereby allowing the walls of cartridge 116 to enter the housing and not the rubber stopper 118. This forces the diluent 166 through needle 126-1 to a manifold or communication passageway 168 and into the vial 102. Again, the resulting reconstituted lyophilized drug 160 in vial 102 is preferably under pressure of about 2.25 bars. A greater or lower pressure may be necessary depending on the volume to be injected. The device 100-1 is preferably vigorously shaken to ensure the reconstituted lyophilized drug 160 is properly mixed in preparation for injection.

It is preferable to insert vial 102 containing the lyophilized drug 102 before insertion of cartridge 116 containing diluent 166 such that the diluent is not spilled into opening 262. In order to ensure the proper insertion sequence of vial 102 and cartridge 116, an interlocking mechanism is provided in accordance with another aspect of the present invention. Interlocking mechanism comprises a bar member 266 pivotally connected to the housing 304-1 between the openings 176 and 262. The bar member is configured to be moved in the direction of arrow 264 (Figure 4A) upon insertion of vial 102. Thus, as shown in Figure 4A, bar member 266 prevents cartridge 116 from being inserted. As vial 102 is inserted, it rotates bar member 266 in the direction of arrow 264 as shown in Figure 4A such that cartridge 116 can subsequently be inserted.

As shown in Figure 4B, the device 100-1 is further provided with an actuator or pushing member 174 for displacing the injection needle 130-1 between a first position within the housing 304-1 and a second position outside the housing. It is

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preferred that the injection needle 130-1 extend out of the housing 304-1 in the range of 5-12 millimeters. The injection needle 130-1 is in the range of a 24-28 gauge needle and is preferably a "U" type needle having a second end 172 configured to puncture sealing member 170. Sealing member 170, which can be any puncturable material such as butyl rubber, sealingly maintains the liquid in the upper part of housing 304-1 prior to use.

It is preferable to prevent displacement of the injection needle 130 when the device 100-1 is not properly oriented, for example, upside down, in order to prevent the compressed gas in vial 102 from being injected. Also, it is preferable to lock the injection needle 130-1 within the housing 304-1 after a single injection to reduce exposure to the contaminated needle. Additionally, it is preferable to only allow displacement of needle 130-1 after insertion of cartridge 116. Accordingly, a locking assembly 268A is provided to accomplish the foregoing.

The locking assembly 268A comprises member 268 as shown in Figure 4C having a first end configured to be moved by pushing member 174 and a second end configured to displace a ball 270 or other appropriate movable locking device. With the pushing member 174 in the first position such that injection needle 130 is within the housing, groove 272 of the pushing member 174 aligns with groove 274 such that ball 270 can freely travel around the groove 274 of the pushing member. When vial 102 is vertically oriented with the compressed gas above the liquid, thus being properly positioned for injection as shown in Figures 4B and 4C, ball 270 rests in the bottom of groove 274 allowing the pushing member 174 to displace the injection needle 130. If the vial 102 is not properly positioned (for example, the assembly being upside down such that compressed gas would be injected, as shown in Figures 4E and 4F), the ball 270 is positioned within grooves 272 and 274 to prevent displacement of the pushing member 174.

The locking assembly 268A can be further configured to allow displacement of the pushing member 174 only after cartridge 116 is inserted. Figures 4G-4L illustrate this aspect of the invention. More particularly, Figure 4G is similar to Figure 4C except cartridge 116 is shown outside of the housing 304-1. Figure 4H is a sectional view taken along line 4H-4H of Figure 4G and shows member 276 of the locking mechanism having a slotted portion 278 therein. Member 276 is slidable

within the housing 304-1 and configured to be moved by insertion of cartridge 116. The lower end of member 276 is positioned within grooves 272 and 274 as shown in Figure 4I. Thus, with member 276 in the position shown in Figure 4H, or before cartridge 116 is inserted into the housing 304-1, the pushing member 174, and hence  
5 injection needle 130-1, is prevented from moving to the injection position.

When the cartridge 116 is fully inserted into housing 304-1 as shown in Figure 4J, member 276 is moved downward as shown in Figure 4K. As shown in Figure 4L, this allows slotted portion 278 to align such that pushing member 174 and hence injection needle 130-1 can be moved to the injection position.

10 With the device 100-1 properly held by the user such that vial 102 is vertically oriented as shown in Figure 4M, the user presses pushing member 174 such that the injection needle 130-1 first extends out of the housing 304-1, thus penetrating the skin of the person being injected. Continued pressing of pushing member 174 causes the second end 172 of injection needle 130-1 to puncture sealing  
15 member 170, thereby allowing the pressurized reconstituted lyophilized drug 166 to travel from vial 102 into the person being injected. It may take in the range of 10-30 seconds to deliver the injection fluid. This pressing motion compresses spring 190 such that upon release of pushing member 174, the member returns to the original position, i.e., the needle 130-1 is withdrawn within the housing 304-1 and locked  
20 therein. Insertion of the pushing member 174 into the housing 304-1 also moves in member 268 such that ball 270 is biased against the pushing member. This is shown in Figure 4N. When the pushing member 174 is returned to the first position, the ball 270 is positioned and held within groove 272 by member 268, thereby preventing displacement of the pushing member and hence the injection needle 130-  
25 1 after a single injection. This configuration is illustrated in Figure 4O. With the injection needle 130-1 locked within the housing 304-1, the device 100-1 may be safely discarded.

Figures 5A-5C illustrate a drug delivery device 100-2 in accordance with a preferred embodiment of the present invention. More particularly, Figure 5A  
30 illustrates the device 100-2 with the cartridge 116 installed but not inserted or penetrated by any needle, and the vial 102 in place ready to be inserted. Figure 5B illustrates the inserted vial 102, while Figure 5C shows the subsequently inserted

cartridge 116. At this stage, the diluent from cartridge 116 has been transferred to vial 102, resulting in a pressurized liquid in the vial. The device 100-2 is vigorously shaken to ensure proper mixing of the reconstituted lyophilized drug. The device 100-2 is now ready for injection. It should be noted that the housing 304-2 advantageously includes a cutaway portion 254 which allows the user to visually inspect vial 102 to verify that the lyophilized drug 160 is thoroughly mixed with diluent 166 and to verify that vial 102 is vertically oriented during injection to ensure air is not being injected into the injection site.

Figures 6A-6C are plan views of a similar device 100-3 corresponding to Figures 5A-5C, respectively. Accordingly, Figure 6A illustrates the cartridge 116 installed but not punctured by needle 126-3. Vial 102, containing the lyophilized drug 164, is also shown ready to be inserted into housing 304-3.

Figure 6B shows the inserted vial 102 which is punctured by needle 124-3. Vial 102 pushes first against surface 178-3 of puncturing device 182-3 and pushes device 182-3 downward before being pierced by needle 124. Pushing puncturing device 182 downward sets a spring which (as will be explained in Figures 7A-7C) moves puncturing device upward such that needle 128-3 penetrates vial 102. Alternatively, the spring can be preloaded. As shown, needles 124-3 and 126-3 are fluidly connected by a manifold 127 comprising a channel 129 or tube. Upon insertion of cartridge 116, the rubber stopper is first pierced by needle 126, and as cartridge 116 is further inserted into the circular opening 176-3 of housing 304-3, the rubber stopper 118 is forced to the bottom of cartridge 118, thereby forcing the diluent 166 through the manifold 127 into vial 102. This also compresses the gas that was heretofore contained in the vial 102 to a pressure sufficient for injection. The resulting stage is shown in Figure 6C. The device 100-3 is preferably vigorously shaken to ensure proper mixing of the lyophilized drug 164. Now, the device 100-3 is ready to inject the reconstituted drug solution 160 contained in the vial 102.

Figures 7A-7C illustrate partial perspective views of the device 100-2, 100-3 shown in Figures 5A-5C and 6A-6C. More particularly, Figure 7A shows the pushing member 174-3 including an internal bore with member 252 slidably contained therein. Member 252 fixedly supports injection needle 130 which is in

fluid communication with needle 128 via tube or channel 120. Needle 128 shown in Figure 7A has yet to pierce the rubber stopper 112 of vial 102. Needle 128 is fixedly supported by puncturing device 182. As the pushing member 174-3 is pressed toward the housing 304-3 (i.e., in the direction of arrow 180), a first spring 190 is compressed allowing the member 252 to move downward until contacting the housing. This allows injection needle 130-3 to extend out of needle aperture 256 in housing 304-3 to penetrate the skin of the person being injected. The spring 190 is set such that it creates both axial and rotational movement. Only upon complete insertion of the vial 102 is the rotational movement of the spring enabled which in turn enables the puncturing of the vial 102. In the preferred embodiment, injection needle 130-3 extends in the range of 5-12 millimeters out of the housing through needle aperture 256. The injection needle 130 partially extending out of the housing 304-3 is illustrated in Figure 7B.

As the pushing member 174 is further pressed toward housing 304-3, spring 200, which is stiffer than spring 190, is compressed allowing ridge 258 of pushing member 174-3 to contact puncture device 182. This causes rotation of puncturing device 182 in the direction of arrow 186 as shown in Figure 7C, such that surface 178 no longer contacts the vial 102. The spring 190 which, as described above, was loaded upon insertion of vial 102, now causes the puncturing device 182 to rotate in the direction of arrow 184, thereby causing needle 128 to penetrate the rubber stopper 112 of vial 102. This arrangement is illustrated in Figure 7C. The reconstituted drug 160 is forced by the compressed gas within vial 102 through injection needle 130 into the person being injected in a time range of approximately 10-30 seconds.

Figures 8A-8E illustrate a drug delivery system 100-4 in accordance with a preferred embodiment of the present invention wherein the same reference numbers refer to the same or similar elements. More particularly, Figure 8A illustrates the device 100-4 which includes housing 304-4 having a first port or opening 176-4 for receiving cartridge 116 and a second port or opening 262-4 for receiving vial 102.

Vial 102 containing the reconstituted drug 164 is inserted into the housing 304, followed by the insertion of cartridge 116 containing the diluent 166. Again, a rubber stopper of the cartridge 116 is forced to the bottom of the cartridge which

forces the diluent under pressure into vial 102. This stage is shown in Figure 8B. Advantageously, the housing 304-4 includes a cutaway portion 400 such that vial 102 is substantially visible during reconstitution and injection. This allows the user to visually verify that the drug is properly reconstituted and that the vial 102 is  
5 vertically oriented during injection with the compressed gas above the reconstituted drug.

Figure 8C is a rear view taken of Figure 8B and illustrates the injection of the reconstituted drug. More particularly, the pushing member or actuator 174-4 is pressed into housing 304-4 which forces injection needle 130-4 out of the housing  
10 and into the person being injected. In the preferred embodiment, the injection needle extends out of the housing in the range of 5-12 millimeters. The reconstituted drug, in fluid communication with the vial 102, is transferred from the vial and into the person being injected. Figures 8D-8F are isometric views of the device 100-4 in the stages shown in Figures 8A-8C, respectively.

Figures 10A and 10B graphically illustrate system characteristics of a preferred embodiment of the drug delivery device. To provide effective delivery of a specified amount of fluid and minimize patient discomfort, the system requires a sufficient fluid pressure in the delivery vial that is manually actuated by the user within a short time period. Figure 10A shows the pressure (millibars) and weight  
20 (grams) characteristics of the system during a delivery period of about 30 seconds for a delivery volume of about 1.6 milliliters. Figure 10B illustrates test results of the delivery of 1.6 milliliters into different animals using a single drug delivery device for the same time period.

Referring to Figures 11A-11D, cutaway views of a preferred embodiment of  
25 a diluent container subassembly and a manifold, which may be used with the drug delivery devices or with an ordinary syringe or other drug delivery devices, are illustrated. The diluent container subassembly 300 includes a preassembled compression portion 310 which allows the user to hold the diluent container 312, which can be in the form of a compressible sealed bag, and insert it into a needle  
30 314. The diluent container 312 contains about 1 milliliter diluent and a controlled volume of gas, such as air, for example, and upon insertion into housing 304-6, is pierced by the needle 314. During storage or shelf life, the diluent container 312 is

sized to allow for expansion of the container as a result of changes to the environment. In addition, the compression portion 310 is used to compress the exterior of the diluent container and apply pressure to the contents of container during delivery of the diluent for mixing. The diluent containers are formed from  
5 flexible, collapsible materials, for example, polyethylene, polypropylene and nylon. The compression portion 310 includes a slider element 316 and two longitudinally extending arms 318, 320 extending therefrom. Two cylindrical drums 322, 324 are spaced between the longitudinally extending arms 318, 320.

Figure 11A illustrates the diluent container subassembly 300 positioned in  
10 the housing 304-6 of the drug delivery system in accordance with the present invention. Figure 11D further illustrates the fully compressed state of a preferred embodiment of the diluent container subassembly 300. The slider element 316 of the compression portion 310 translates in at least one axis, for example, in the illustrated embodiment, it can move up or down. The downward movement of the  
15 slider element 316 causes the diluent container 312 to wrap around the cylindrical drum 324 which compresses the contents of the diluent container 312, thus forcing the diluent from the container 312 and through the needle 314 and into the vial 102. The movement of the slider element 316 is limited by an end of travel position. At this end of travel position, the slider element 316 may be locked by a locking  
20 mechanism which ensures that the diluent container is kept compressed.

A manifold 330 includes two needles 314, 332 fixedly mounted at the ends of an extending member 334. The needles can also comprise a penetrating member that is formed from an injection molded material such as medical grade polycarbonate or acrylic with the required level of rigidity to penetrate the vial or  
25 container. A channel 331 provides for fluid communication between the needles 314 and 332. Needle 314 pierces the diluent container 312 upon insertion of the container, while needle 332 pierces the vial 102 upon insertion of the vial containing the lyophilized drug 164. In a preferred embodiment of the present invention, container 312 contains approximately 1 milliliter of diluent and a controlled volume  
30 of air which is forced into vial 102, resulting in a pressure inside vial 102 of approximately 2.25 bars. The pressure inside vial 102 results from forcing the controlled volume of air in the diluent container 312 into the rigid volume in the vial



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102. Thus, the diluent 166 is forced into vial 102 to mix with the lyophilized drug 164 contained therein. The entire assembly is preferably shaken to ensure the reconstituted drug 160 is properly mixed in preparation for injection. The vial 102 is vertically oriented during injection to ensure air is not being injected into the  
5 injection site.

Referring to Figure 11C, the injector needle 130-6 is shown in a first position within the housing 304-6. As described hereinbefore, the injection needle 130-6 is in the range of a 24-28 gauge needle and is preferably a "U" shaped needle having a second end 172-6 configured to puncture sealing member 170-6. An area 171 is  
10 located adjacent to the sealing member 170-6 and is in communication with the channel 331 as shown in 11B.

When the user compresses the button 305, it causes the needle 130-6 to penetrate the skin and the second end 172 to penetrate the sealing member 170. The drug and diluent solution will flow from the needle 332, through the channel 331,  
15 and area 171 and to the user via the injector needle 130-6. As the user compresses the button 305, which is spring loaded by spring 306, a pair of mating pawls 307, 308 fit together and prevent the button from being pulled out and the reuse of the device as shown in Figure 11C.

Figures 12A-12B illustrate perspective views of a preferred embodiment of  
20 the diluent container subassembly 300 and provide further details of the components of the compression portion 310. The cylindrical drum 324 is slotted such that the diluent container can be inserted therein. The cylindrical drum 322 serves as a backing drum. Thus, the diluent container 312 is typically inserted between the cylindrical drum 324 and the backing drum 322. The drum apparatus 322, 324  
25 moves in a rack and pinion gear apparatus 340. An end of travel position 342 in the rack and pinion gear apparatus 340 constrains the movement of the cylindrical drum 324 at its end of movement position. This end of travel position correlates with the end of the wrapping of the diluent container 312 around the cylindrical drum and maximum compression of the contents of the container. A flange 344 can be used to  
30 hold the diluent container 312 at the bottom of the subassembly 300. The diluent container 312 can be sealed by means of heat welding techniques or ultra sonic techniques to the flange 344 after it has been filled with the diluent. The

longitudinally extending arms 318, 320 in the compression portion 310 each comprise two members 350, 352, as shown in Figure 12B. A cylindrical drum is attached to each member. The two members 350, 352 are spaced apart from each other to accommodate the wrapping of the diluent container on the cylindrical drum

5 324.

Referring to Figures 13A-13B, cutaway views illustrate an alternate embodiment of the invention similar to that shown in Figures 11A - 11D including a manifold 350. The manifold 350 has two needles 352, 354 for the purpose of piercing the vial 102 and diluent container 312 respectively. Once the diluent 166 and the controlled volume of air are forced to move into vial 102, the diluent mixes with the lyophilized drug 164 and results in the reconstituted drug 160 which is under pressure. Because the reconstituted drug is under pressure due to the controlled volume of air, it is forced through the needle 352 and into the person being injected through a needle 351 that is actuated by movement of pushing

10 15 member 353. This embodiment of the device provides a user comfort as it does not have to be vigorously shaken to ensure the reconstituted lyophilized drug 160 is properly mixed in preparation for injection. The controlled volume of air facilitates the mixing of the diluent and the lyophilized drug. The pushing member 353 displaces the injection needle 351 between a first position within the housing 304 and a second position outside the housing, or in an injection state.

20

It is preferable to prevent displacement of the injection needle 351 when the device 100-7 is not properly oriented, for example, upside down, in order to prevent the compressed gas in vial 102 from being injected. Also, it is preferable to lock the injection needle 351 within the housing 304-7 after a single injection to reduce and preferably to prevent the exposure to the contaminated needle. Additionally, it is preferable to only allow displacement of needle 351 after insertion of diluent container 312. Accordingly, a locking mechanism comprising member 268 as shown in Figure 4B is provided to accomplish the foregoing. The member 268 has a first end configured to be moved by pushing member 353 and a second end

25 30 configured to displace a movable locking device, substantially similar to the device shown in Figure 4B.

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With the device 100-7 properly held by the user such that vial 102 is vertically oriented, the user presses pushing member 353 such that the injection needle 351 first extends out of the housing 304-7, thus penetrating the skin of the person being injected. Continued pressing of the pushing member 353 causes the  
5 second end 355 of injection needle 351 to puncture sealing member 357, thereby allowing the pressurized reconstituted drug 166 to travel from vial 102 into the person being injected. It may take in the range of 10-30 seconds to deliver the injection fluid. The pressing motion compresses spring 359 such that upon release of pushing member 353, the member returns to the original position, i.e., the needle  
10 is withdrawn within the housing 304 and locked therein.

Referring to Figure 14, a cutaway view illustrates a manifold of another preferred embodiment of the drug delivery device 100-8 in accordance with the present invention. The manifold 350 has two needles 352, 354 for the purpose of piercing vial 102 and diluent container 312, respectively. A flange, substantially  
15 similar to the flange 127 shown in Figure 6B, holds the septum or stopper 313 in place in the container 312. An extending member or communication chamber 356 which is in fluid communication with the needles 352, 354, has a membrane such as a hydrophilic membrane or barrier 360 disposed therein. It should be noted that the hydrophilic membrane needs to be wetted before it functions to minimize or  
20 preferably prevent the flow of gas into a user's tissue. The hydrophilic membrane allows gas, for example, air to pass freely till it comes in contact with liquid and gets wet. Thus, when wet, no air such as the controlled volume of air in the diluent container 312 can pass through the hydrophilic membrane, preventing air from entering the user's tissue. The presence of the hydrophilic membrane prevents risks  
25 caused by any wrong use of the device 100-8 by the user such as incorrect positioning of vials or containers.

Referring to Figures 15A-15B, cutaway views illustrate another preferred embodiment of a manifold of the drug delivery device in accordance with the present invention. The needle 352 pierces the vial 102 while needle 354 pierces the  
30 diluent container 312. The needle 354 and channel 352 on spike 352A are in fluid communication. Diluent 166 moves from the diluent container 312 into vial 102, thus mixing with the lyophilized drug to result in a reconstituted drug. A channel

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358 is in communication with an area 361 sealed by a stopper 313. Channel 358 also includes a hydrophilic membrane. Thus, upon the introduction of air to the channel, the membrane expands in the presence of air and disallows the passage of air therethrough.

5 In use, the user presses the button 363 which first moves injector needle 130 into the users skin. Further movement of the button 363 causes piercing member 172 to penetrate the stopper 313. This enables liquid drug/diluent solution to move, via the air pressure in the vial 102 through the injector needle 130 and the user's skin.

10 It should be noted that the embodiment illustrated with respect to Figures 15A and 15B being more position independent, is not subject to air blocking the flow of liquids through the gas impermeable membrane until all the drug solution has been transferred out of the vial 102. Figure 15A shows the position of channel 358 relative to channel 352. Thus, only if the vial 102 is completely filled with air  
15 would it pass into channel 358. In contrast, the embodiment illustrated with respect to Figure 14 and the absence of the lower channel 358 is more position dependent and thus subject to air blocking the flow of liquids through the gas impermeable membrane even while the drug solution is being transferred out of the vial 102.

Further, it should be noted that the delivery times of the drugs is dependent  
20 on the volume of vial which maybe adjusted. The pressure is adjusted in part by adjusting the vial volume size. A large vial volume of air relative to the drug would result in greater air pressure and faster drug delivery.

In the preferred embodiments of the present invention the drug vials and the diluent containers are shown as being inserted in the housing 304 and aligned in the  
25 same direction along parallel axes. In the alternative, it is contemplated that the vials and containers may not be aligned in the same direction along parallel axes. The vials and containers may be inserted along two different axes that are oriented at oblique or orthogonal angles relative to each other.

Referring to Figure 16 a cutaway view illustrates an alternate preferred  
30 embodiment of an injection device 236 in accordance with the present invention. The device 236 facilitates the sterilized injection of a prefilled cartridge or vial containing an injectable liquid, for example, a vial containing a liquid drug 160.

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The device 236 includes first opening 161 for receiving vial 102 and a manifold 370 including member 372 sealingly engaged with the first opening 161. Member 372 fixedly supports needle 374 and is supported by a collapsible volume, such as bellows 378, or any other device capable of injecting a fluid such as a gas upon  
5 being compressed. A check valve 380 ensures that the flow from the bellows is unidirectional, that is, the drug under pressure can not enter the bellows 378. The check valve 380 comprises a tubular member 381 adapted to deliver gas, for example air, to the vial 102. Air is moved out of the bellows and into the tubular member 332 by compressing, the bellows 378. The check valve 380 allows the flow  
10 of air out of the bellows 378 and into the vial but disallows the reverse flow of air from the vial into the bellows. Air from the bellows 378 is forced up through needle 374 and into vial 102 applying pressure to the contents of the vial 102. The liquid drug 160 is under pressure and is injected into the user directly from the vial 102. The injection process is the same as discussed earlier with respect to embodiments in  
15 Figures 13 - 15, in that the use of a U-shaped needle assembly is compressed into the skin to activate injection. As discussed earlier, due to the nature of the hydrophilic material, a hydrophilic membrane 360 in the drug delivery path minimizes and preferably prevents gas from being injected into the user.

Referring to Figures 17A-17C, cutaway views illustrate an alternate  
20 embodiment of the drug delivery device 100 in accordance with the present invention. The diluent container comprises a syringe 390. When pressure is applied to a plunger shaft 392, the diluent 166 is forced out of the syringe 390 through the channel 398 and into the contents of vial 102 via the needles 394, 396 which are in fluid communication with each other through the member 398. Thus, the diluent  
25 166 is provided to vial 102 under pressure and is mixed with the reconstituted drug to result in a reconstituted drug solution ready for injection or delivery under pressure to a patient. The drug solution is delivered to a user using a u-shaped needle assembly as disclosed with respect to Figures 13A - 13B, 14, and 15A and 15B. This syringe embodiment facilitates the use of a standard prefilled container or  
30 cartridge containing only a diluent. The device is flexible and does not require special means or training.

The present invention includes alternate preferred embodiments of injection devices. Figures 9A-9F illustrate an injection device 236 which facilitates the sterilized injection of a prefilled cartridge or vial containing an injectable liquid, for example, a vial containing a reconstituted drug 160. It is preferable to use a standard  
5 vial, for example, a 2 milliliter vial, with this device 236. As shown in Figure 9A, device 236 includes a first opening for receiving the vial 102 and a manifold including member 232 which is slidably and sealingly engaged with the first opening. Member 232 fixedly supports needle 224 and is supported by a collapsible volume, such as bellows 228, or any other device capable of injecting air upon being  
10 compressed. Needle 224 is in sealed communication with the bellows 228 as shown in Figure 9A. The vial 102 is pressed into the housing 304-5 such that needle 224 pierces the rubber stopper 112. This arrangement is shown in Figure 9B.

The vial 102 is further pressed into the housing 304-5 which forces member 232 to compress bellows 228, thus forcing the air contained in bellows 228 up  
15 through needle 224 and into cartridge 116. Now, as illustrated in Figure 9C, the cartridge 116 is under pressure for forcing the drug 166 into the person being injected. The bellows or other compression device can also be actuated by member 174-5.

As shown in Figures 9A-9F, device 236 is further provided with a pushing  
20 member 226 for displacing the injection needle 130-5 between a first position within the housing 304-5 and a second position outside the housing, or in an injection state. In the preferred embodiment a distal end of the injection needle 130-5 can extend out of the housing 304-5 in the range of 5-12 millimeters. In this particular embodiment, the injection needle 130 is preferably a "U" type needle having a  
25 second end 250 configured to puncture sealing member 230. Sealing member 230, which may comprise any puncturable material such as butyl rubber, maintains the liquid in the upper part of housing 304. As the user presses pushing member 226 into housing 304, the first end of the injection needle 130 first penetrates the skin of the person being injected as shown in Figure 9D. Continued pressing of pushing  
30 member 226 into the housing 304 causes the second end 250 of injection needle 130-5 to puncture sealing member 230, thereby allowing the reconstituted drug 160 to travel from cartridge 116 into the person being injected. This is illustrated in

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Figure 9E. The pressing of the pushing member 226 into the housing 304-5 compresses a spring such that upon release of pushing member 226, the member returns to the original position, i.e., the injection needle 130-5 is in the first position within the housing 304-5 as shown in Figure 9F. This embodiment may be further  
5 provided with a locking mechanism similar to that disclosed in Figures 4A-4K. With the injection needle locked within the housing 304-5, the device 236 may be safely discarded.

Further, Figures 18A-18C illustrate an injection device in accordance with an alternate preferred embodiment of the present invention. More particularly, the drug  
10 delivery device 400 includes a straight needle 402 having a lancet 404 disposed on a first end. A cavity 405 in the septum 406 contains a liquid drug under pressure. The straight needle 402 includes a side hole 407 disposed on the shaft. The second end 408 of the straight needle is blocked. In operation, as shown in Figures 18A, 18A-1, 18B and 18B-1, when the member 410 is moved forward toward the housing 412,  
15 the injection needle 402 is displaced from a first position in the housing 412 to a second position outside the housing such that the needle 402 penetrates the skin of the user. After the lancet 404 penetrates the user's tissue, continued pressing motion of the member 410 toward the housing causes the side hole 407 to be in fluid communication with the cavity 405 of the septum 406 creating a path for the drug  
20 under pressure to flow into the user's tissue. The straight needle punctures the septum 406 at two locations. As shown in Figure 18C, as the member 410 is released, the injection needle is withdrawn within the housing 412.

More particularly, referring to Figure 18A-1, a 3 part ring structure including member 414, latch 416, gap 418 and spring 419, as shown in Figure 18A provide an  
25 interlocking system. This safety mechanism which includes the members 410, 414, latch 416, gap 418 and spring 419 provides an interlock to ensure against reuse of the drug delivery device 300 and exposure of needle 402 after the first use. Once the member 410 is compressed the mating ridges 413A and 413B come together. The ridges are angled on one side to allow ridge 413B to pass under 413A when member  
30 410 is depressed against the housing 412. The ridges are pressed together when the force of the spring 419 moves member 410 away from the housing 412. Because the ridges interface at a right angle to the direction of movement of the member 410

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they serve to prevent further movement by the member and the needle 402.. This mechanism ensures that the device 400 is not reused.

Figures 19A-19F illustrate cutaway views of alternate preferred embodiments of systems which allow reconstitution of drug and subsequent transfer  
5 into a drug delivery device in accordance with the present invention. Once the drug is made into a solution it may be transferred into a user by means of direct injection as shown in Figure 11, for example, or into a drug delivery device such as an infusion pump, needleless injector or the like. The systems include a vial 420 containing a predetermined volume of a drug and a vial 422 containing a volume of  
10 a diluent. The use of standard vials facilitate the use of the drug delivery device by different drug suppliers.

An air source 424 maybe included for the delivery of drugs. With drugs of higher viscosity, the use of pressure becomes more important. As illustrated in Figure 19A, the sources of pressurized air can vary and may include, but are not  
15 limited to, a compressed air delivery supply 426, a chemical gas generator 428, a standard syringe 430 and a collapsible volume container, such as a bellow container 432. The air source supplies the driving force to the diluent volume which moves the diluent solution 434 into the standard lyophilized drug vial 420. Once reconstituted, the liquid drug is transferred via the air separator, such as a  
20 hydrophilic membrane 436, to a drug delivery system. It should be noted that spike 438 in the diluent vial 422 and spike 440 in the drug vial 420 each have two paths. The spike 438 has a first path for compressed air to enter the diluent vial 422 and a second path for the pressurized diluent 434 to be in fluid communication with the drug vial 420. The spike 440 has a first path for the pressurized diluent to enter the  
25 drug vial 420 and a second path for the delivery of the drug solution into a drug delivery device. As discussed earlier, it is contemplated that other drug delivery devices may be received into this system to receive the drug solution.

Referring to Figure 19B, the air source is a compressed air canister 426. The compressed air canister typically is a standard addition for domestic drug delivery  
30 devices. The user attaches the compressed air canister 426 to the drug delivery system 450 and punctures a seal 452 located in the compressed air canister. The air canister is then in fluid communication with the diluent vial 422 by means of



channel 453. Air is released from the compressed air canister 426 and is introduced into the diluent vial 422, which in turn forces the diluent solution 434 to move into the drug vial 420 via channel 455. After reconstitution is completed, the liquid drug is ready to be transferred. The concentration of the reconstituted drug can be  
5 controlled in this and other embodiments by changing the quantity of diluent transferred to reconstitute the drug. A hydrophilic membrane 436 in the drug delivery path minimizes and preferably prevents gas from being transferred to the drug delivery device.

Figure 19C shows a chemical gas generator 428 as the air source used in this  
10 particular embodiment to deliver the diluent 434 under pressure to the lyophilized drug vial. The chemical gas generator 428 includes a chemical compartment 456 which typically contains two materials 458, 460. The two materials 458, 460 can be two liquids or a liquid and a solid palette 460 that are separated during shelf life. It should be noted that the materials used in the chemical compartment 456 and the  
15 reaction that ensues during the mixing of the materials are safe and biocompatible. Pushing a member 462, in the chemical compartment 456 results in tearing of a seal 464, for example, aluminum foil, which separates the two materials 458, 460 during shelf life. The two materials are then in fluid communication and react to produce a gas such as, for example, carbon dioxide. The chemical gas generator 428 also  
20 includes a gas compartment 466 which is typically an air reservoir having a flexible enclosure 468. The carbon dioxide produced in the chemical compartment 456 due to the reactions enters the gas compartment 466 and is accommodated in the flexible layers 468 that form the gas compartment. The movement of the flexible layers 470, 472 force the air or carbon dioxide into the diluent vial 422 through the  
25 air pathway 423. It should be noted that the gas compartment 466 has a double layer 470, 472 comprising the flexible containment area. The two layers 470, 472 provide for safety as if the air or gas generated as a result of the reaction in the chemical compartment does leak, it can be accommodated between the flexible enclosure 468 of the gas compartment 466. Further, the gas compartment 466 is vented using a gas  
30 leakage pathway or vent port 474. The air that is released from the chemical gas generator 428 enters the diluent vial 422 via the channel 423 which in turn forces the diluent solution 434 to move into the drug vial 420 via the channel 425. After

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reconstitution is completed, the drug is ready to be used, and is transferred to a drug delivery system such as one described with respect to Figure 19B.

Referring to Figure 19D, the air source used in this particular embodiment to deliver the diluent under pressure is a standard syringe 430 or an air reservoir. The syringe 430 is locked at an end of travel position. When pressure is applied to a  
5 syringe 430 is locked at an end of travel position. When pressure is applied to a plunger shaft 480 the air is forced out of the syringe 430 and into the contents of the diluent vial 422 through the needle 482 and needle 434 which are in fluid communication through the member 484. The diluent 434 is then forced into the drug compartment or drug vial 420 via member 484 under pressure which provides  
10 for the mixing with the lyophilized drug to result in a reconstituted drug which is then ready for injection or delivery under pressure to a user. In an alternate embodiment, a lever can be included to reduce the force required for pushing the plunger member 480. The lever will increase the displacement and thus delivery of pressurized air to the diluent container in this case, the drug solution may be injected  
15 as shown in Figure 19D, the sectional of which is the same as shown and described in other needle assemblies, for example, shown in Figures 11, 13, 14, 15, 16, and 32 or transferred into a drug delivery device.

Referring to Figure 19E, the air source used in this particular embodiment to deliver the diluent under pressure to the lyophilized drug is a collapsible volume  
20 container such as a bellows container 432. A check valve 488 or a one-way valve insures that the flow from the bellows container 432 is unidirectional, that is, the drug or diluent can not enter the bellows. The check valve 488 comprises a tubular member 490 adapted to deliver gas, for example air, to the diluent vial 422. The resilient nature of the bellows is checked by the check valve 480 which does not  
25 allow air to enter the bellows and thus reinflate the bellows once the bellows have been compressed and air has exited. Once compressed, air contained in the bellows 432 is forced through needle 438 and into the diluent vial 422 via channel 491 applying pressure to the contents of the diluent vial. The diluent solution 434 in turn, is delivered under pressure to the drug vial 420 where the drug is reconstituted  
30 and can be transferred either by injection as described above or into a drug delivery device, as also described and shown relating to the embodiment of Figure 19A.

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Referring to Figure 19F, the air source used in this particular embodiment to deliver the diluent under pressure is cylinder 490. This embodiment is similar to the embodiment containing a standard syringe as described with respect to Figure 19D. The plunger 492 is depressed to compress the air in the cylinder 490. The air is  
5 driven into the diluent vial 422 through channel 494 which brings the cylinder and the diluent vial in fluid communication. The pressurized diluent in diluent vial 422 then moves into the vial 420 and mixed with the drug. The pressurized drug solution is then ready to be delivered. This can either comprise delivery to a drug delivery device as described with respect to the embodiment of Figure 19A or  
10 injected as shown in the present embodiment having a straight needle assembly as shown and described in Figure 18.

Referring to Figures 20A-20C, an alternate embodiment of the drug delivery system 498 in accordance with the present invention includes standard vial 500 containing a liquid drug 502. A volume of gas, for example air, contained in an air  
15 chamber 504 is introduced in the standard liquid drug vial 500, creating air pressure above the liquid drug which allows for delivery of a liquid drug under pressure. The usage is position dependent, that is the delivery of the liquid drug, is performed with the standard vial 500 in a vertical position. In addition, a hydrophilic membrane minimizes or preferably prevents the introduction of the extra volume of air into the  
20 user's tissue.

In use, as shown in Figure 20A, the standard vial 500 containing the liquid medicament 502 is inserted into the drug delivery device 498 in accordance with the present invention. An air chamber 504 is provided which upon insertion of the drug vial 500 and the puncturing of the seal 506 of the vial, is in fluid communication  
25 with the drug vial. Once inserted, the lip 505A of a standard vial 500 is locked into position by means of a pair of arms 505 having ridges 507 projecting inwardly therefrom. The injector system is the straight needle 402 embodiment as disclosed in Figures 18A-18C. Once the air from the air chamber is introduced into the standard drug vial 500 the liquid drug is pressurized and is ready to be injected using  
30 the injector system described with respect to Figures 18A-18C. After injection into the user's tissue, the needle is retracted automatically. The drug delivery device 498 is then disposed.

Referring to Figure 21, an alternate preferred embodiment of a drug delivery system 510 which uses standard vial 500 containing a medicament is disclosed. A plunger 512 is included in the drug delivery device 510. In order to reduce forces which are required to insert the standard vial 500 in the drug delivery device 510. In  
5 an alternate embodiment, the drug delivery system 510 can have a compact configuration without a plunger. Snaps 514 lock the standard vial 500 into position. Snaps 516 hold the end portion of the vial having the seal 506 in place to ensure that the spike 518 pierces the seal 506 of the vial 500 before the vial is moved in the downward direction. Air in the air chamber 520 is delivered to the vial 500 when  
10 the air is compressed and displaced by the downward movement of the vial 500. The liquid drug under pressure is delivered to an injector using tubing 522. A hydrophilic membrane 524 minimizes or preferably prevents gas from entering the user's tissue. The injector system used can be similar to one described with respect to Figures 18A-18C. The member 410 is moved to displace the injection needle  
15 402.

Referring to Figures 22A-22E, the views illustrate an alternate preferred embodiment of the drug delivery system 530 in accordance with the present invention. This particular embodiment may be used as a reconstituted system and a drug delivery system and includes two vials 532, 534 a first containing a diluent 533  
20 and a second containing the lyophilized drug 535. In addition, there is an air delivery system for pressurizing system, such as a built-in air cylinder 533 in fluid communication with the diluent vial 532 which is disposed between the lyophilized drug vial 534 and the diluent vial 532. Air is pushed into the diluent vial 532 forcing the diluent 533 from its vial into the lyophilized drug compartment or vial  
25 534. After reconstitution is completed, the liquid drug is ready for injection. A hydrophilic membrane is used as an air separator to minimize or preferably prevent the entry of air into the user's tissue. This particular embodiment uses a straight needle 402 injector system as described with respect to Figures 18A-18C. Additionally, a positioning interlock, such as the mechanism, described with respect  
30 to Figures 2A-2B is used. Further, in an alternate embodiment, the air cylinder can be replaced with a standard syringe to be the air source as shown in Figures 22D and 22E. A check valve (as shown in Figure 16) disposed in the air inlet between the

syringe and manifold is included in the embodiment containing the syringe.

The drug delivery system of the present invention is used to deliver an accurate volume of a drug solution. The predetermined volume can be delivered using different methodologies. A first embodiment controls the dose by changing the height of the outlet spike 535 in the liquid drug vial 537 as shown in Figures 23A, i.e. the higher the spike, the lesser is the amount of drug transferred out of the vial 537. The spike is adjusted by means of threads 539 upon which the spike rotates or upon which it sealably slides. This can be used for to transfer or to inject the drug solution. Another preferred embodiment which increases the accuracy of the volume of drug delivered uses the residual drug volume as a parameter to indicate the volume delivered. One way of controlling delivered drug solution volume is to use the assembly shown in Figure 23B. After the drug is pushed in solution in vial 102 the solution may be pulled into cavity 541 by piston 555. The cavity 541 has indications thereon to aid the user in determining the proper volume. At the desired level, the piston is stopped. The drug solution is then transferred from the cavity 541 either via a needle into a user or into a drug delivery device. Yet another embodiment to provide an accurate volume of drug is disclosed with respect to Figures 24A-24C and Figure 25. The reconstitution system having the vial containing the reconstituted drug is essentially used as a filling station by a detachable delivery device, for example, a standard syringe or a pen type pump.

Referring to Figures 24A-24C a position independent injector system 540 is illustrated. The drug 545 is reconstituted similar to the description provided with respect to earlier systems such as illustrated in Figure 19F. After the drug has been reconstituted it can be aspirated by a conventional standard syringe 542 for the exact dose required. The accuracy using this method is about +/- 5%. The fluid level in the cavity 550 is controlled by adjusting the pressure and geometry of the device 540. The needle is held in place by the elastomeric septum or stopper 552. In use, once the reconstituted drug is aspirated into the syringe 542 by moving plunger 548 which moves the stopper 554 upwards allowing the syringe 542 to be filled with the liquid drug, the syringe 542 is removed from the drug delivery device 540. The accuracy of the volume of the liquid drug delivered is determined by the scale on the syringe. The user then injects the drug and disposes of the syringe by one of

several potential ways. One of the ways of disposing the syringe is by attaching the syringe to the open cavity 550 left in the drug delivery device 540. A second way is by securing the needle 547 prior to disposing the syringe by locking it with a piece of plastic tubing. The system 540 and procedure used is free of air inclusions and does not require an air separator. The syringe needle 547 is placed in a closed cavity penetrating a septum 544 and thus allows for fluid communication between the needle 547 and the reconstituted drug. The volume of the closed cavity is designed to ensure the availability of the liquid drug to the needle 547 under controlled pressurized conditions. The position of the syringe piston 548 is fixed under pressurized conditions and the dose is manually aspirated from the syringe.

Referring to Figure 25 an alternate preferred embodiment of the drug delivery system 540 as described in Figures 24A-24C is illustrated. The reconstitution stage is similar to the one described with respect to Figures 24A-24C. However, the injector system including an attachable delivery device is different. The user dials or tunes the required dose using a pen type pump 560 that includes a dial 562 that is inserted into the drug delivery device. The dialing process retracts a floating piston which moves upward and creates an internal pressure which provides for aspiration of the reconstituted drug. A trigger 564 releases a preloaded spring to push the floating piston. Thus aspiration occurs by dialing the dose into the pen-type injector. Once the pump 560 is filled as indicated by an indicator 566, it is disconnected from the filling device. Injection and disposal of the pump is performed after disconnection with a process similar to the process described with respect to Figures 2A-24C.

Figures 26A-26D are perspective views of a drug transfer system having a drug delivery device 510 in accordance with the present invention. A diluent vial is inserted in a cavity 572 and a lyophilized drug vial is inserted in cavity 574. A cavity 576 accommodates an air pressurization system to deliver drugs having a low level of viscosity. Further, the drug transfer system includes an access 578 to receive a drug delivery device. The drug is transferred thereto via a needle 580.

Figures 27A-27C are cutaway views of a preferred embodiment of a transfer system 600 in accordance with the present invention. Once pressurized by the air in cavity 603, the liquid drug from vial 602 is transferred to a drug delivery device 604

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via an extension 606. The liquid drug flows out of the vial 602 through spike 608 and through the tubing 610 into the needle 616 which is received into the drug delivery device 604.

Referring to Figure 27B, the drug delivery device 604 is attached to the transfer system 600. The filling process continues until the entire drug level reaches the outlet 604A (shown in phantom in Figure 26B) of the device 604. At this point the filling process is completed. It should be noted that during the filling process, if the user stops pushing the vial 602 into the transfer system 600 the drug may drain into the cylinder 614. This is prevented by getting the friction forces higher than the impedance of the tubing 610 to the drug flow. In the alternative, it is also possible to dispose a one-way valve at the end of the tubing 610. Once the drug delivery device 604 is filled with a liquid drug, it is disconnected from the transfer system 600. Any residual drug in the system 600 can stay protected, and the needle 616 is retracted and as described earlier with respect to the needle locking mechanisms is secured in the cover 606, and cannot be reexposed to cause harm or injury.

Figures 28A-28C are cutaway views of the operation of another preferred embodiment of a drug delivery system 630, in particular of a position independent injection system in accordance with the present invention. In this embodiment, the injection system 630 is position independent, that is the injector is not required to be in a vertical position during the injection process. Referring to 28A, the drug delivery system 630 includes a vial 632 containing the liquid drug 634. The liquid drug 634 flows through the spike 636 along a tube 644A into a cavity 652. The spike includes two paths, one path 642 for delivering pressurized air into vial 632 from chamber 641 and another path 644 to deliver the liquid drug to the user via a needle 664. The liquid drug exits from the path 644 and travels along tube 644A disposed at the bottom of the spike. A one-way valve 638 insures the unidirectional flow of the liquid drug 634 into the cavity 652A. Spring 640 holds piston 656 within the cavity 652. A floating piston 650 moves in the cavity 652. A seal 654 is included in the floating piston. Member 660 rests atop a needle assembly 664A. Member 660 is hingedly connected to member 662. Member 662 has a finger 662A.

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Prior to use, the finger 662A rests within an aperture 662B of the housing 660A. The notch 658 is the end of travel position for the piston 656.

The path 642 from the air chamber 641 to the vial 102 pressurizes the vial by delivering air thereto. The air chamber 641 is depleted of air when the vial is moved  
5 downward. As the vial moves downward, a member 641A sealably slides within the walls of the chamber and forces the air into the vial. The member 641A is prevented from leaking air out of the chamber by the seal 641B.

In use, when vial 632 is pushed into the device 630, air from the cavity 641 enters into the vial 632 and pressurizes the liquid drug. This drug 634 under  
10 pressure flows via path 644 through the one-way valve 638 into the left side of the cavity 652. Pressurized air pushes the floating piston 650 to the right side of the cavity 652. The floating piston 650 moves until the position of the notch 658, which is the end of travel position for the piston 656 and thus for filling of the cavity 652. Thus, as illustrated in Figure 28B, an accurate volume of liquid drug is filled in  
15 cavity 652 and the device 630 is ready to be used.

As illustrated with respect to Figure 28C, once the member 660 is depressed, it causes the needle 664 to move downwardly outside the housing 660A and into the user's tissue. Member 662 is hingedly connected to member 660. When 660 is depressed, it causes member 662 to move upwardly disengaging the finger 662A  
20 from the aperture 662B and enables the spring 640 to return to a less compressed state. As it does, the spring 640 forces the piston towards the opposing end of the cavity 652. This causes the liquid drug therein to move via channel 652A and needle 664 into the user's tissue, the piston 656 is released due to the movement of member 662 in the upward direction. The piston 656 moves to the left. The floating  
25 piston 650 is under pressure and moves the liquid drug in cavity 652 through the injector needle 664 and into the user. It should be noted that after delivery of the liquid drug, the position of the floating piston 650 depends on the load on the spring 640. To prevent the flow of residual drug under pressure, the spring 640 continues to be in a preloaded state. The seal 654 is pushed to the left side of the cavity 652  
30 under pressure of spring 640 to seal against the exit of the pressurized residual drug via the channel 652A. Although disclosed as having a pushing spring 640, other



mechanisms may be included in the injector system to result in a position independent injector.

Referring to Figure 28D, a cutaway view of a spike 636 which brings the liquid drug 634 in fluid communication with the injector system is illustrated. The spike 636 penetrates the septum 639 of the vial 632 when the vial is inserted into the cavity 640. The spike functions as a piston 641A and is sealably and slidably movable by means of the seal 641B within the interior walls of the chamber 641. As described hereinabove, the spike also consists of two paths, an air inlet 642 and a drug outlet 644. Once the vial 632 is inserted, pressurized air enters the vial 632 from an air chamber 641 and forces the liquid drug 634 via a flexible tube 644A to the injector system. The filling process for the injector system in a preferred embodiment is preferably done under a maximum pressure gradient of 0.3 bar. This includes a margin for example, priming at an altitude of 5,500 feet and is the maximum expected back pressure.

Figures 29A and 29B illustrate partial cutaway views of another preferred embodiment of the drug transfer system 670 in accordance with the present invention.

The drug vial 672 containing the liquid drug 674 is inserted into a cavity 676. A spike 678 provides air into the liquid drug vial 672 for pressurization of the drug 674 and additionally the spike provides for an outlet for the liquid drug to be delivered to a drug delivery system 680. The drug transfer system 670 is in fluid communication with the liquid drug vial 672 through a flexible tubing 682 and a needle 684. A hydrophobic membrane 686 is disposed in the flexible tubing 682 to prevent the transfer of air into the drug delivery system. This hydrophobic membrane 686 prevents back flow. The air to pressurize the liquid drug 674 is provided by air in the reservoir 675. Further, a latch mechanism 688 secures the vial 672 to the detachable delivery system 680 during a filling process.

Referring to Figure 29A -1, an enlarged view of the interface between the drug transfer system 670 and the detachable drug delivery device 680 is illustrated. A hydrophobic membrane 692 is disposed at the interface for blocking the flow of the drug once the drug delivery device 680 is filled. An elastomeric cover 694 is

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disposed around the needle 684 for protection against the needle 684. Tab 693 is pulled off to remove the hydrophobic membrane 692 prior to use of the device 680.

In operation the liquid drug vial 672 is pressed into the cavity 676 which causes the air in the reservoir 675 to be compressed and enter the liquid drug vial 672. Air is prevented from leaking out of the cavity 675 by means of seal 685. The liquid drug 674 is pressurized and delivered through the spike outlet 690. Residual air from the air reservoir 675 is vented from an opening in the latch mechanism 688 once the latch is disengaged from the drug delivery device at the end of travel of the vial and subsequent end of the transfer process.

Referring to Figures 30A and 30B, the two piece 696, 697 construction of the manifold in accordance with the present invention is illustrated. The manifold is a biocompatible material such as, for example, polycarbonate or acrylic or pvc molding having a gas impermeable membrane 698 welded in the part 696. The two pieces 696, 697 are ultrasonically welded together.

Referring to Figures 31A - 31E, perspective views illustrate an alternate preferred embodiment of a drug delivery system 700 in accordance with the present invention. This particular embodiment maybe used with the reconstituted drug delivery system and includes two vials 702 and 704, a first containing a diluent and a second containing a drug that needs to be reconstituted. In addition there is a pressurizing system, such as a built- in cylinder 706 in fluid communication with the diluent vial 702. The built-in pressurization system such as the cylinder 706, is disposed between the lyophilized drug vial and the diluent vial. A plunger 708 is slidably received into the cylinder 706 to provide the necessary air pressure to effect drug transfer. Air is pushed into the diluent vial forcing the diluent from its vial into the lyophilized drug compartment or vial 704. As discussed previously, a hydrophilic membrane is used as an air separator to minimize or preferably prevent the entry of air into the user's tissue. In use, a diluent vial is inserted into the drug delivery system 700 followed by the insertion of a drug vial. The plunger 708 is pushed downwards to pressurize the air in the cylinder 706 and deliver it to the diluent vial 702. Once the diluent solution is pressurized it is delivered to the drug vial 704 to reconstitute the drug. Pressing the knob mechanism 710 displaces an injection needle which is used to inject the reconstituted drug into a user tissue. The

depression of the knob mechanism and subsequent injection is similar to that described earlier with regard to either the straight needle assembly shown in Figure 18 or the U-shaped needle shown in Figures 11, 13 through 17.

Referring to Figures 31F and 31G, two preferred embodiments 711, 713  
5 which provide a visual indication of device orientation are illustrated. The vertical indicators 711, 713 are shown as being disposed on the top of the plunger 708, however their location can vary to provide appropriate visual indication. In the first embodiment of the vertical indicator 711, a metal ball 714 rests upon a curved surface having visual indicators or scale 712 thereon. The ball 714 is enclosed  
10 within a clear casing 712A. The positioning of the ball 714 in the middle of the scale is an indication of vertical orientation. In the second embodiment 713 of the vertical indicator, an air bubble 716 disposed in a liquid 718 enclosed within a clear housing 718A is used as the visual indicator of orientation with respect to the scale 719. The positioning of the air bubble 716 in the middle of the scale is an indication  
15 of vertical orientation.

Referring to Figures 32A-32E, perspective views illustrate a further alternate embodiment of the drug delivery system 720 in particular a reconstitution and injection system, in accordance with the present invention. In this embodiment the reconstitution of the drug occurs by the mixing of the diluent solution with the drug.  
20 A separate pressurization system for the diluent is not required for this particular embodiment and can only be used with low viscosity drugs. In use, the knob 730 is moved in a counter clockwise direction to begin the reconstitution process of the drug which opens a pathway connecting the diluent with the drug. The knob 730 is turned from a non-use position (as indicated when notches A and B align) to a ready  
25 to use position as indicated with the alignment of notches B and C. At this point, the knob 730 may be depressed and the solution injected. The internal pressure of the diluent vial and gravity cause the diluent to transfer to the vial containing the drug. Further movement of the knob or dial 730 activates an injection needle which interfaces with the user's tissue to deliver the reconstituted drug. Again, the  
30 injection assembly is similar to the embodiments shown in Figures 11, 13-17.

Referring to Figures 33A - 33I, cutaway views of preferred embodiments of the drug delivery system emphasizing the interlocks disposed to provide for a safe

system are illustrated. Referring in particular to Figure 33A and 33B, the interlocks as required during shelf life of the drug delivery device 750 are illustrated. The end of the cylinder 752 has a biasing lip 766 extending outward to matingly fit with wall 758 and the lip must be flexible enough to bend with the pressure of wall 758 when  
5 vials are inserted in the assembly. During shelf life the cylinder 752 is secured by latch 754 and mating lip 756. This mating fit prevents the movement of the movable cylinder 752 in the vertical direction prior to use. As previously described, the cylinder 752 provides pressurized air to the drug delivery system 750. The movement in the downward direction of the cylinder 752 is minimized or preferably  
10 prevented by holding the latches 754 and 756 on the wall 758. An upward movement of the cylinder 752 is prevented by latch 754.

Referring to Figure 33C, the next step includes the insertion of the vials 760 and 762 into the device 750. Only after the insertion of both vials 760, 762 is the cylinder 752 free to be pushed in the vertical direction. The insertion of the vials  
15 forces the lip 766 inward enabling it to clear the wall 758 and thus enable the cylinder 752 to move downward. In addition, the latches 754 secure the vials in the device 750.

Referring to Figures 33D and 33E, the interlocks that play a role once the cylinder 752 is pushed as illustrated. The cylinder 752 is pushed downward until the  
20 end of travel position and is locked by the mating of lip 766 and interlock element 768. Again, as described above with regard to pre-use, the lip 766 moves downward and catches on element 768 and moves to a radially expanded position which prevents the cylinder from travelling upward again. A locking element 768 keeps the cylinder in the bottomed out position. The element 768 is formed as a part of the  
25 wall 758.

In the area where the drug solution is injected there is a pushing member that moves in a relative perpendicular fashion to the direction of travel by the cylinder. A ball 772 is positioned prior to use within the housing to prevent depression of the member 776. When the cylinder is fully depressed, the lip 766, pushes a member  
30 770 which allows the ball 772 to drop into a groove 774 making the movement of the pushing member 776 possible only if the device is in a vertical orientation.

Referring to Figures 33F and 33G, during the injection process different interlock elements insure the safe use of the drug delivery system. As the pushing member 776 is depressed, which is only allowed if the drug delivery system 750 is in a vertical orientation, the horns 778 spread the latch 780 which allows the

5 member 770 to press the ball 772 in the upward direction. Note the pushing member 776 is already pushed to expose the needle 782.

Referring to Figures 33H and 33I, the interlocks during the phase of disposing of the drug delivery device which follows the injection phase are illustrated. The pushing member 776 is released by the action of the spring 777

10 pushing the member 776. Since the movement of the ball 772 was limited by the body of the member 776, with the release of the member 776, the ball 772 can now move back into the groove 774 as it is assisted by the pressure applied by the rear shell latch 780. This locks the pushing member 776 into position thereby preventing further use of the drug delivery device 750.

15 Referring to Figures 34A through 34D, a preferred embodiment of the drug delivery device having an end of delivery indicator is illustrated. As discussed previously with respect to preferred embodiments of the drug delivery system of the present invention, the drug delivery system is activated by pressurized gas, for example, air. The air forces the drug to the injection site by pressurizing the drug.

20 A hydrophillic membrane minimizes and preferably prevents the passage of air into the user's body. The hydrophillic membrane is disposed in the drug path to the user's tissue. Once wetted, the hydrophillic membrane allows liquid drug to proceed into the user's tissue and stops the passage of air into the user's tissue. In order to insure the effectiveness of the membrane, the hydrophillic membrane has to become

25 wetted. To enhance the effectivity of the drug delivery device, a hydrophobic membrane is also positioned in the drug path. Referring to the figures 34A and 34B, an inlet 800 which provides the liquid drug 802 into a cavity 803 has both a hydrophobic membrane 806 and a hydrophillic membrane 810 disposed therein. The hydrophobic membrane 806 allows air to pass, but stops liquids. On the other

30 side of the cavity 803 the hydrophillic membrane 810 allows liquid drug to pass while stopping the flow of gas. At one end of the hydrophobic membrane 806 a flexible elastomeric diaphragm is disposed that acts as an indicator once filled with

gas, for example, air. The membrane being flexible, once filled with air gives an external indication for end of delivery. The presence of air occurs only once the liquid drug has been delivered. It should be noted that the hydrophillic membrane 810 is disposed close to the injection site as it allows liquid to go through to the injection site minimizing or preventing the flow of gas into the user's tissue. Figure 34D illustrates a manifold structure utilizing the end of delivery indicator 804 built into the manifold. The septum 814 surrounds a cavity containing the liquid drug. The spikes 816 and 818 interface with the elastomeric stoppers of vials containing a diluent and a medicament.

10        Figure 35 graphically illustrates the delivery profile from a high volume vial having no additional air pressure in the vial. The profile illustrates pressure (in millibars) versus time (in seconds). The initial pressure in the vial is in the order of about 300 millibars which decreases during the delivery process to approximately 0 millibars at the end of delivery process. This is in contrast to the pressure in a vial that initially contained approximately 3 milliliters of air as illustrated with respect to Figure 33. As a result, there is no residual air pressure in the vial once delivery is complete. The delivery process spanned a time period of approximately 86.4 seconds.

20        Figure 36 graphically illustrates delivery duration and delivery pressure with respect to an air volume in a vial. Three different profiles are illustrated with a first one 830 which is indicative of the pressure (in millibars) before delivery, a second profile 832 indicative of the residual pressure of the delivery and a third profile 834 which is indicative of delivering 0.95 ml of a liquid drug over a time span of about 8 seconds.

25        Figure 37 is a graphical illustration of the delivery parameters for an injection of a liquid drug having no additional air in the vial. As delivery of the drug occurs, the pressurization within the liquid vial decreases over the approximately 17 seconds of delivery. These curves illustrate test results of the delivery process of approximately 1 gram of liquid drug using a single drug delivery device for the same time period.

30        Figure 38 illustrates test results showing the air pressure gradient on hydrophilic membranes used to minimize or preferably prevent the entry of gas for

example, air into the user's tissue. The test results prove membrane safety to insure that the membrane can withstand the pressures in the order of 2,700 millibars for a time duration of about six minutes.

Figure 39 graphically illustrates the performance of a drug delivery device in accordance with the present invention. Three delivery profiles 840, 842, 844 (in ml) vs. time (in seconds) are illustrated for a reconstituted lyophilized drug delivery system. The system includes a 0.45 micron pore size hydrophilic membrane to minimize or preferably prevent the flow of gas into the user's tissue. This particular pore size of the membrane provides an adequate particle filter and also allows the shortest time to deliver the drug to the user's tissue.

Figure 40 is a flow chart that describes the methods for delivery of a lyophilized drug in accordance with the present invention. The methods include the step 899 of inserting the drug and diluent containers into the drug delivery device. Further per step 900, the method includes activating a pressurized air source which in turn is followed by the step 902 of pressurizing a diluent solution in a diluent vial. As discussed with respect to Figures 19A-19F, the pressurizing can be provided by subsystems which include but are not limited to a compressed air supply, a chemical gas generator, a collapsible volume air supply, a standard syringe or cylinder.

The methods further include the step 904 of delivering the pressurized diluent solution to the lyophilized drug vial. The lyophilized drug is reconstituted per step 906 as a result of the mixing of the diluent with the lyophilized drug. The methods further include the step 908 of providing the liquid drug to an injector system or transferring the liquid drug to a detachable delivery device. The liquid drug is then injected into a user's tissue per step 910. The injection needle is then moved to a safe storage position per step 912.

Figure 41 is a flow chart that describes the methods for delivering a liquid medicament in accordance with the present invention. The methods include the step 913 of inserting a drug container such as a vial into the drug delivery system. Further, per step 914 the method includes activating a pressurized air source for low viscosity drugs. It should be noted that for drugs with a high level of viscosity no pressurization may be required. The method then includes the step 916 of pressurizing the standard drug vial. The pressurized liquid drug is transferred to a

drug delivery system such as an injector system, or detachable delivery devices per step 918. The liquid drug is then injected into the tissue of a user per step 920. The method further includes the step 922 of retracting the injector into a safe storage position.

- 5           It is further appreciated that the present invention may be used to deliver a number of drugs. The term "drug" used herein includes but is not limited to peptides or proteins (and mimetic thereof), antigens, vaccines, hormones, analgesics, anti-migraine agents, anti-coagulant agents, medications directed to the treatment of diseases and conditions of the central nervous system, narcotic antagonists,
- 10 immunosuppressants, agents used in the treatment of AIDS, chelating agents, anti-anginal agents, chemotherapy agents, sedatives, anti-neoplastics, prostaglandins, antidiuretic agents and DNA or DNA/RNA molecules to support gene therapy.

- Typical drugs include peptides, proteins or hormones (or any mimetic or analogues or any thereof) such as insulin, calcitonin, calcitonin gene regulating
- 15 protein, atrial natriuretic protein, colony stimulating factor, betaseron, erythropoietin (EPO), interferons such as  $\alpha$ ,  $\beta$  or  $\gamma$  interferon, somatropin, somatotropin, somastostatin, insulin-like growth factor (somatomedins), luteinizing hormone releasing hormone (LHRH), tissue plasminogen activator (TPA), growth hormone releasing hormone (GHRH), oxytocin, estradiol, growth hormones, leuprolide
- 20 acetate, factor VIII, interleukins such as interleukin-2, and analogues or antagonists thereof, such as IL-1ra; analgesics such as fentanyl, sufentanil, butorphanol, buprenorphine, levorphanol, morphine, hydromorphone, hydrocodone, oxymorphone, methadone, lidocaine, bupivacaine, diclofenac, naproxen, paverin, and analogues thereof; anti-migraine agents such as sumatriptan, ergot alkaloids, and
- 25 analogues thereof; anti-coagulant agents such as heparin, hirudin, and analogues thereof; anti-emetic agents such as scopolamine, ondansetron, domperidone, metoclopramide, and analogues thereof; cardiovascular agents, anti-hypertensive agents and vasodilators such as diltiazem, clonidine, nifedipine, verapamil, isosorbide-5-monotritate, organic nitrates, agents used in treatment of heart
- 30 disorders, and analogues thereof; sedatives such as benzodiazepines, phenothiazines, and analogues thereof; chelating agents such as deferoxanone, and analogues thereof; anti-diuretic agents such as desmopressin, vasopressin, and analogues thereof; anti-



- anginal agents such as fluorouracil, bleomycin, and analogues thereof; anti-neoplastics such as fluorouracil, bleomycin, and analogues thereof; prostaglandins and analogues thereof; and chemotherapy agents such as vincristine, and analogues thereof, treatments for attention deficit disorder, methylphenidate, fluvoxamine,
- 5 bisoprolol, tacrolimus, sacrolimus and cyclosporin.

- While this invention has been particularly shown and described with references to preferred embodiments thereof, it will be understood by those skilled in the art that various changes in form and details may be made therein without departing from the spirit and scope of the invention as defined by the appended
- 10 claims. For example, some of the features of the position independence can be used in connection with reconstitution combination systems, transfer systems or injection systems. Likewise interlock features may be used with any of the aforementioned systems.

## CLAIMS

What is claimed is:

1. A transfer system comprising:
  - a housing;
  - 5 a first port in said housing that receives a first container having first contents therein;
  - a second port in said housing that receives a second container that contains second contents to be mixed with the first contents to form a material;
  - 10 a first channel that provides communication between the first container and the second container; and
  - a second channel to transfer the material mixture.
2. The system of Claim 1 wherein the first channel comprises a fluid pathway in a manifold, the manifold further comprising the second channel.
- 15 3. The system of Claim 1 further comprising an interlock such that the first container must be received by the first port before the second container can be received by the second port.
4. The system of Claim 1 further comprising a first penetrating member fixed to said housing and that penetrates said first container.
- 20 5. The system of Claim 1 further comprising a second penetrating member fixed to said housing and that penetrates said second container.
6. The system of Claim 1 further comprising an actuator in the housing that transfers the contents from the second container into the first container.

7. The system of Claim 1 wherein the material is a drug that is transferred with a needle into tissue.
8. The system of Claim 1 wherein the material is a drug that is transferred to a drug delivery device.
- 5 9. The system of Claim 5 further comprising a sealing element in said second container that allows a fluid from second container to flow through said second penetrating member to said first container when an actuator moves the sealing element.
10. The system of Claim 9 wherein the actuator includes a pressure source.
- 10 11. The system of Claim 1 further comprising a support surface on the housing such that the first and second containers are received along axes extending orthogonal to the support surface.
12. The system of Claim 1 wherein the contents of the first container is a solid material.  
15
13. The system of Claim 1 further comprising a metering element that controls a volume of the drug being transferred.
14. The system of Claim 13 wherein the metering element includes a penetrating member that extends an adjustable distance into the first container.
- 20 15. The system of Claim 1 further comprising a position indicator that indicates a position of the first container.
16. The system of Claim 1 further comprising a transfer indicator that indicates movement of the drug within the housing.

17. The system of Claim 1 further comprising a membrane that impedes that transfer of a gas.
18. The system of Claim 1 further comprising a support surface on the housing such that a user can insert the first container and the second container with one hand while the housing is positioned with the support surface.
19. The system of Claim 12 wherein the solid material comprises a powder.
20. The system of Claim 12 wherein the solid material is a lyophilized drug.
21. A method for forming a drug comprising:  
providing a housing that receives a first container having a first contents therein and that receives a second container having a second contents therein;  
inserting a first container and a second container into the housing;  
moving the second contents from the second container into the first container along a channel in the housing to form a solution in the first container; and  
transferring the solution from the first container.
22. The method of Claim 21 further comprising the step of pressurizing the second container.
23. The method of Claim 22 wherein the step of pressurizing the second container includes the use of one of a compressed air container, a changeable volume container, a syringe, and a chemical gas generator.
24. The method of Claim 21 wherein the step of moving second contents from the second container to the first container along a channel comprises the step of providing a fluid pathway for liquid to travel from the second container into the first container.

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25. The method of Claim 21, further comprising providing a first contents that is a liquid drug.
26. The method of Claim 21 further comprising providing a first contents that is a powder.
- 5 27. The method of Claim 21 further comprising providing a first contents that is a lyophilized drug.
28. The method of Claim 21 wherein a user inserts the first container and the second container into the housing using one hand.
29. The method of Claim 21 further comprising providing a manifold in the  
10 housing in which the channel has been formed.
30. The method of Claim 29 further comprising providing a second channel in the manifold through which the solution is transferred from the first container.
31. The method of Claim 21 further comprising providing an interlock such that  
15 the first container must be inserted before the second container.
32. The method of Claim 21 further comprising providing a position indicator that indicates a position of the housing to a user.
33. The method of Claim 21 further comprising providing a transfer indicator that indicates a movement of the solution to a user.
- 20 34. The method of Claim 21 further comprising a membrane that prevents movement of a gas.
35. A drug transfer system comprising:

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- a housing having a manifold and an actuator, the manifold having a  
first channel that provides communication between the first container and second  
container and a second container to transfer the drug from the first container;  
a first port in said housing that receives a first container having a  
5 powder therein; and  
a second port in said housing that receives a second container that  
contains a fluid to be mixed with the first contents to form a material;  
a first channel that provides communication between the first  
container and the second container; and  
10 a second channel to transfer the material mixture.
36. The system of Claim 35 further comprising an interlock such that the first  
container must be received by the first port before the second container can  
be received by the second port.
37. The system of Claim 35 further comprising a first penetrating member fixed  
15 to said housing and that penetrates said first container and a second  
penetrating member fixed to said housing and that penetrates said second  
container.
38. The system of Claim 35 wherein the material is a drug that is transferred  
with a needle into tissue or the drug is transferred to a drug delivery device.
- 20 39. The system of Claim 35 further comprising a pressure source that pressurizes  
the first container to cause transfer of the drug within a selected time.
40. The system of Claim 5 further comprising a metering element that controls a  
volume of the drug being transferred.
41. An injection device comprising:  
25 a housing having a penetrating member aperture,

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a port in said housing that receives a rigid container that contains an injectable drug;

a first penetrating member movable from a storage position in the housing to an injection position extending outside the housing through the aperture; and

a channel that brings said penetrating member into fluid communication with the first container.

42. The injection device of Claim 41 wherein the channel comprises a fluid pathway in a manifold, the manifold further comprising a second channel to transfer the injectable drug from the housing to the user.
43. The injection device of Claim 41 further comprising an actuator that displaces the penetrating member from the storage position to the injection position.
44. The injection device of Claim 43 wherein the actuator includes a plunger mechanism on a first housing surface that displaces said first penetrating member through the aperture on a second housing surface between the storage position and the injection system.
45. The device of Claim 41 further comprising a locking mechanism that prevents displacement of said first penetrating member to said injection position after injection.
46. The injection device of Claim 41 further comprising a biasing mechanism that resiliently biases the penetrating member in said storage position.
47. The injection device of Claim 41 further comprising a penetrating member retraction system that retracts said penetrating member into the housing after injection.

48. The injection device of Claim 41 wherein the penetrating member extends in the range of 5 - 12 millimeters out of said housing in said injection position for a subcutaneous injection.
49. The injection device of Claim 41 wherein the penetrating member extends up  
5 to about 3 cm out of said housing in said injection position for an intermuscular injection.
50. A drug injection device comprising:  
a housing having a port that receives a container of injectable fluid;  
a pressurizing mechanism that pressurizes the container to move the  
10 injectable fluid; and  
a penetrating member movable from a storage position in the housing to an injection position extending outside the housing, the penetrating member being in fluid communication with the container.
51. The device of claim 50 further comprising a sealing member to maintain the  
15 injectable fluid in an upper end of the housing.
52. The device of claim 51 wherein the sealing member further comprises a membrane that is gas impermeable.
53. The device of claim 51 wherein the injection penetrating member includes a  
20 first end to pierce skin of the body being injected and a second end to pierce the sealing member after the first end has penetrated the skin.
54. The device of claim 50 further comprising an actuator that displaces the injection penetrating member between the storage position and the injection position.
55. A method of fluid delivery comprising the steps of:



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providing a housing having a first port that receives a first container of fluid;

inserting the first container in the housing;

pressurizing the fluid in the container; and

5       transferring the fluid from the first container through a channel in the housing.

56.   The method of claim 55 further comprising the steps of:

10       providing a movable member slidable and sealingly positioned within the first port, the movable member fixedly supporting a first penetrating member in fluid communication with the container; and

      collapsing a collapsible volume with the movable member upon insertion of the first container into the first port, the collapsible volume being in sealed communication with the first penetrating member to pressurize the container.

15   57.   The method of claim 55 further comprising a second port in the housing that receives a second container that pressurizes the fluid in the first container as said second container contains a fluid to be transferred into the first container, further comprising the step of pressurizing the first container upon transfer of the fluid.

20   58.   The method of claim 55 further comprising the step of penetrating the container with a first end of a penetrating member on the housing and then coming into fluid communication with the fluid.

59.   The method of claim 55 further comprising providing a gas impermeable membrane along at least a portion of a fluid path in the housing.

25   60.   The method of claim 55 further comprising providing a compressible volume, and compressing the volume to pressurize the container.

61. A fluid injection device comprising:
- a housing having a penetrating member aperture;
  - a first port in said housing that receives a first container that contains a solid compound for injection;
  - 5 a second port in said housing that receives a second container that contains a fluid to be mixed with the solid compound in the first container to form a reconstituted drug to be transferred from the first container;
  - a first channel that provides fluid communication between the first and second containers; and
  - 10 a first penetrating member movable from a storage position in the housing to an injection position extending outside the housing through the aperture, said penetrating member being in fluid communication with the first container.
62. The device of claim 61 wherein the first channel comprises a fluid pathway in a manifold, the manifold further comprising a second channel between the first container and the penetrating member.
63. The device of claim 62 wherein the manifold further comprises an actuator that displaces the penetrating member from the storage position to the injection position, said actuator including a plunger mechanism on a first housing surface that displaces said first penetrating member through the aperture on a second housing surface between the storage position and the injection position.
64. The device of claim 61 further comprising a locking mechanism that prevents displacement of said first penetrating member to said injection position after injection.
65. The device of claim 61 further comprising a locking mechanism that prevents movement of the penetrating member to said injection position before the second container is inserted into the first port.

66. The device of claim 61 further comprising a locking mechanism that prevents movement of said injection penetrating member to the injection position when the first container is not vertically oriented.
- 5 67. The device of claim 63 wherein said actuator includes a handle member pivotally attached to said housing and a bar member connected to a slidable member, said slidable member supporting said first penetrating member and displaced by said handle for moving said first penetrating member between said storage and said injection position.
- 10 68. The device of claim 61 further comprising a mixing device that mixes said fluid with said material, said mixing device comprising:  
a second penetrating member fixed to said housing and that penetrates said second container;  
a third penetrating member fixed to said housing and that penetrates said first container; and  
15 a compression element in the housing that displaces the fluid in the second container.
- 20 69. The device of claim 68 further comprising a sealing element in said second container that displaces the fluid from said second element container through said second penetrating member to said first container upon insertion of said second container into said second port such that the compression element moves the sealing element.
- 25 70. The device of claim 68 further comprising:  
a fourth penetrating member positioned within said housing and that penetrates said first container; and  
a second channel that fluidly connects said first and said fourth penetrating members.

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71. The device of claim 70 further comprising a handle member pivotally attached to said housing and that actuates said fourth penetrating member to penetrate said first container.
- 5 72. The device of claim 61 further comprising a biasing mechanism that resiliently biases said first penetrating member in said storage position.
73. The device of claim 61 further comprising a second and third penetrating member fixed to said housing that penetrates said first and said second containers, respectively, said second and third penetrating members being in fluid communication by a manifold.
- 10 74. The device of claim 61 further comprising a penetrating member retraction system that retracts said first penetrating member into the housing after injection.
75. The device of claim 61 wherein said fluid is transferred into the first container upon insertion of the second container into the second port.
- 15 76. The device of claim 61 wherein the first container comprises a light transmissive vial having a visible surface when connected to the first port.
77. The device of claim 61 wherein said first container is orientated at a perpendicular angle relative to an injection axis of the first penetrating member during injection.
- 20 78. The device of claim 61 wherein a compressed fluid, provided in said first storage container upon insertion of the second container into the second port, is used to inject said injectable fluid.
79. The device of claim 61 wherein said housing is a single integrally molded housing.

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80. The device of claim 61 wherein said first and second containers comprise vials having a two millimeter volume.
81. The device of claim 61 wherein said first penetrating member extends in the range of 5-12 millimeters out of said housing in said injection position for subcutaneous injection.
82. The device of claim 61 wherein said first penetrating member extends up to about 3 cm out of said housing in said injection position for intermuscular injection.
83. The device of claim 61 wherein the solid compound is one of a powdered drug and lyophilized drug.
84. The device of claim 61 further comprising an interlocking mechanism that prevents insertion of said second container before insertion of said first container into the housing.
85. The device of claim 61 wherein the material for injection is a lyophilized drug.
86. A method of transferring a fluid comprising the steps of:  
providing a housing member having an aperture;  
providing a first port in said housing that receives a first container that contains a solid compound for injection;  
inserting a first container in said housing;  
providing a second port in said housing that receives a second container that contains a fluid to be mixed with the solid compound to form a mixed fluid;  
inserting a second container in said housing;  
providing a first channel in fluid communication between the first and second containers;

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providing a second channel in fluid communication with the first container; and  
transferring said fluid through the aperture.

87. The method of claim 86 further comprising the step of actuating transfer with  
5 an actuator on the housing.

88. The method of claim 87 further comprising the step of locking said container in the housing.

89. The method of claim 87, further comprising the steps of:  
providing a first penetrating member fixed to said housing and  
10 configured to penetrate said first container; and  
providing a second penetrating member fixed to said housing and configured to penetrate said second container.

90. The method of claim 86 further comprising the step of forcing the liquid from said second storage container to said first container upon inserting the  
15 second container into the second port such that the liquid is pressurized in the first container.

91. A drug delivery device comprising:  
a housing having a penetrating member aperture;  
a first port in said housing that receives a first vial that contains a first  
20 drug component;  
a second port in said housing that receives a second vial that contains a second drug component to be mixed with said first drug component to form an injectable fluid;  
a manifold that fluidly connects said first and second vials;  
25 an injection penetrating member movable from a first position inside the housing to a second position extending outside the housing through the penetrating member aperture; and

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an actuator which causes the manifold to come into fluid communication with the injection penetrating member.

- 5 92. The device of claim 91 further comprising a locking mechanism that prevents displacement of said injection penetrating member to said second position after a single injection.
93. The device of claim 91 further comprising a biasing mechanism that resiliently biases said injection penetrating member in said first position.
- 10 94. The device of claim 91 further comprising a penetrating member retraction system that retracts said injection penetrating member into the housing after injection.
95. The device of claim 91 wherein said injection penetrating member extends outside of the housing to establish fluid communication with the first vial.
- 15 96. The device of claim 91 wherein said second drug component is transferred under pressure into the first vial upon insertion of the second vial into the second port.
97. The device of claim 91 wherein the first vial comprises glass which is visible during transferring of the second drug component and during injection.
98. The device of claim 91 wherein the injectable fluid in said first vial is pressurized to inject said injectable fluid.
- 20 99. The device of claim 91 wherein the first drug component is a lyophilized drug.
100. A method of transferring a fluid comprising the steps of:  
providing a housing having an aperture;

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providing a first port that receives a first vial that contains a first contents;

providing a second port that receives a second vial that contains a second contents to be mixed with said first contents to form a fluid;

5       providing a manifold fluidly connecting said first and second vials; and

causing the manifold to come into fluid communication with the first vial and the aperture.

101. A drug delivery device comprising:

10       a housing having a penetrating member aperture and a first port that receives a first container that contains an injectable fluid;

a pressurizing mechanism that pressurizes the container; and

15       an injection penetrating member movable from a storage position in the housing to an injection position extending through the penetrating member aperture outside the housing, the injection penetrating member being in fluid communication with the first container.

102. The device of claim 101 wherein the pressurizing mechanism includes:

20       a movable member slidably and sealingly positioned within the first port, said movable member fixedly supporting a first penetrating member in fluid communication with the container; and

a collapsible volume in sealed communication with the first penetrating member and configured to be collapsed by the movable member to pressurize the container.

103. The device of claim 102 further comprising a second port in the housing that

25       receives a second container that contains a fluid to be transferred into the first container, wherein the first container is pressurized upon transfer of the fluid.



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104. The device of claim 102 further comprising a sealing member to maintain the injectable fluid in the fluid container in an upper end of the housing.
105. The device of claim 104 wherein the injection penetrating member includes a first end to pierce skin of the body being injected and a second end to pierce the sealing member after the first end has penetrated the skin.
106. The device of claim 101 further comprising an actuator that displaces the injection penetrating member between the storage position and the injection position.
107. A method of transferring a fluid comprising the steps of:
- 10 providing a housing having an aperture and a first port that receives a first container that contains an injectable fluid;
- pressurizing the fluid in the container; and
- actuating a valve to transfer the fluid through the aperture.
108. The method of claim 107 further comprising the steps of:
- 15 providing a movable member slidable and sealingly positioned within the first port, the movable member fixedly supporting a first member in fluid communication with the container; and
- collapsing a collapsible volume with the movable member upon insertion of the first container into the first port, the collapsible volume being in sealed communication with the aperture to pressurize the container.
109. The method of claim 107 further comprising a second port in the housing that receives a second container that contains a fluid to be transferred into the first container, further comprising the step of pressurizing the first container upon transfer of the fluid.
- 25 110. A liquid drug transfer system comprising:
- a housing;

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a port in said housing that receives a container; and  
a delivery device that can be connected to the housing to receive a  
liquid from the container, the delivery device having a needle.

111. The liquid drug transfer system of Claim 110 wherein the delivery device  
5 includes a syringe.
112. The liquid drug transfer system of Claim 110 further comprising an end of  
delivery indicator.
113. The liquid drug transfer system of claim 112 wherein the end of delivery  
indicator comprises a diaphragm.
- 10 114. The liquid drug transfer system of claim 110 further comprising a  
pressurizing mechanism that pressurizes the container.
115. The liquid drug transfer system of claim 110 further comprising a locking  
mechanism that prevents activation of the pressurizing mechanism before the  
container is inserted in the port.
- 15 116. The liquid transfer system of claim 110 further comprising a locking  
mechanism to secure the container in the housing.
117. The liquid transfer system of claim 110 further comprising a locking  
mechanism to prevent activation of the pressurizing mechanism when the  
device is not vertically oriented.
- 20 118. The liquid transfer system of claim 110 wherein a predetermined volume of a  
liquid drug is delivered using one of an adjustable height of a penetrating  
member that pierces the container of liquid drug, residual volume of liquid  
drug and removing a predetermined volume of liquid drug using the  
detachable delivery device.

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119. The liquid drug transfer system of Claim 110 wherein the delivery device comprises a pen injector.
120. The liquid drug transfer system of Claim 110 wherein the delivery device comprises a detachable housing having a needle having a storage position  
5 within the detachable housing and an operating position that extends through an aperture in the detachable housing.
121. The liquid drug transfer system of Claim 110 wherein the housing further comprises a manifold having a channel through which liquid is transferred from the container to the delivery device.
- 10 122. The liquid drug transfer system of Claim 110 further comprising a second port in the housing that receives a second container having a fluid therein.
123. The liquid drug transfer system of Claim 122 further comprising a manifold in the housing having a first channel that connected the second container with the container and a second channel that connects the container to the  
15 delivery device.
124. A method for transferring a liquid comprising:  
inserting a container in a housing;  
transferring a liquid in the container to a delivery device, the delivery  
device having a penetrating member; and  
20 separating the delivery device from the housing.
125. The method of Claim 124 further comprising providing a delivery device including a syringe.
126. The method of Claim 124 further comprising providing an end of delivery indicator.

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127. The method of Claim 126 wherein the step of providing an end of delivery indicator includes providing a diaphragm.
128. The method of claim 124 further comprising actuating a pressurizing mechanism that pressurizes the container.
- 5 129. The method of claim 128 further comprising using a locking mechanism that prevents activation of the pressurizing mechanism before the container is inserted in the port.
130. The method of claim 124 further comprising providing a locking mechanism to secure the container in the housing.
- 10 131. The method of claim 124 further comprising providing a locking mechanism to prevent activation of the pressurizing mechanism when the device is not vertically oriented.
132. The method of claim 124 further comprising transferring predetermined volume of a liquid is delivered using one of an adjustable height of a penetrating member that pierces the container of liquid, adjusting a residual volume of liquid and removing a predetermined volume of liquid using the detachable delivery device.
- 15
133. The method of Claim 124 further comprising providing a manifold in the housing having a first channel that connects the container to the delivery device.
- 20
134. The method of Claim 124 further comprising providing a second container that is inserted in the second port of the housing.

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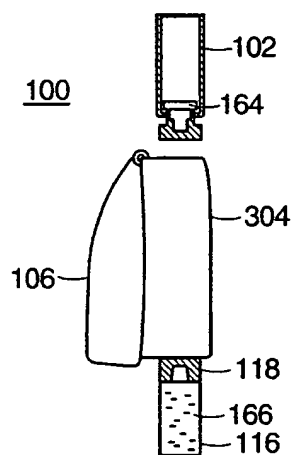


Figure 1A

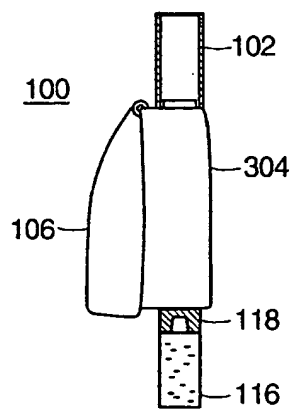


Figure 1B

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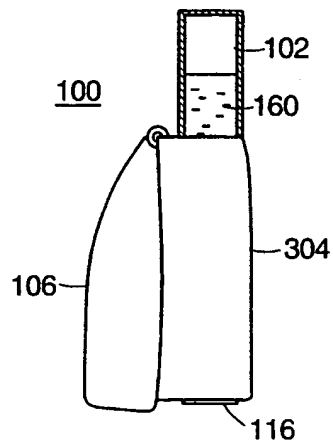


Figure 1C

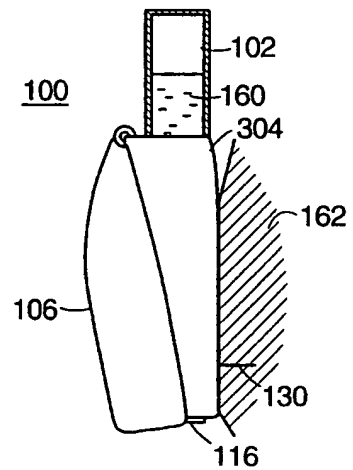


Figure 1D

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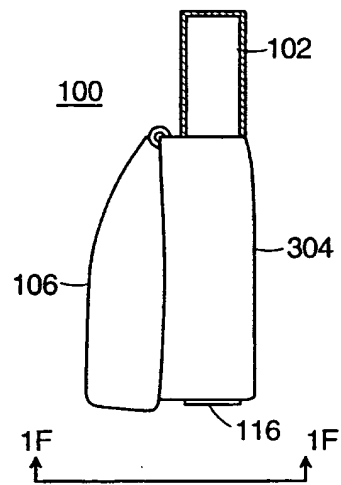


Figure 1E

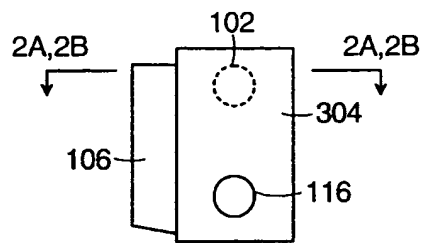


Figure 1F

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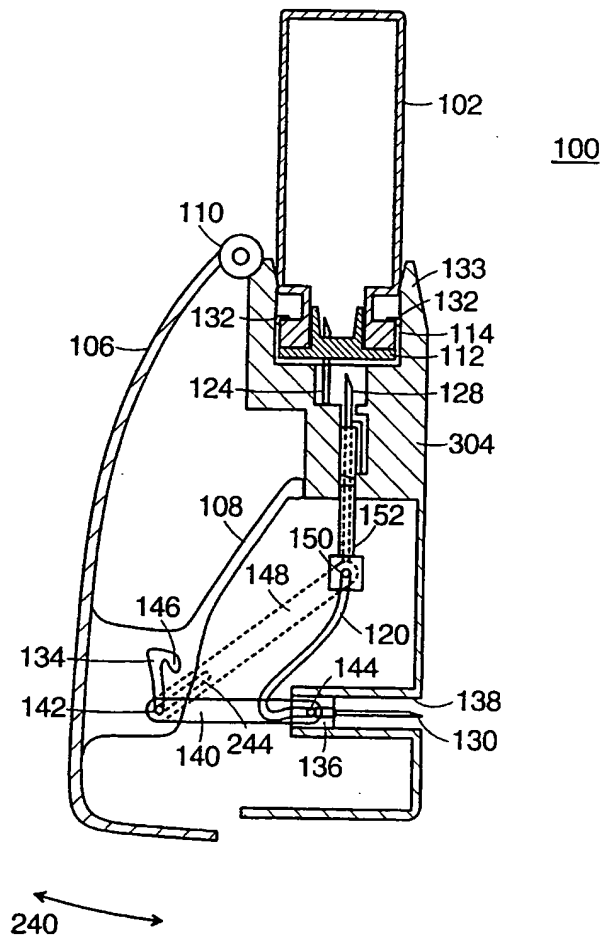


Figure 2A



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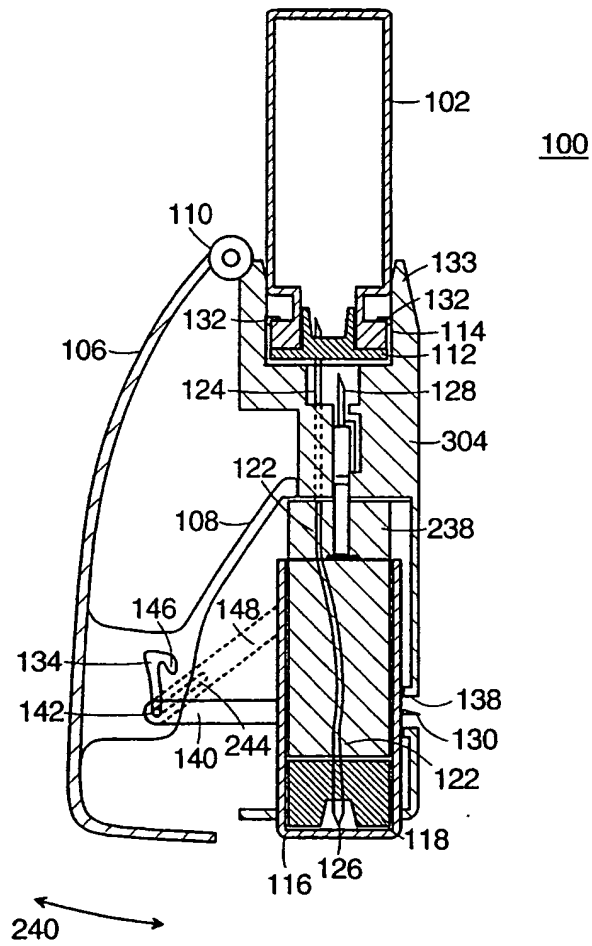


Figure 2B

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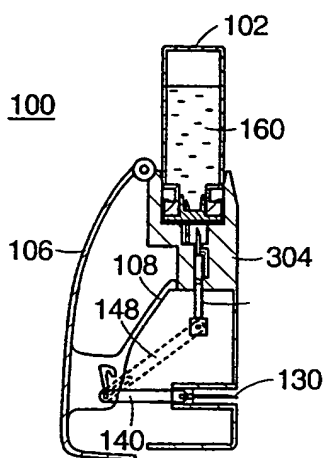


Figure 3A

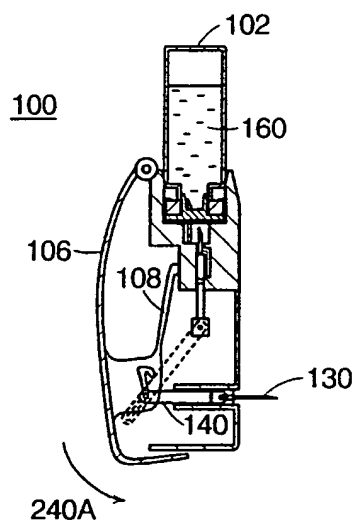


Figure 3B

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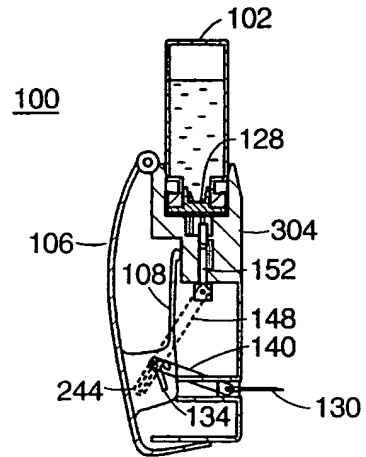


Figure 3C

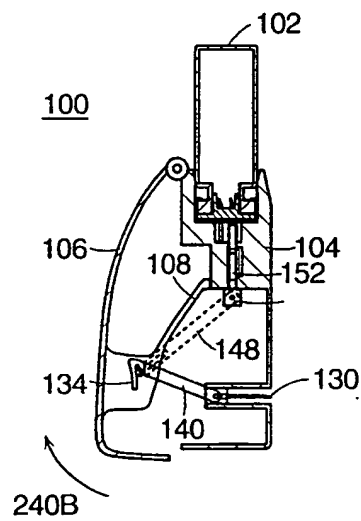


Figure 3D

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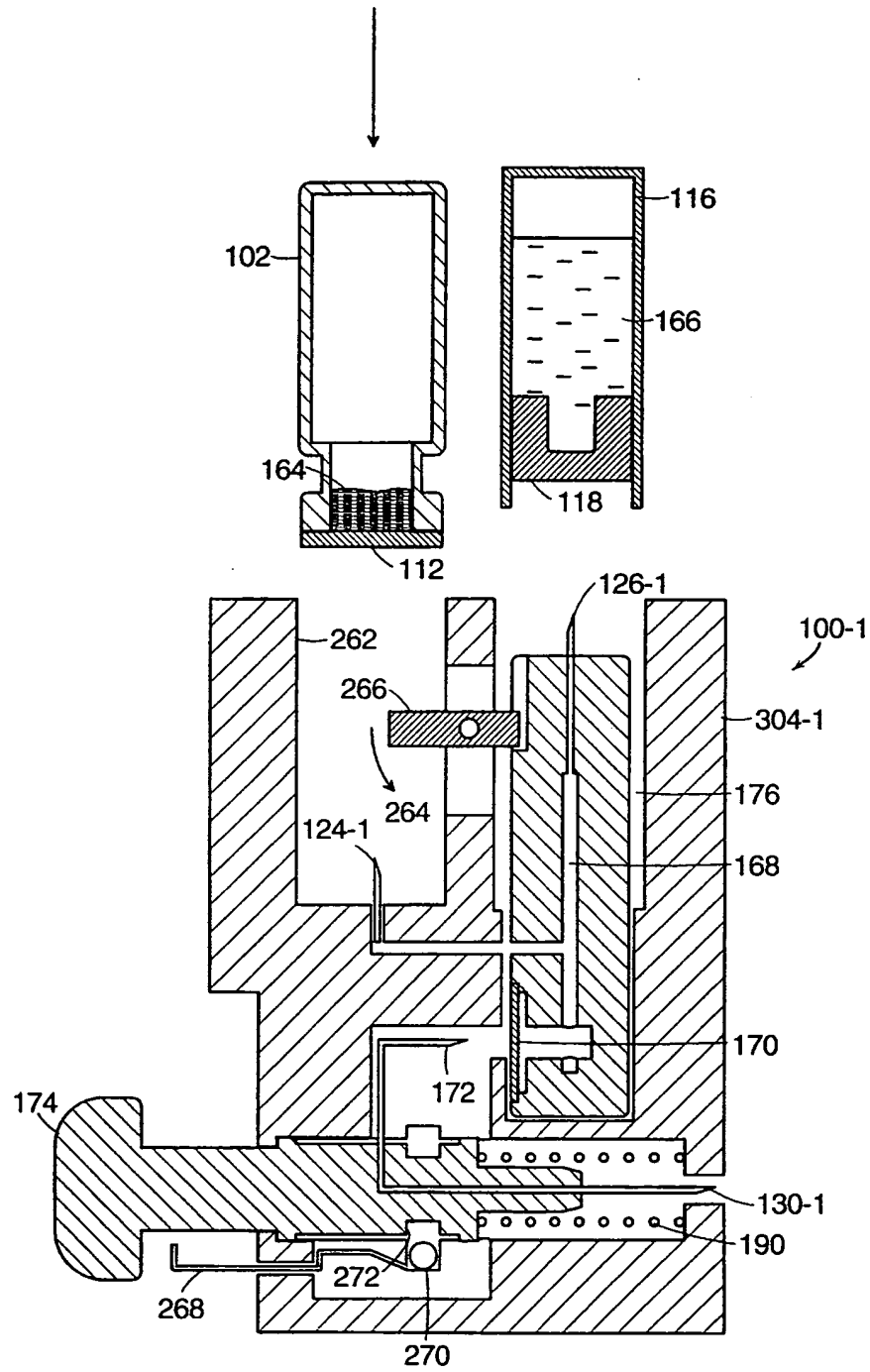


Figure 4A

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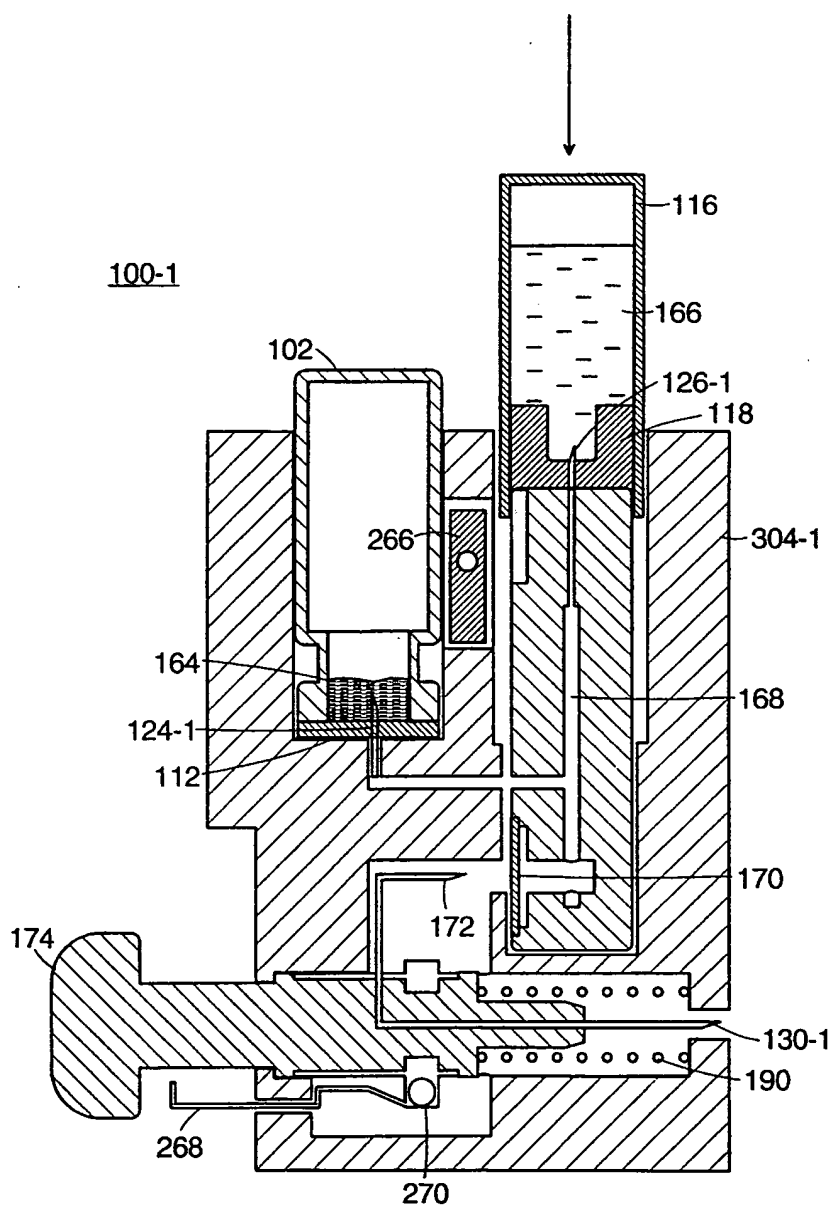
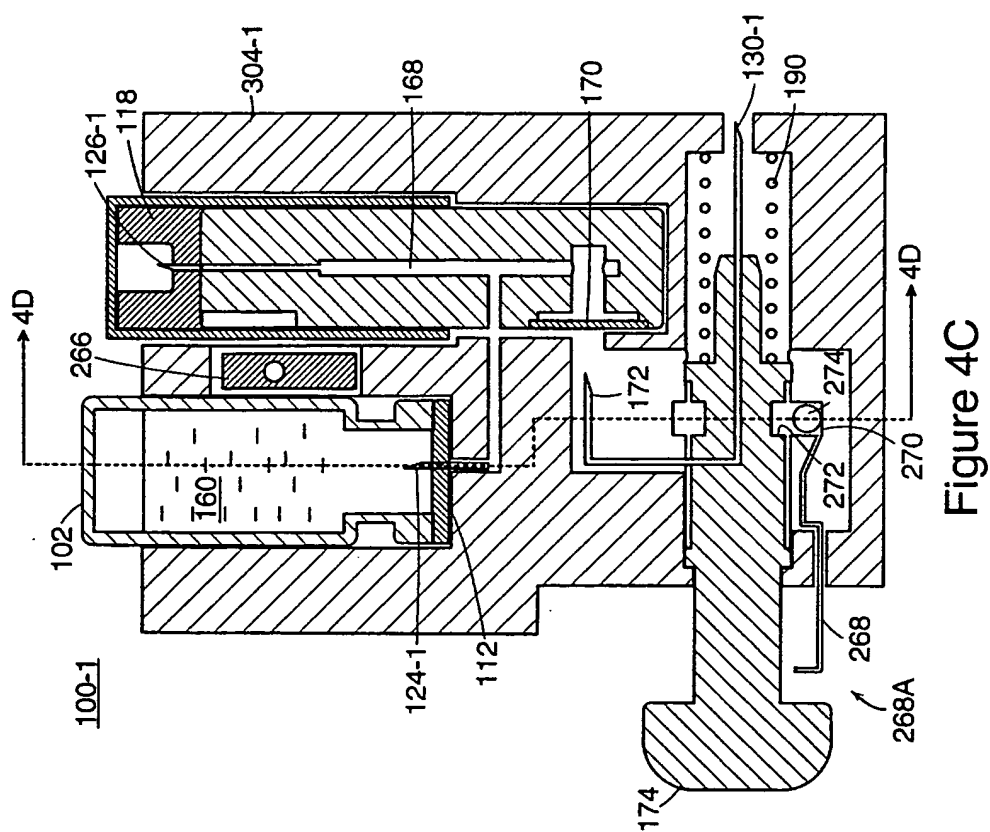
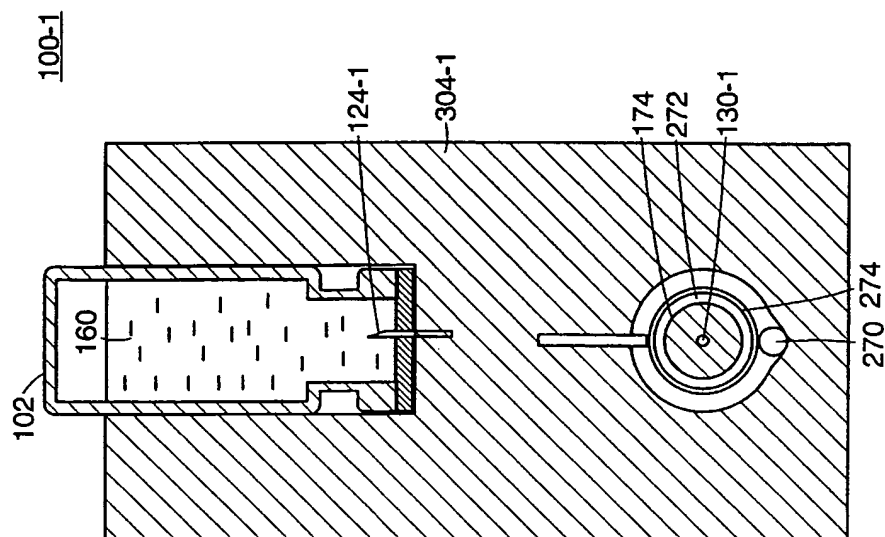


Figure 4B

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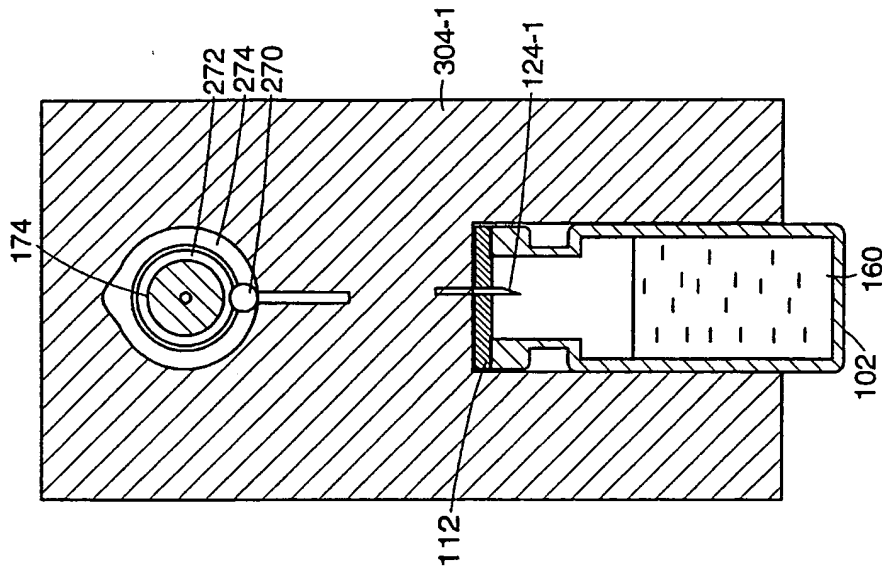


Figure 4F

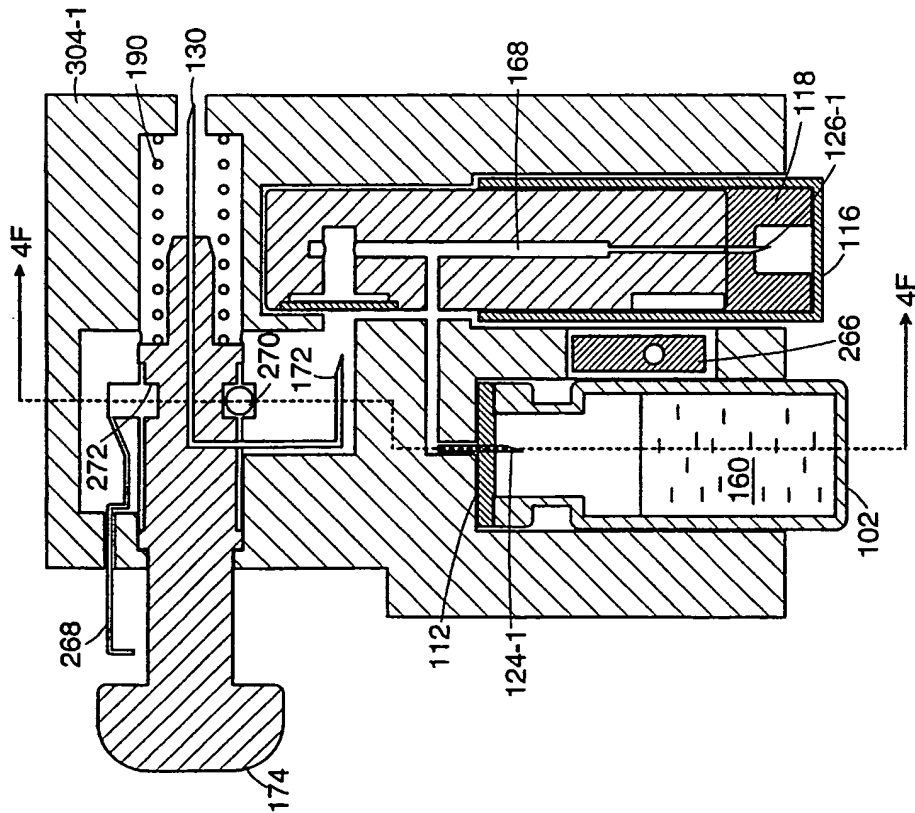


Figure 4E

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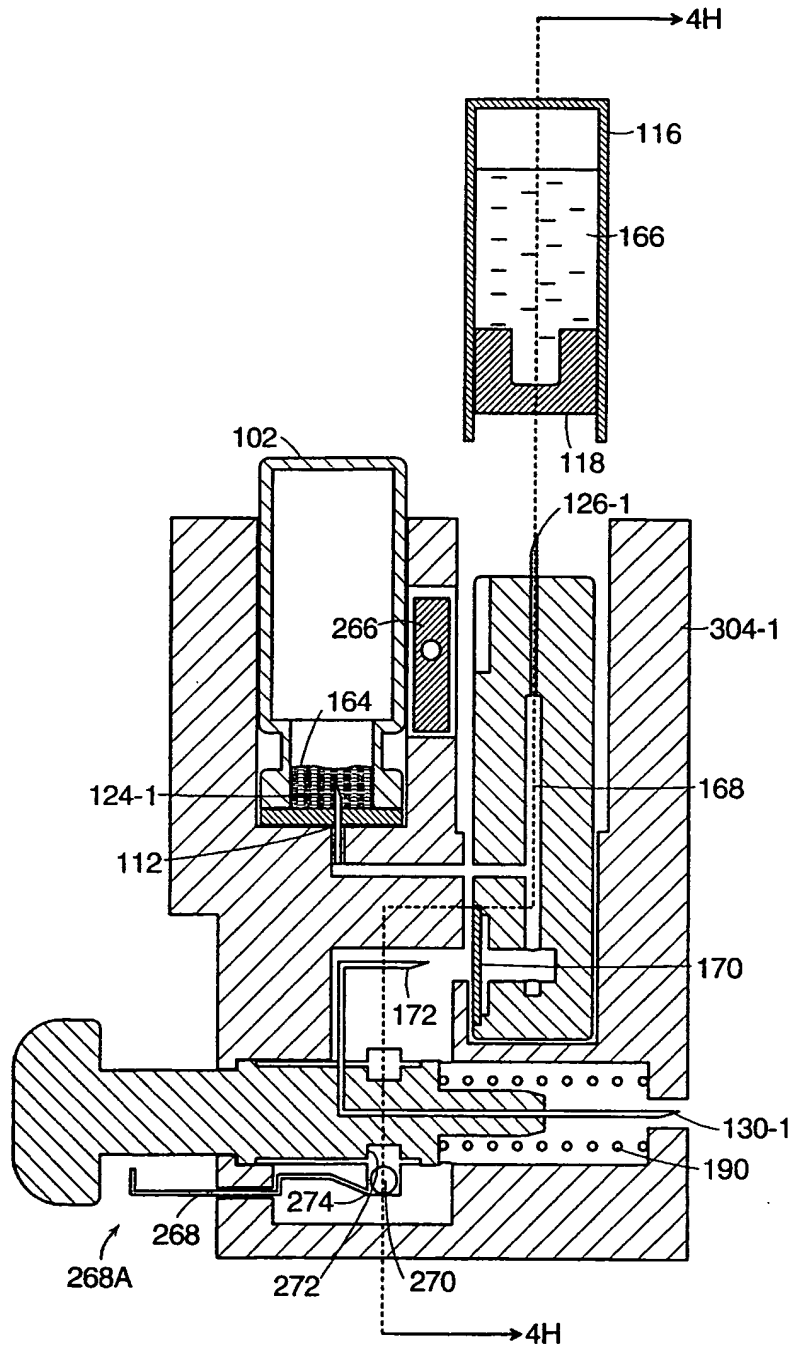


Figure 4G



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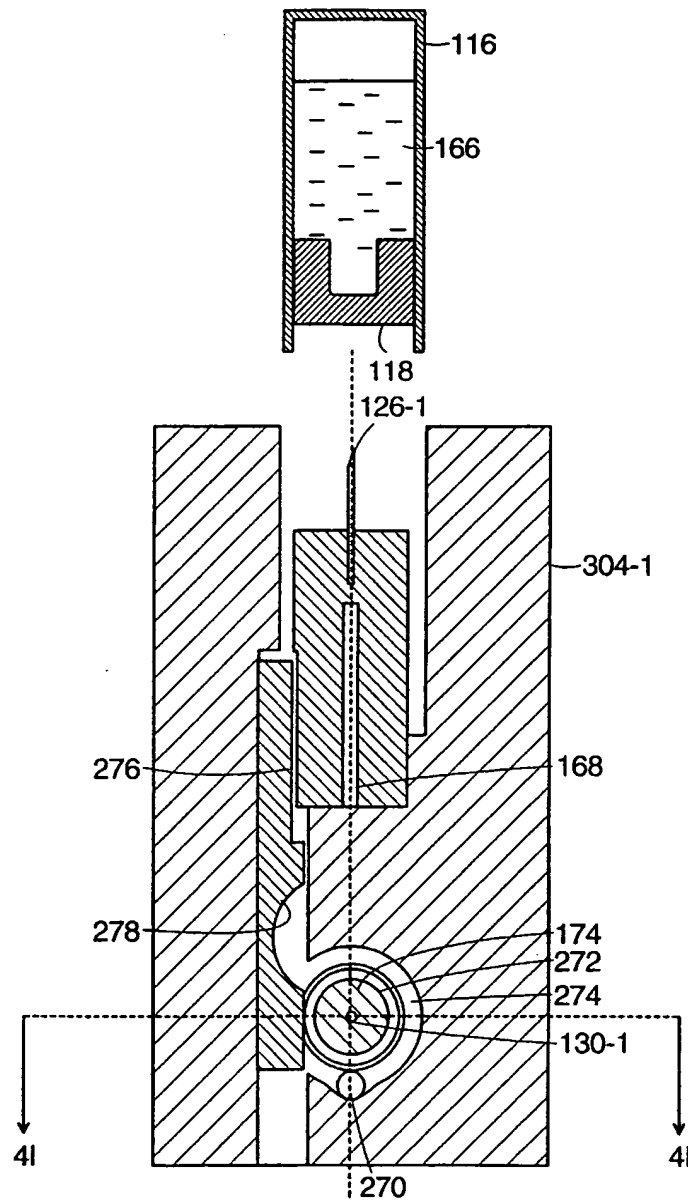


Figure 4H

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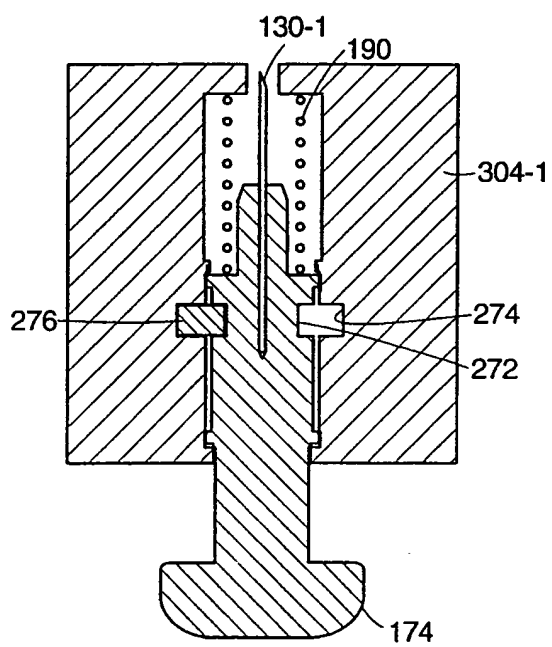


Figure 4I

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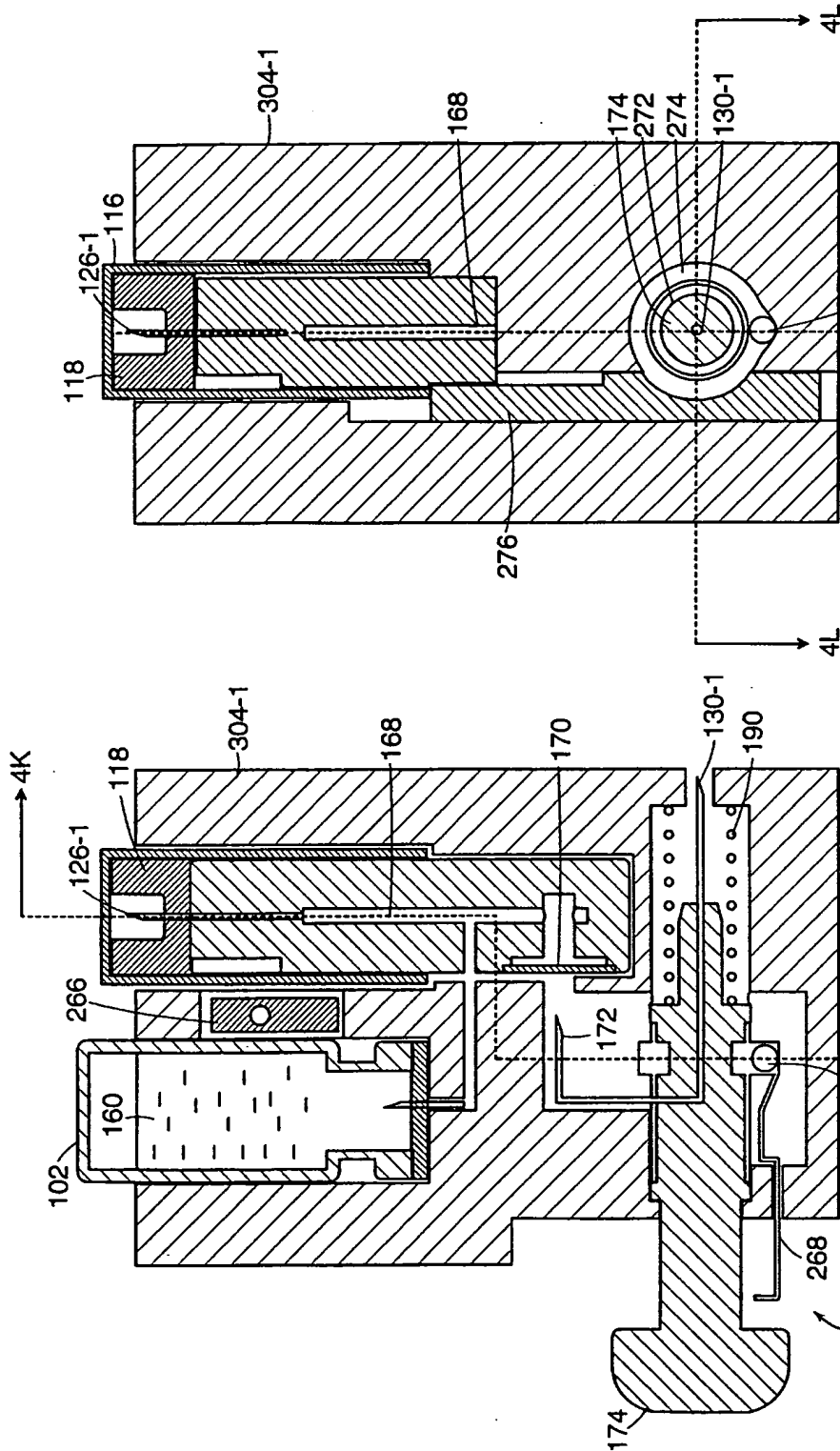


Figure 4K

Figure 4J

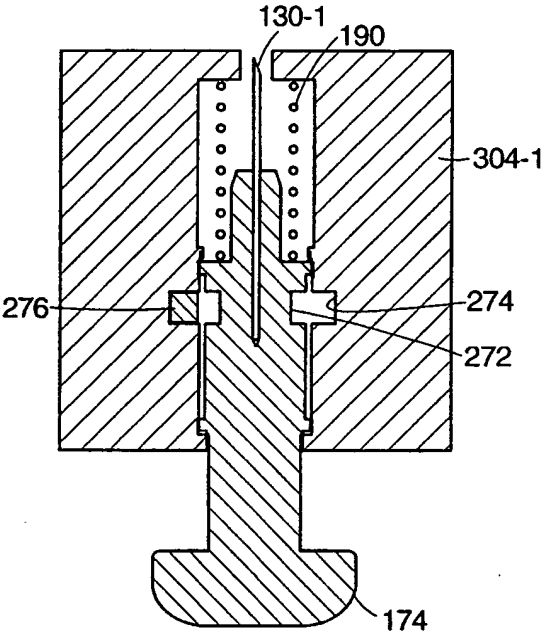


Figure 4L

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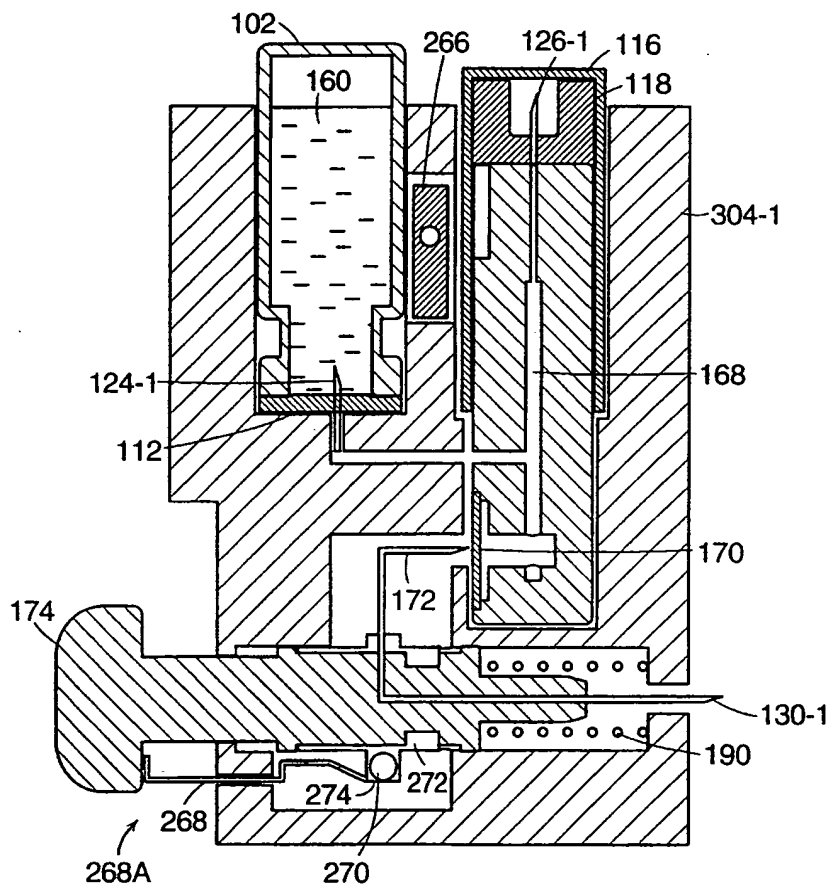


Figure 4M

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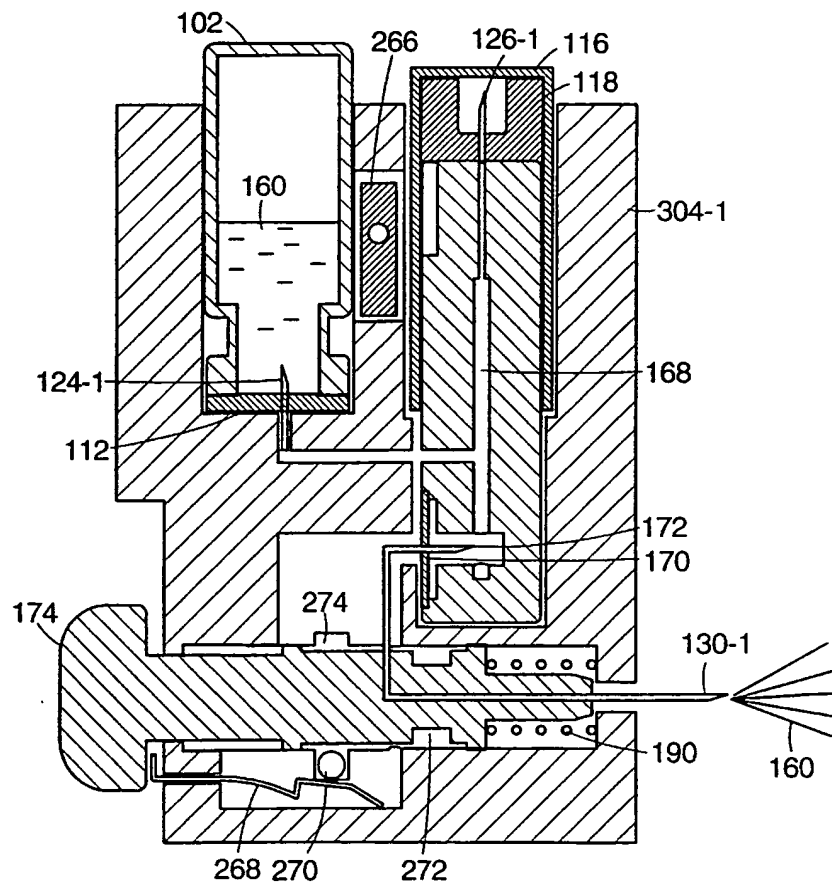


Figure 4N

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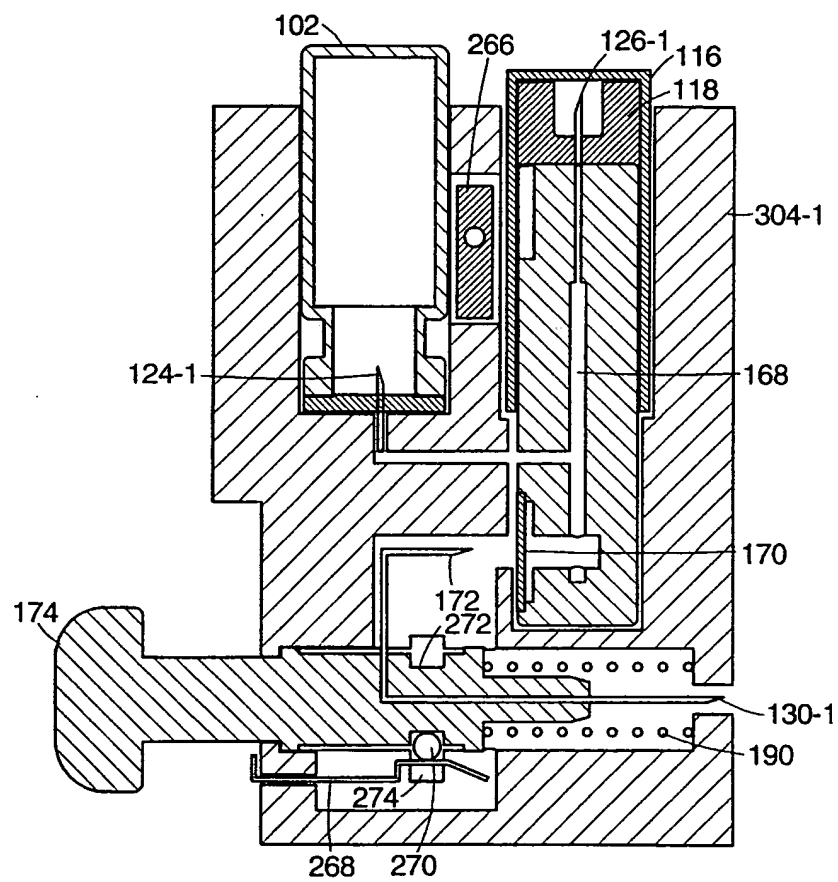


Figure 40

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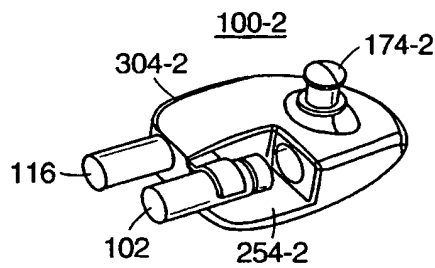


Figure 5A

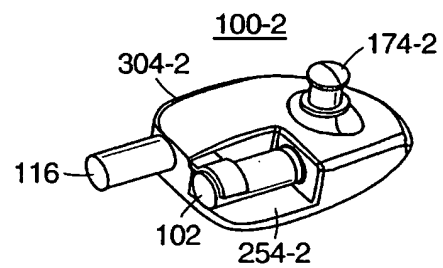


Figure 5B

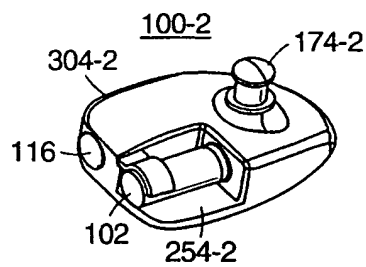


Figure 5C



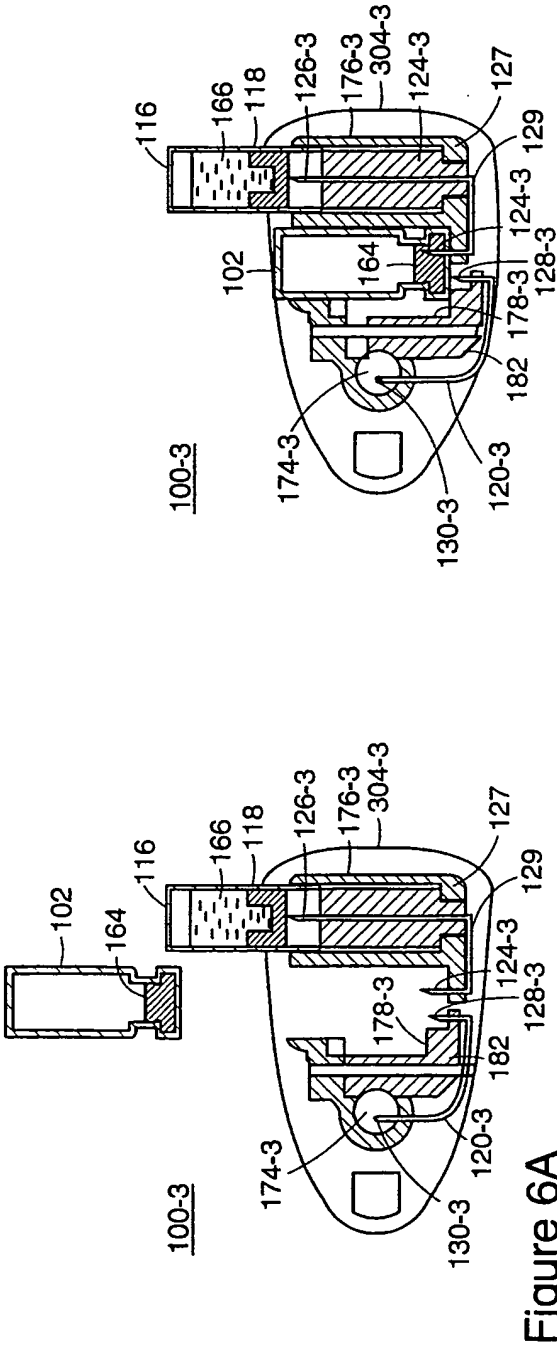


Figure 6A

Figure 6B

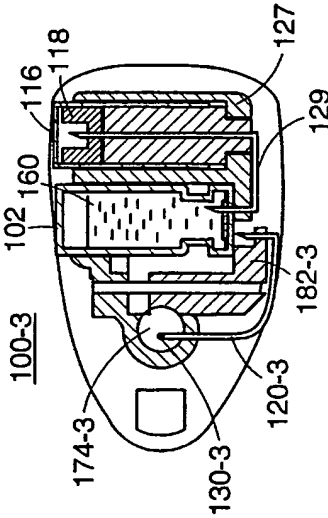


Figure 6C

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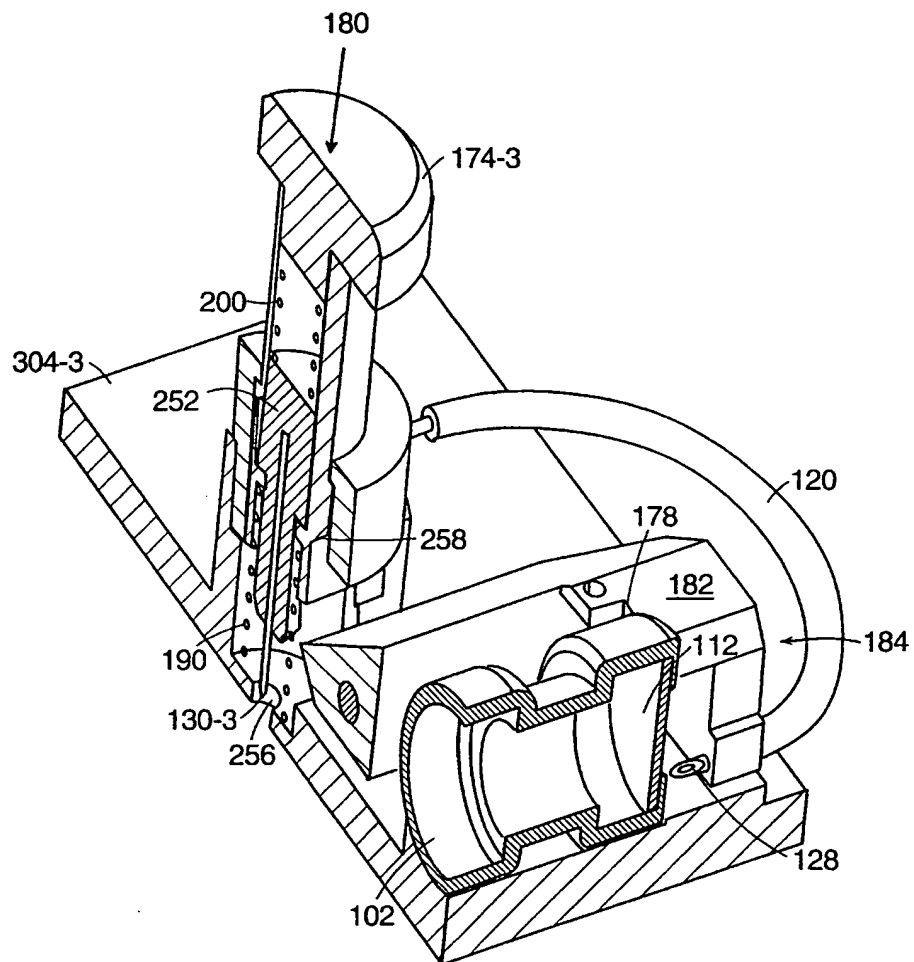


Figure 7A

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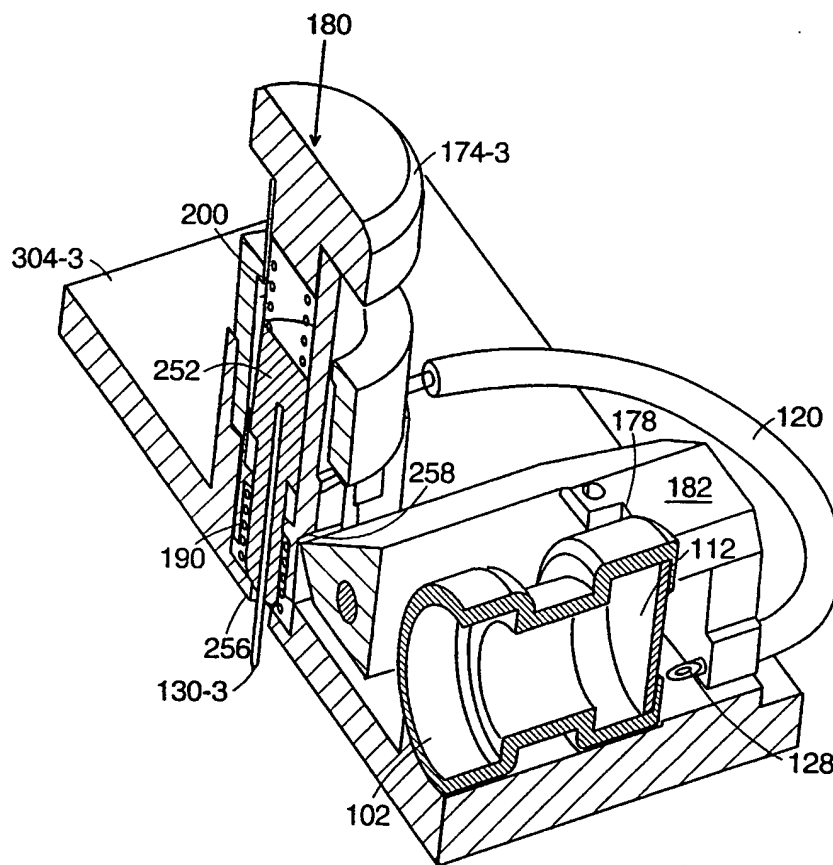


Figure 7B



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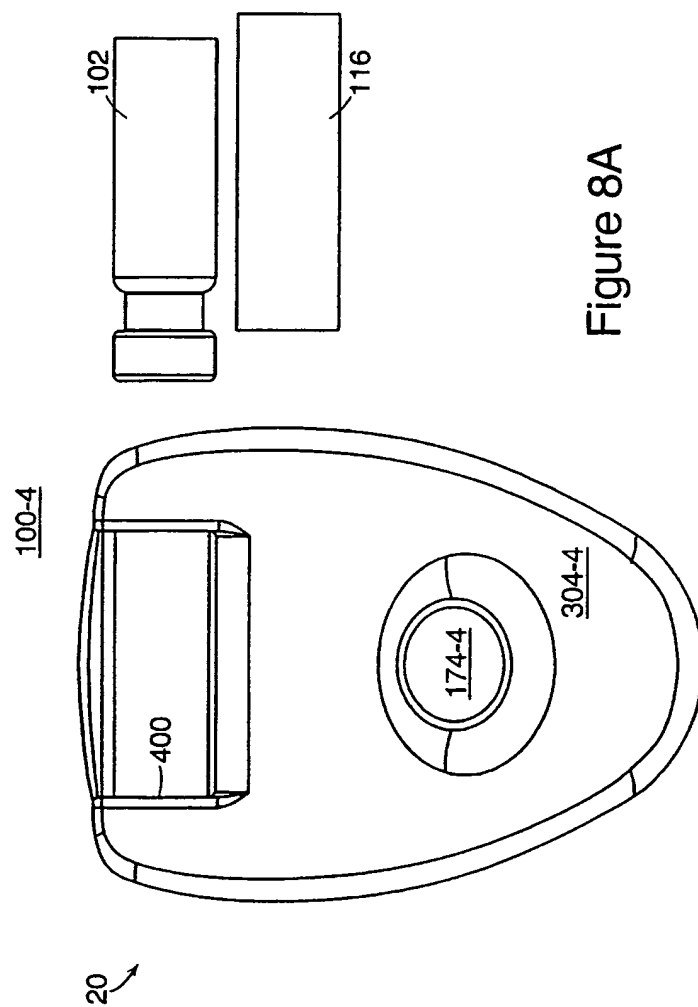


Figure 8A

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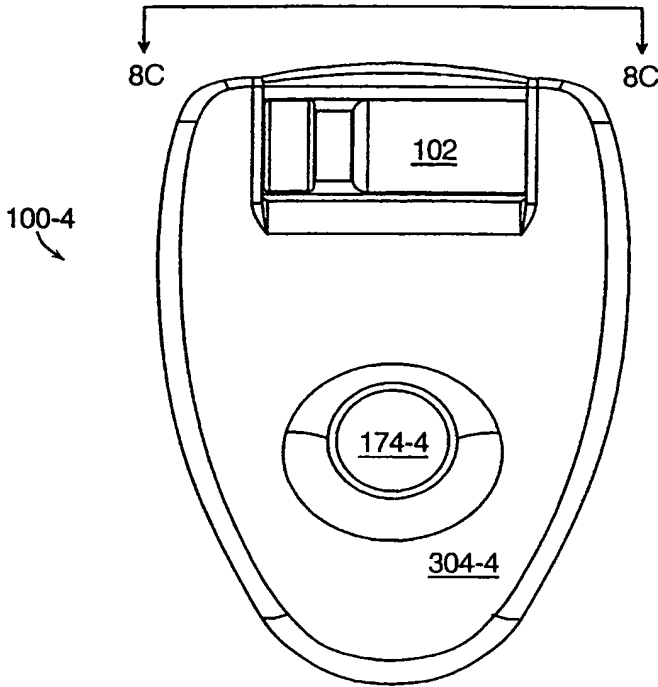


Figure 8B

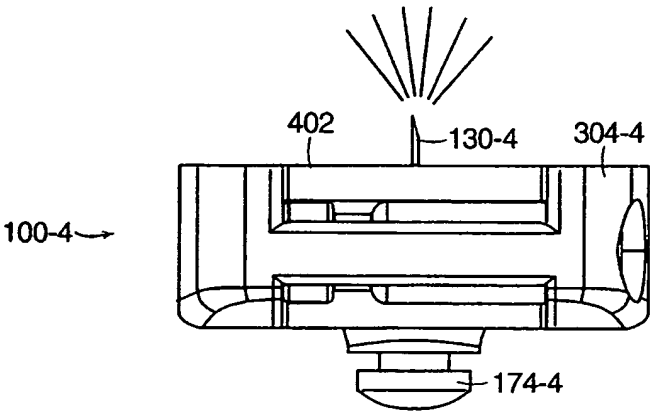


Figure 8C

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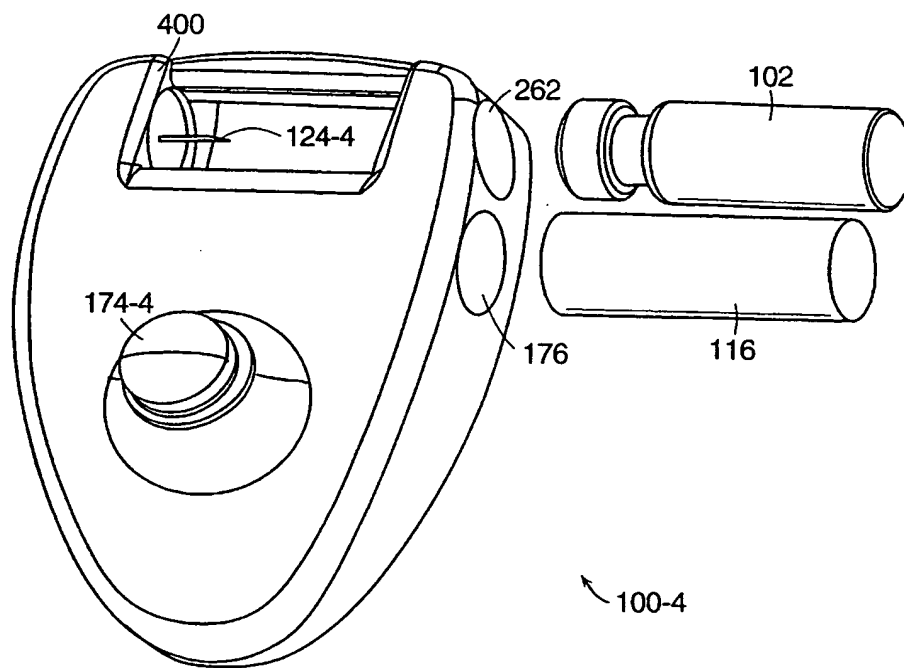


Figure 8D

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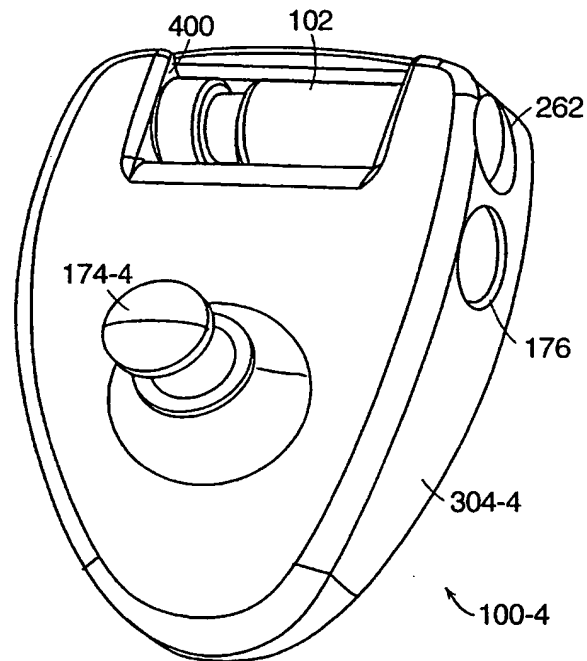


Figure 8E



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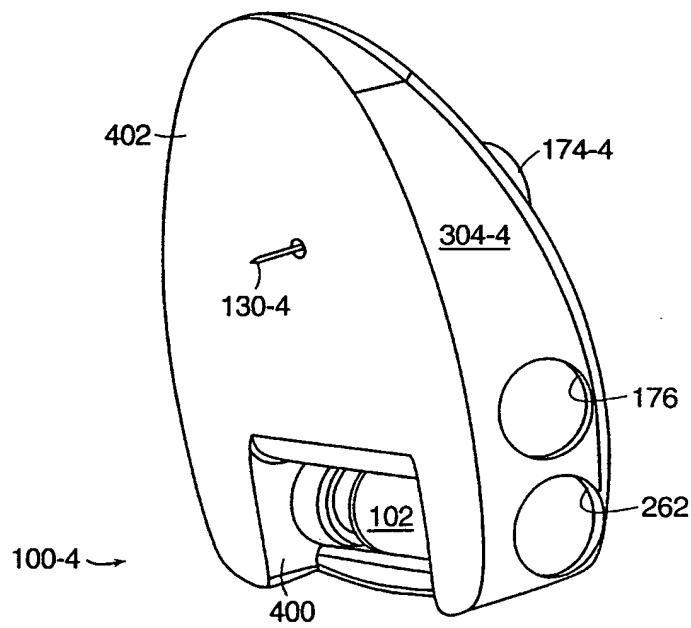


Figure 8F

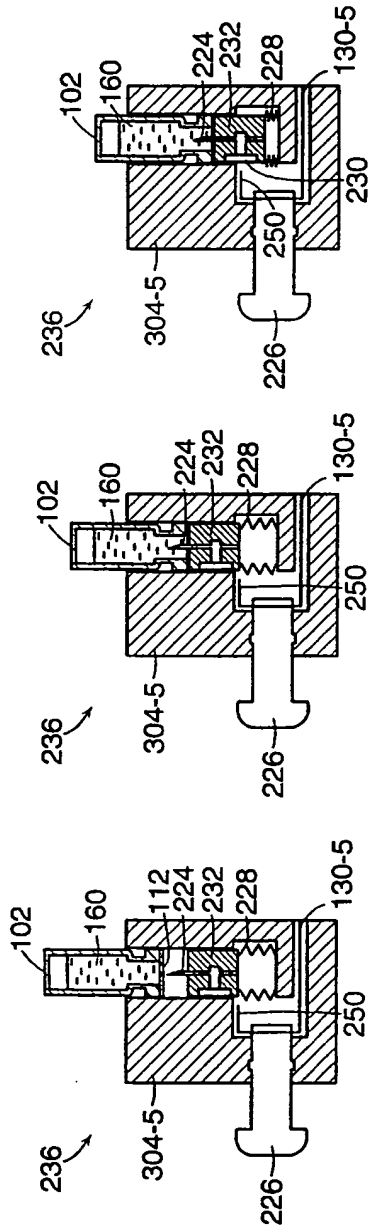


Figure 9A

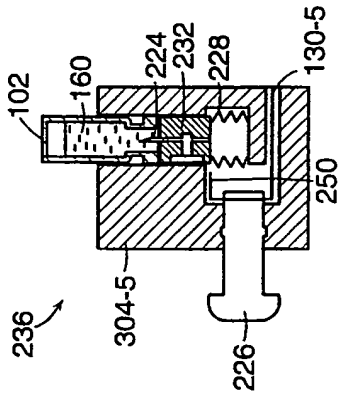


Figure 9B

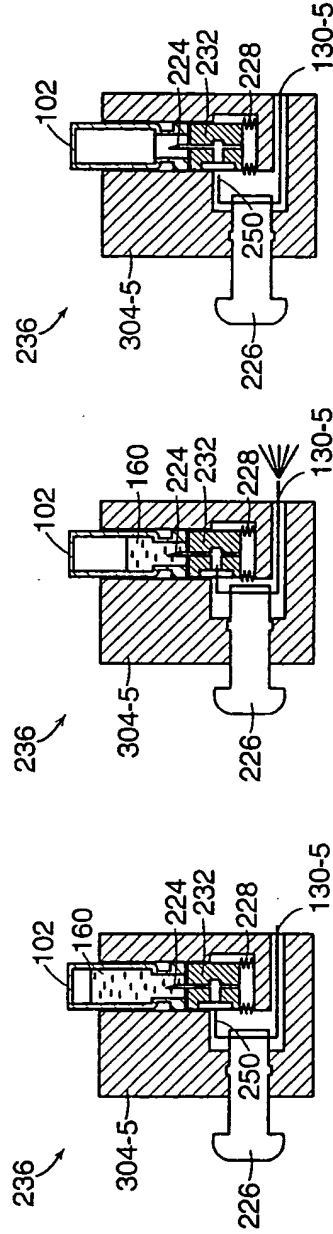


Figure 9C

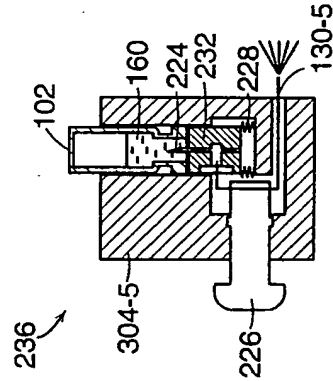


Figure 9D

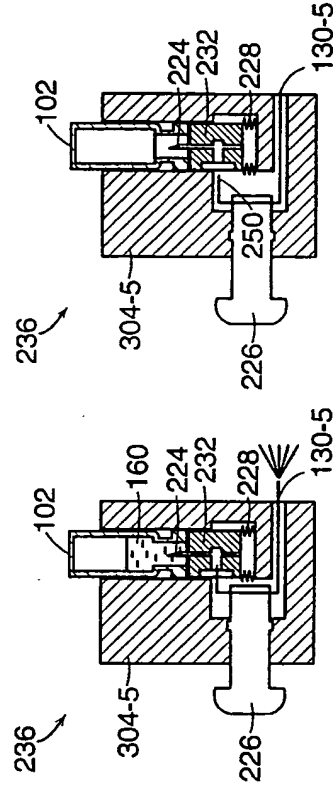


Figure 9E

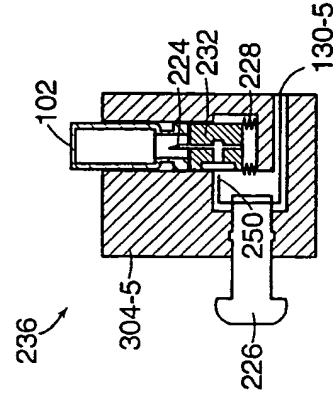


Figure 9F

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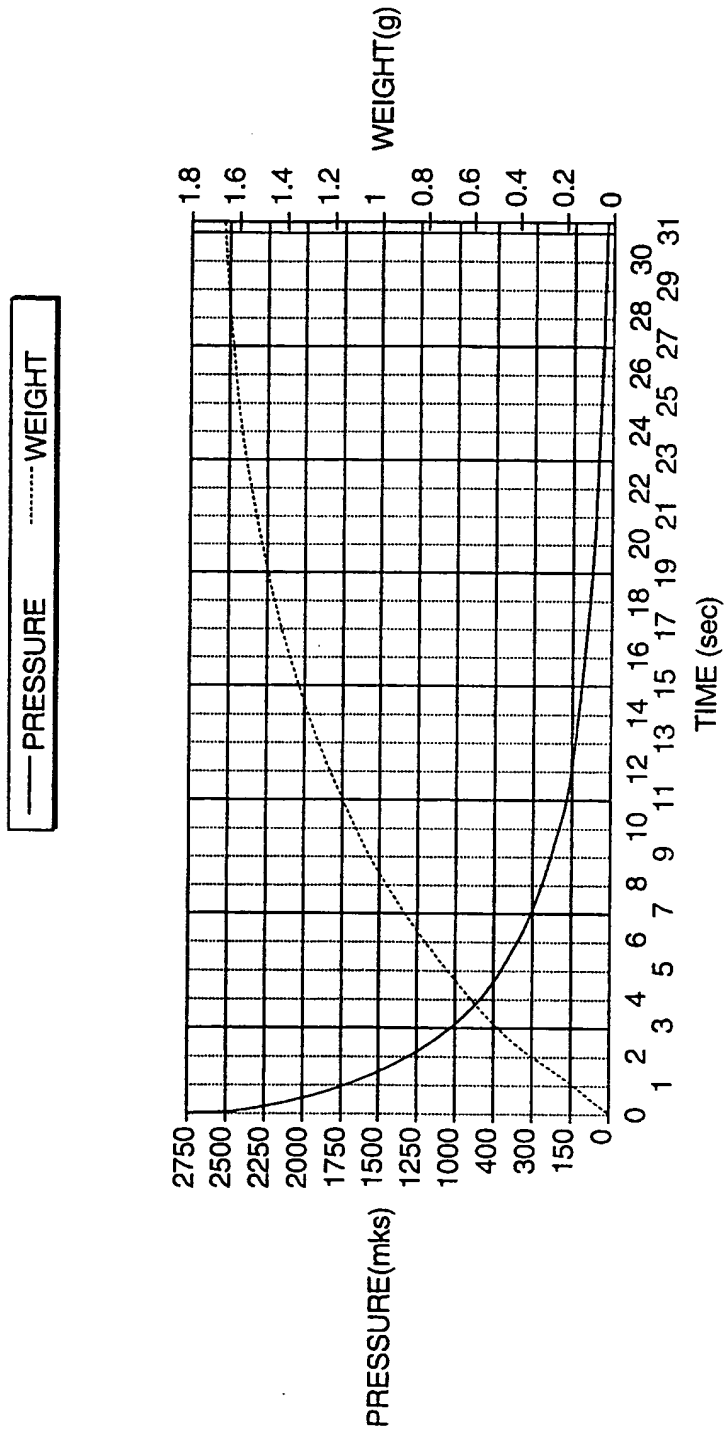


Figure 10A

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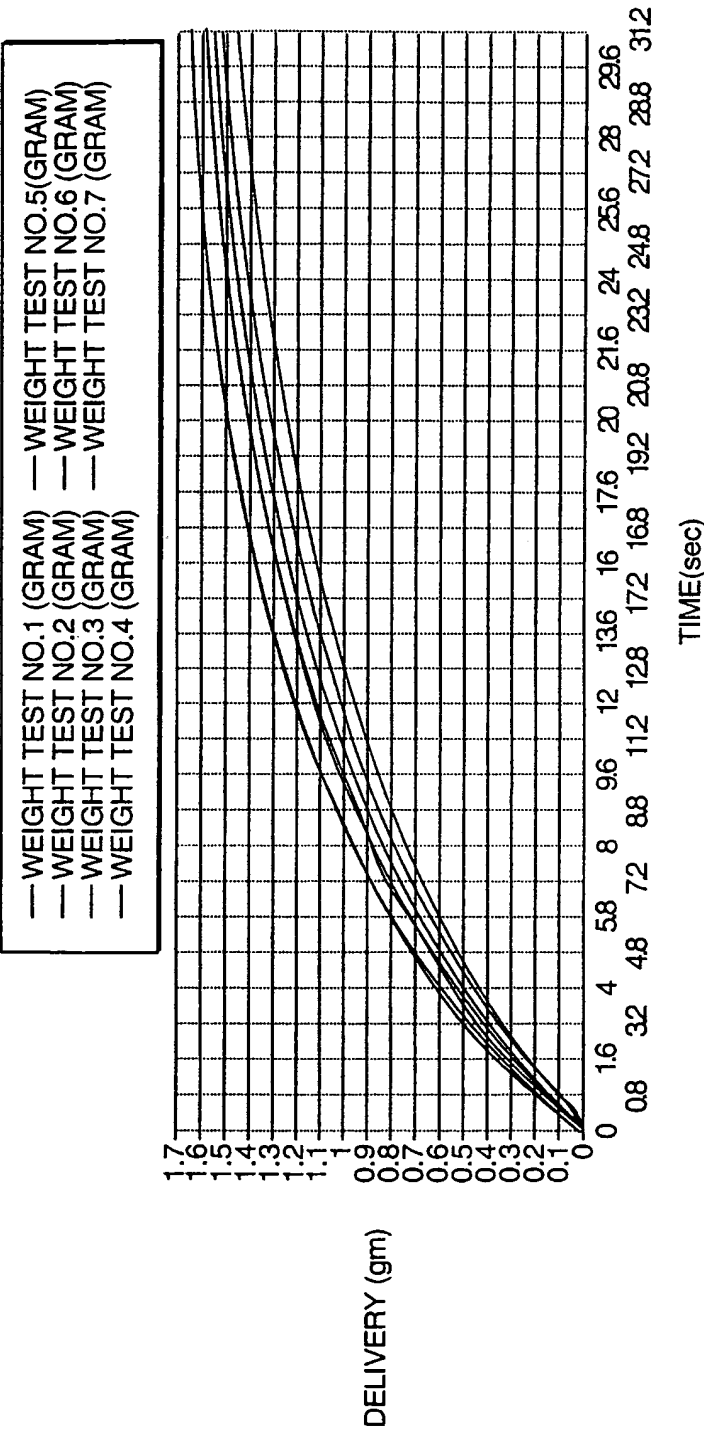


Figure 10B

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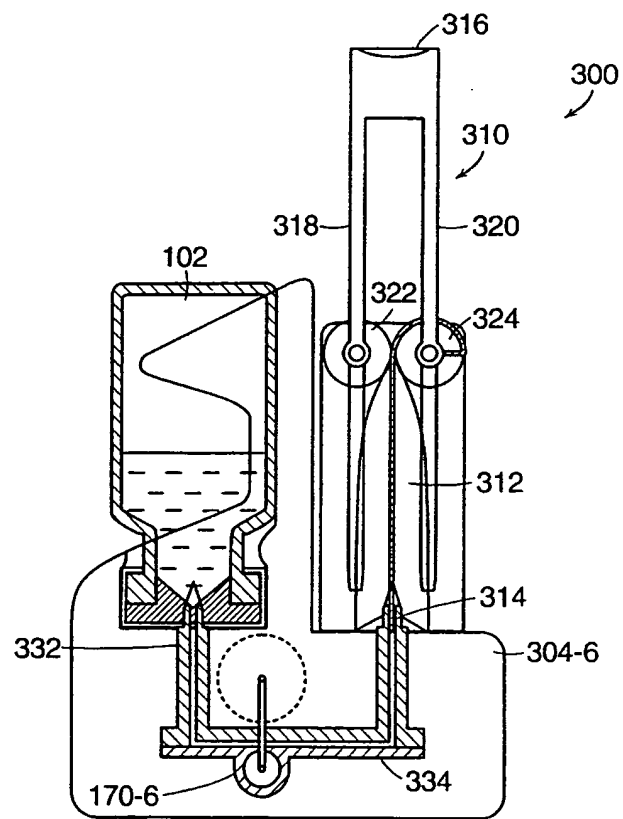


Figure 11A

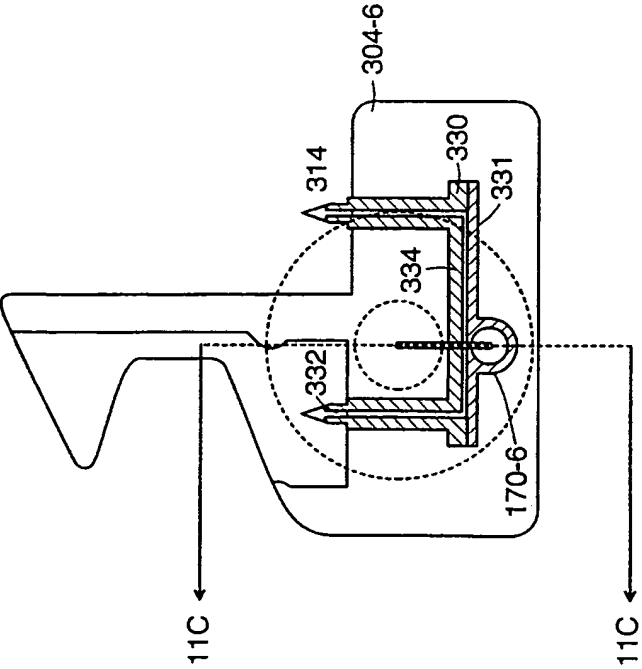


Figure 11B

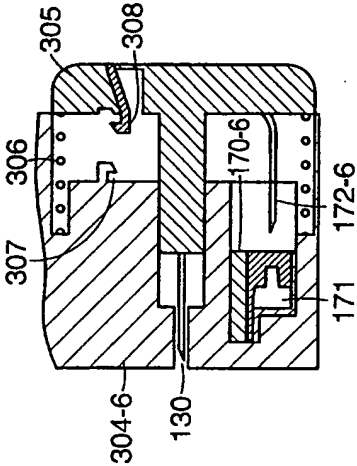


Figure 11C

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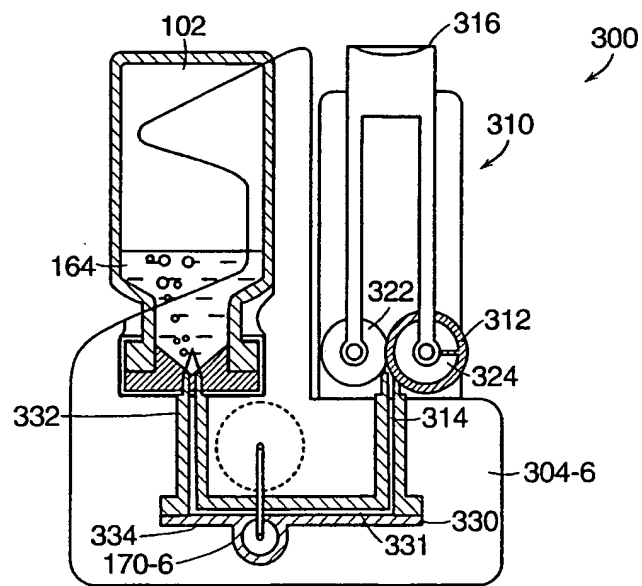


Figure 11D

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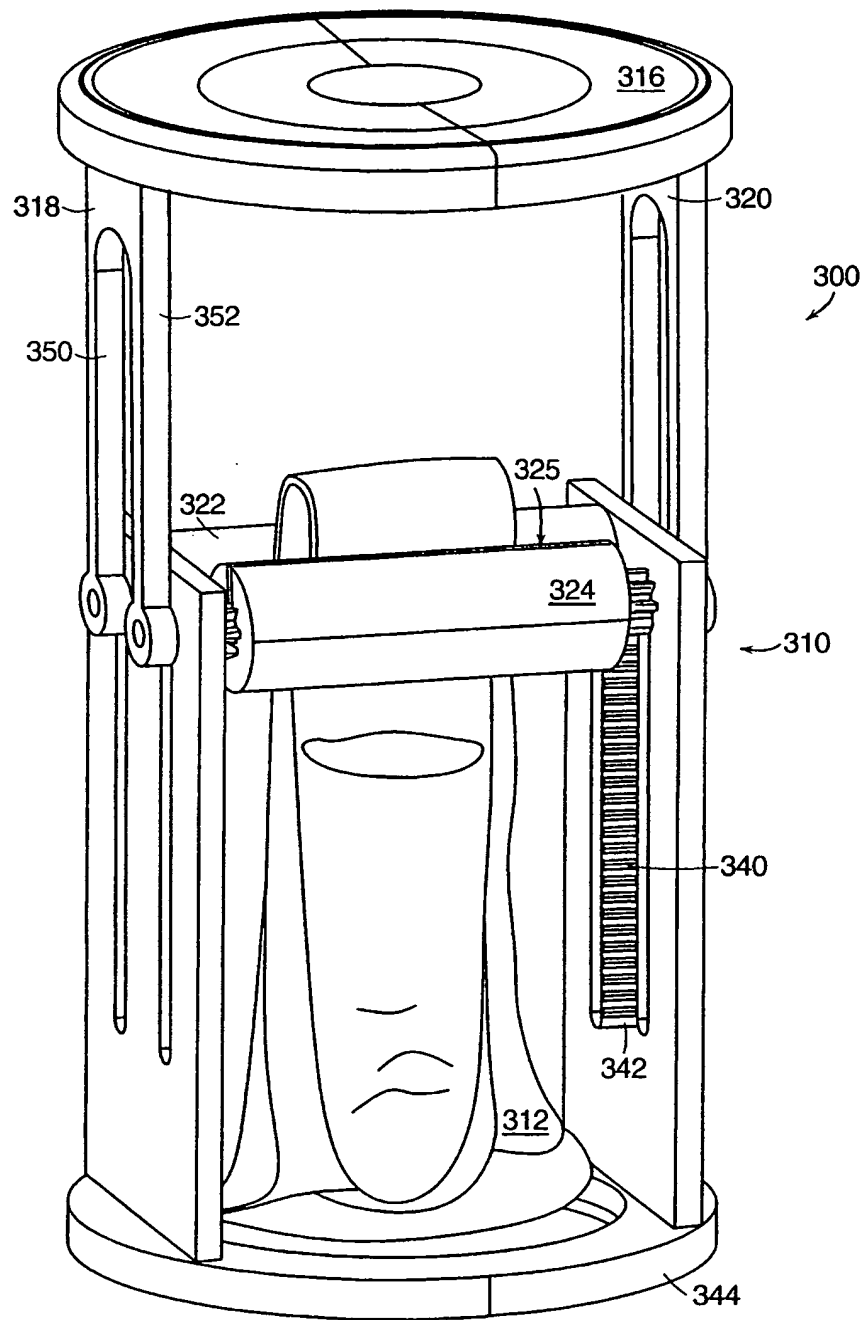


Figure 12A



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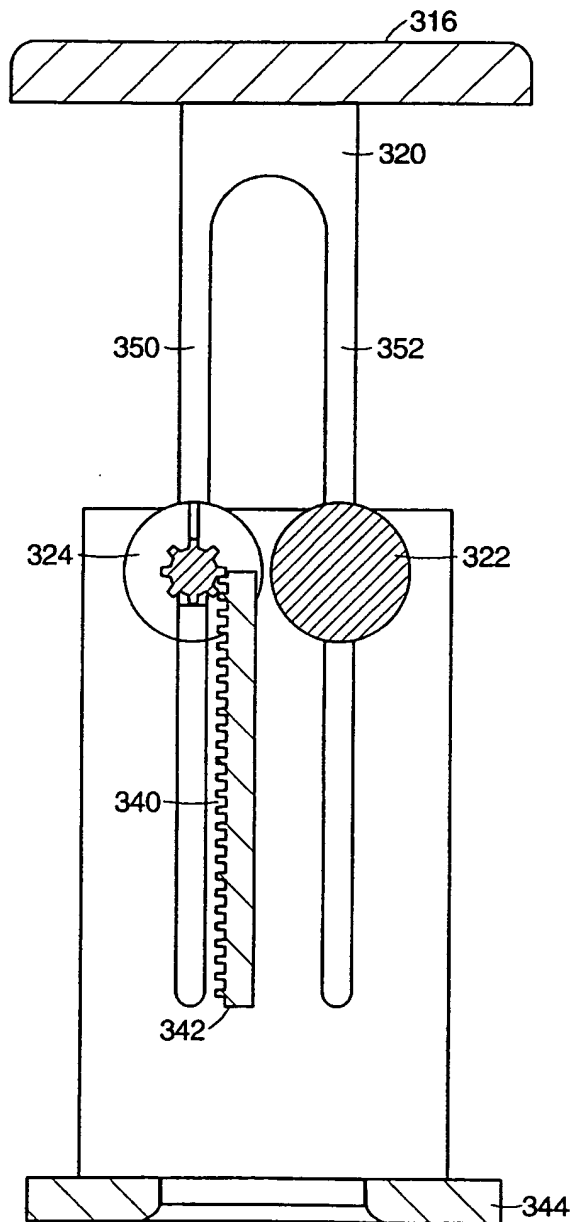
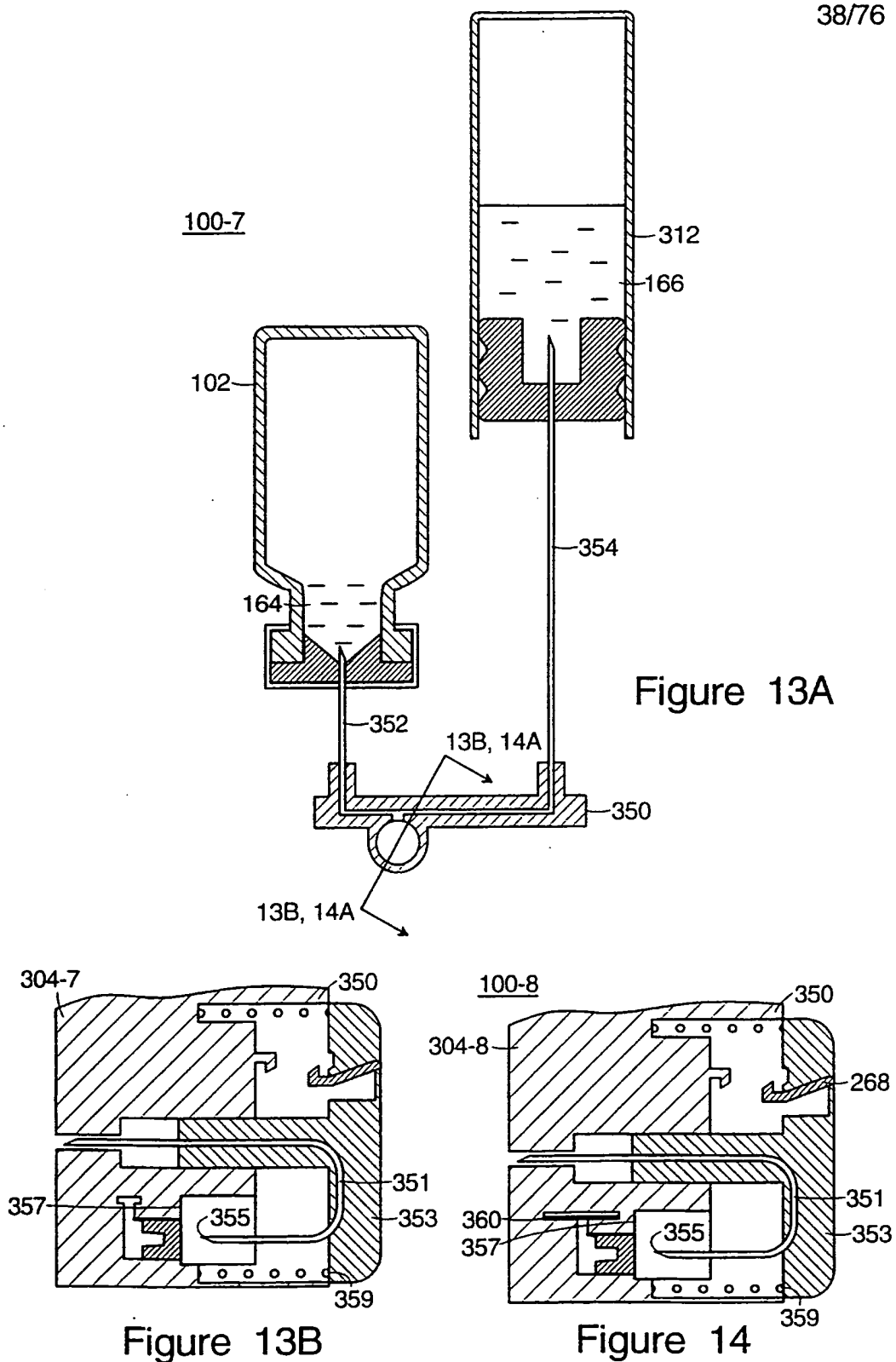


Figure 12B



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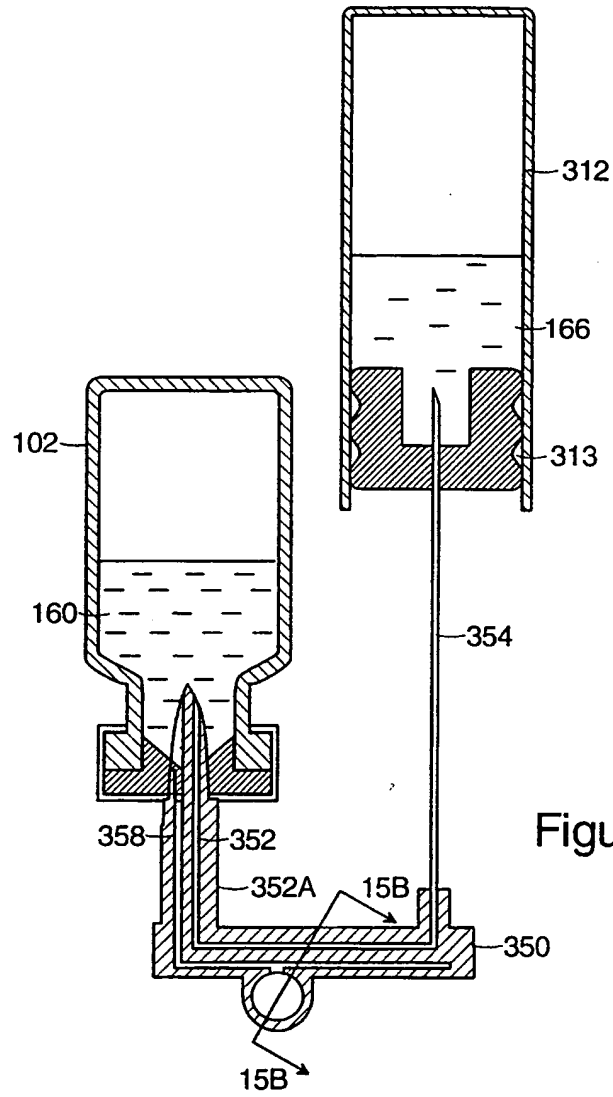


Figure 15A

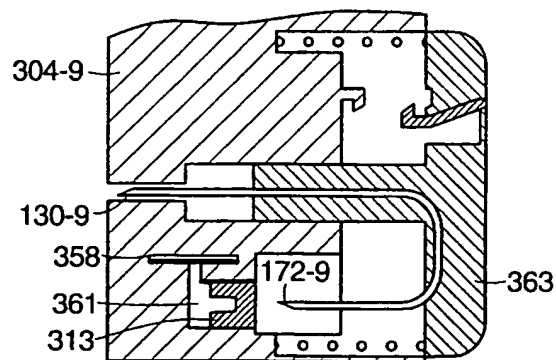


Figure 15B

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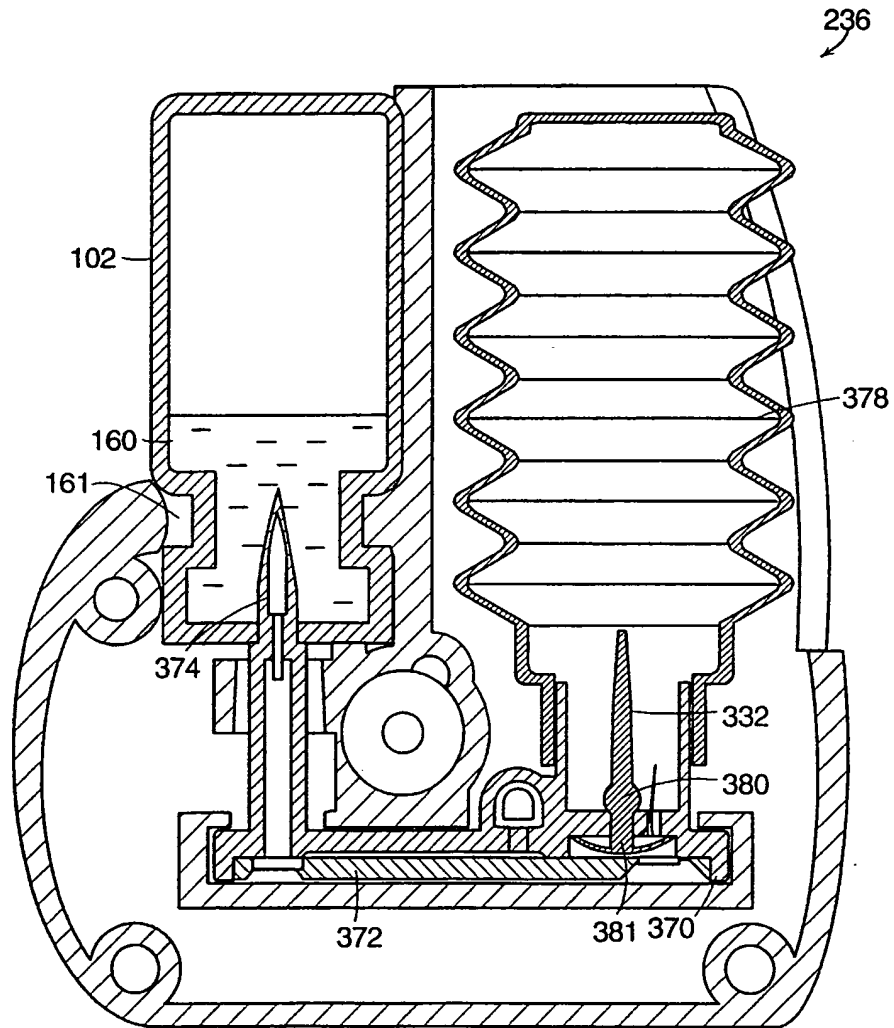


Figure 16

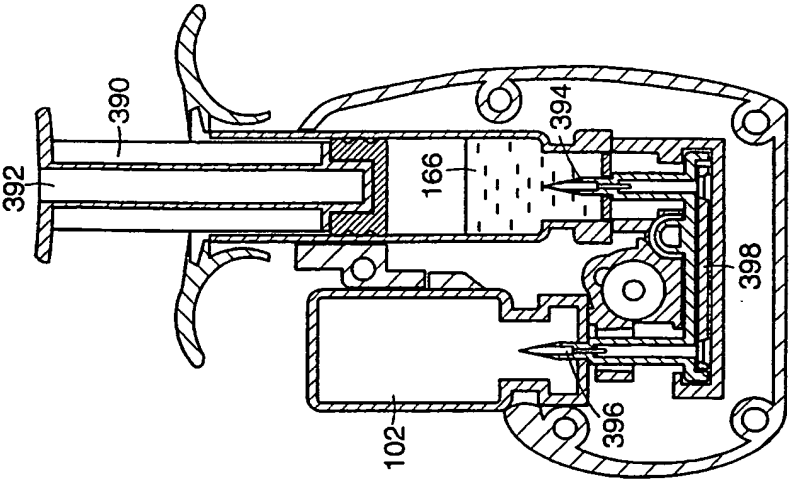


Figure 17A

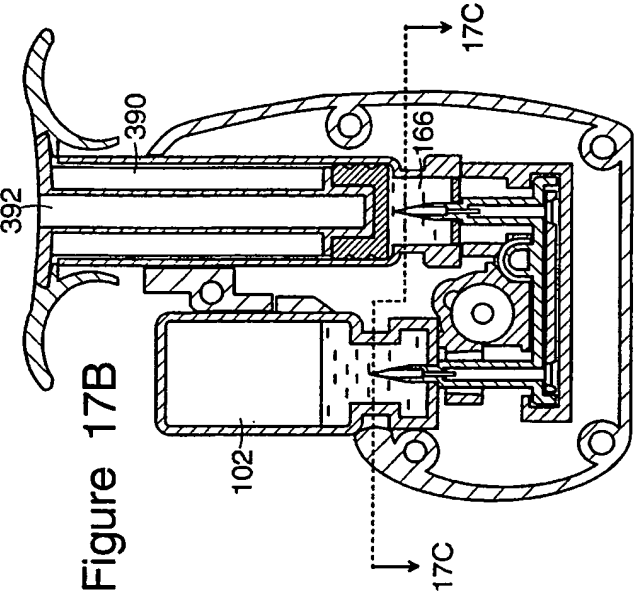


Figure 17B

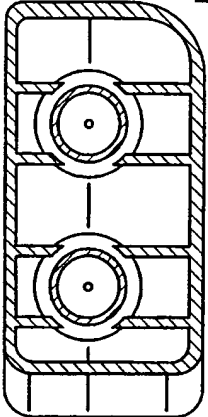


Figure 17C

Figure 18B-1

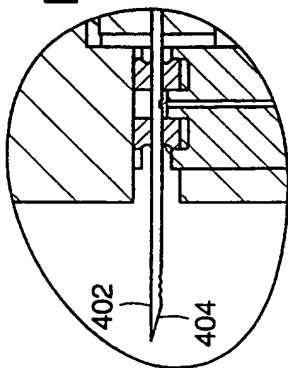
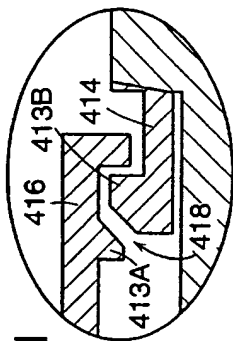


Figure 18A-1



400

400

400

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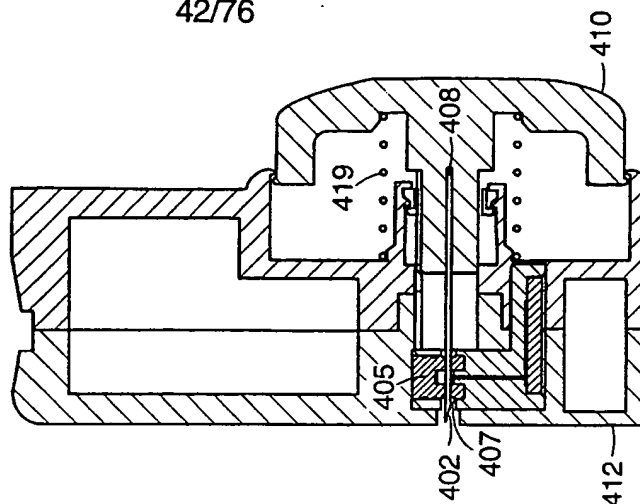


Figure 18C

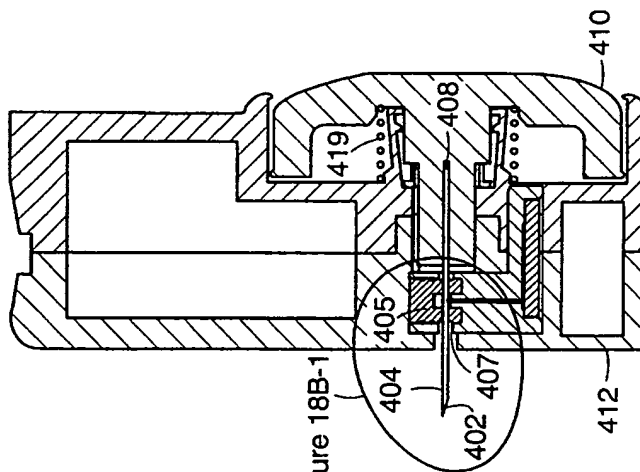


Figure 18B

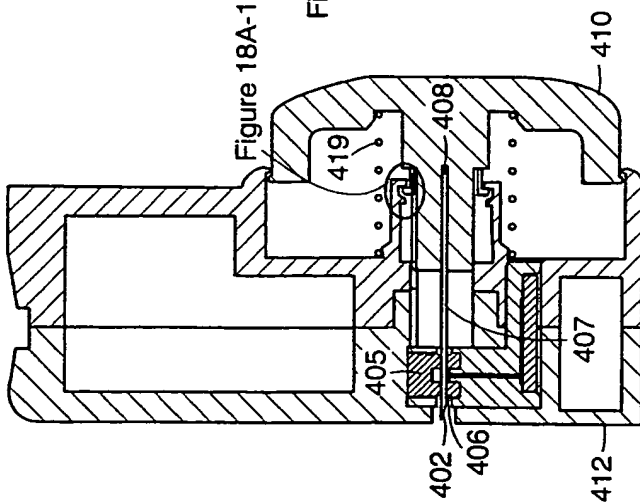


Figure 18A

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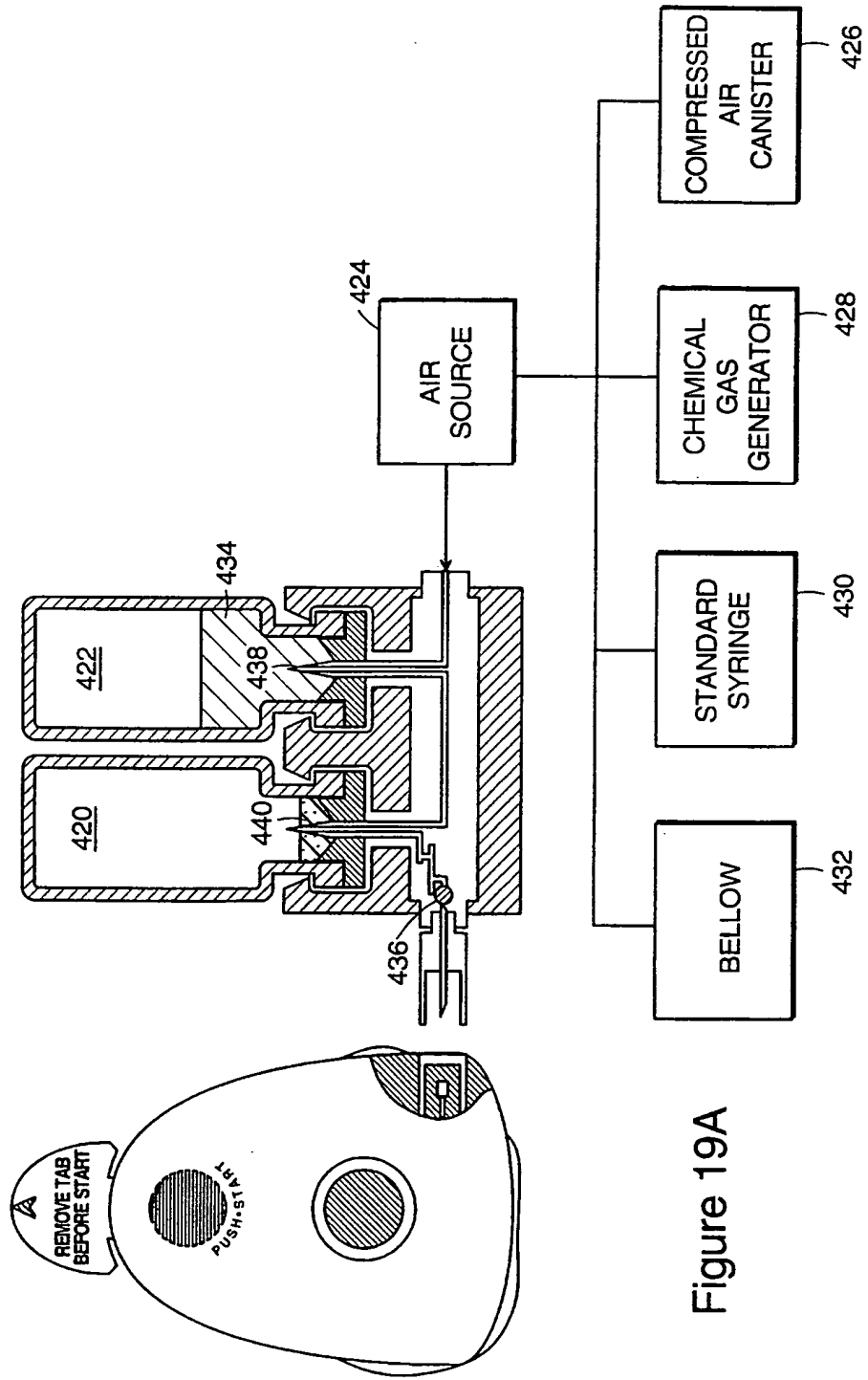


Figure 19A

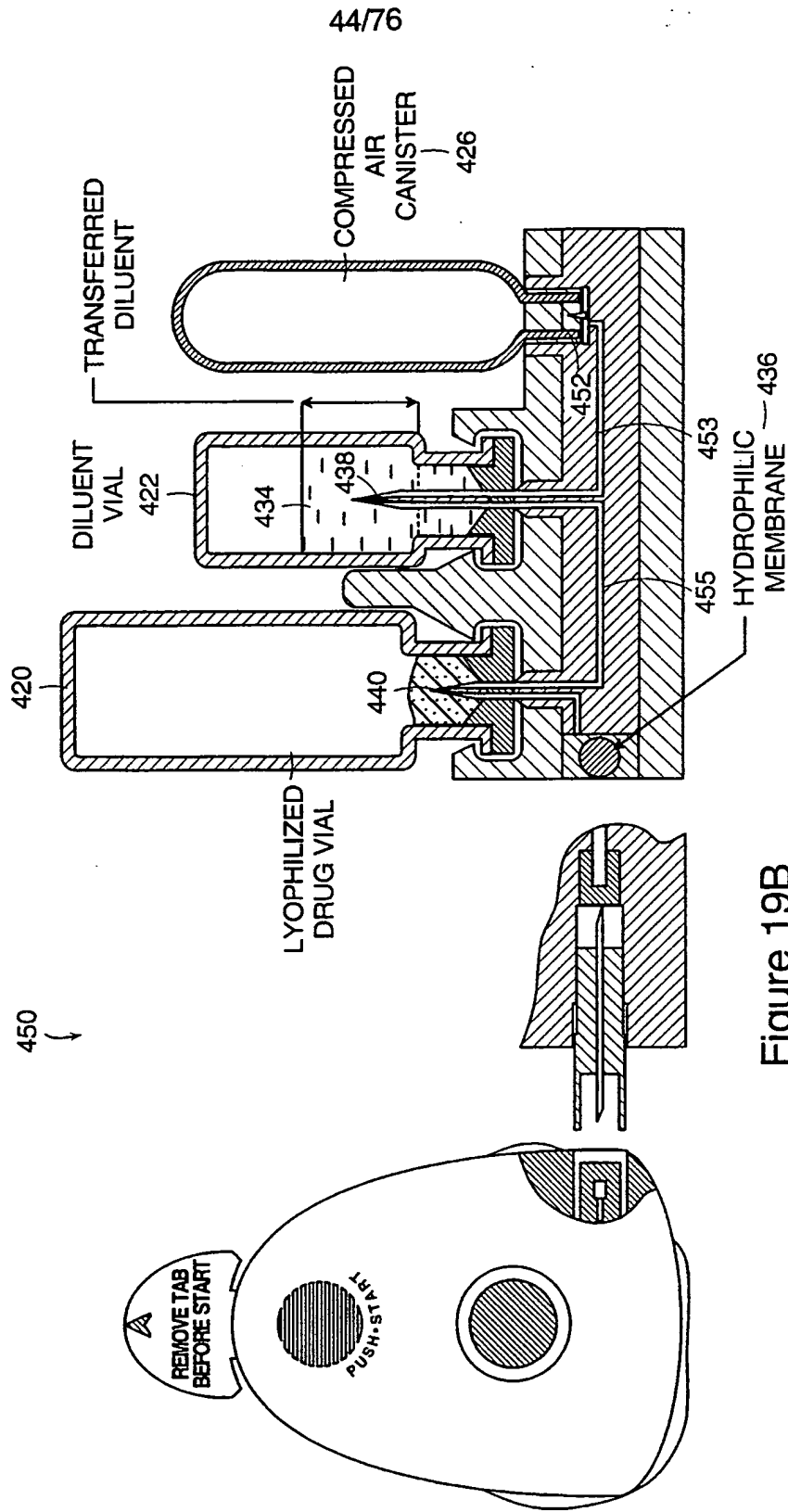


Figure 19B



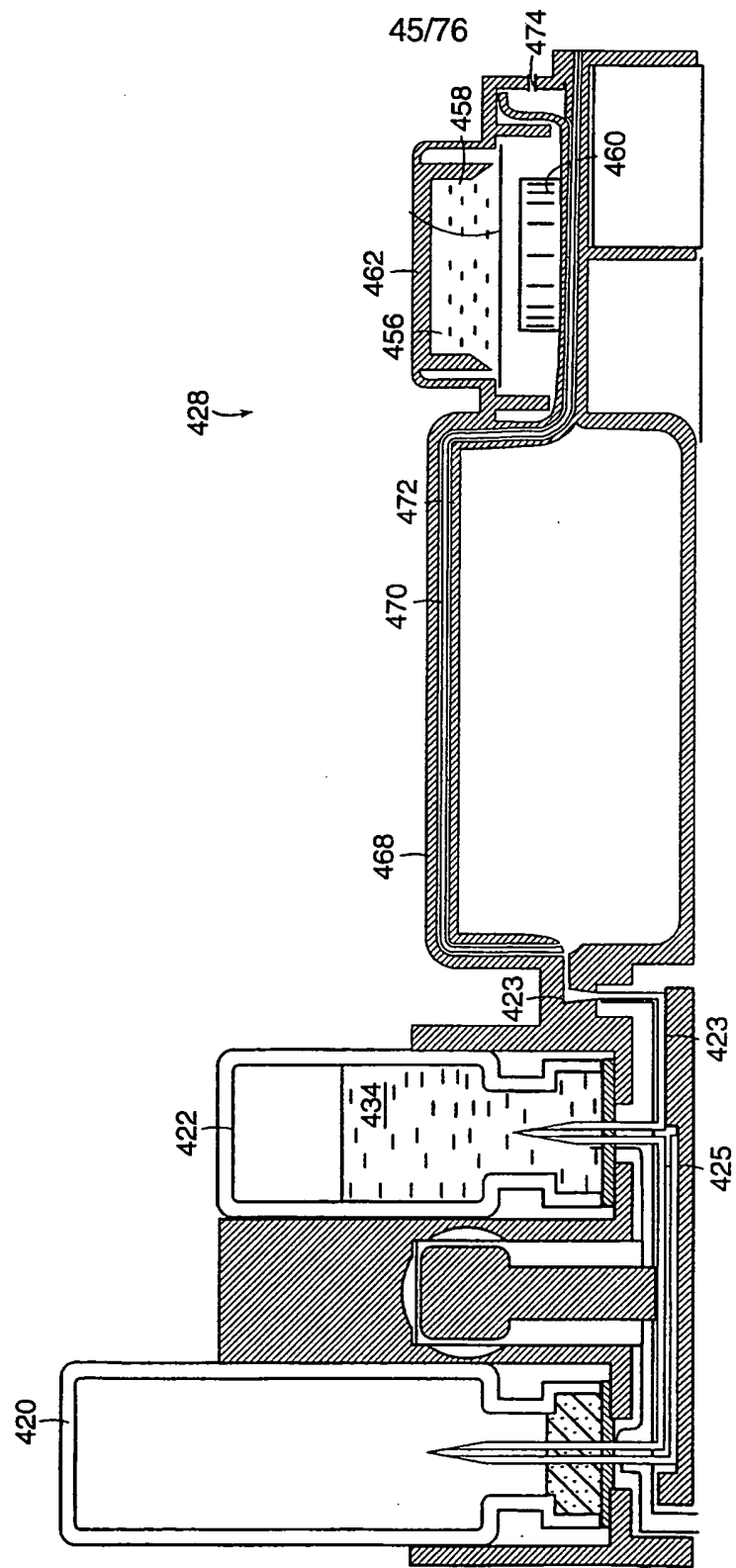


Figure 19C

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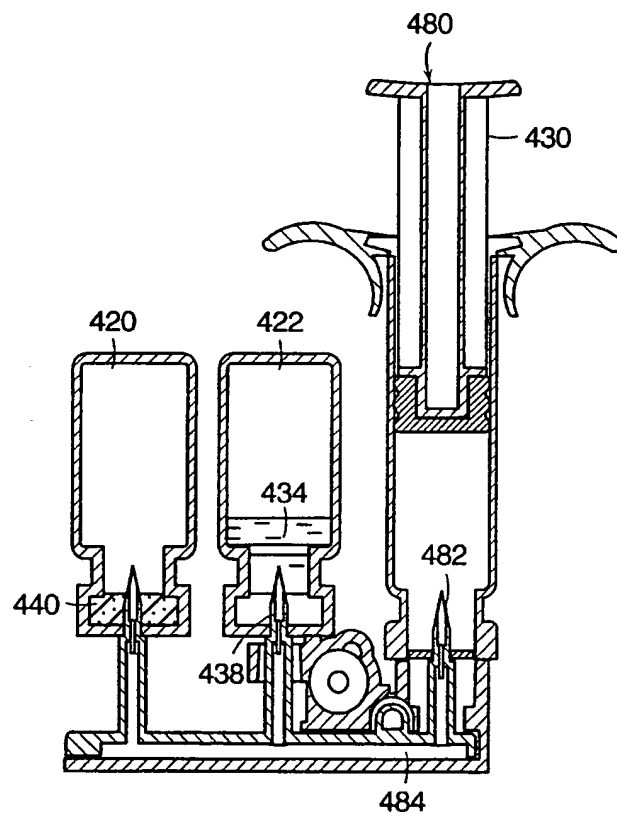


Figure 19D

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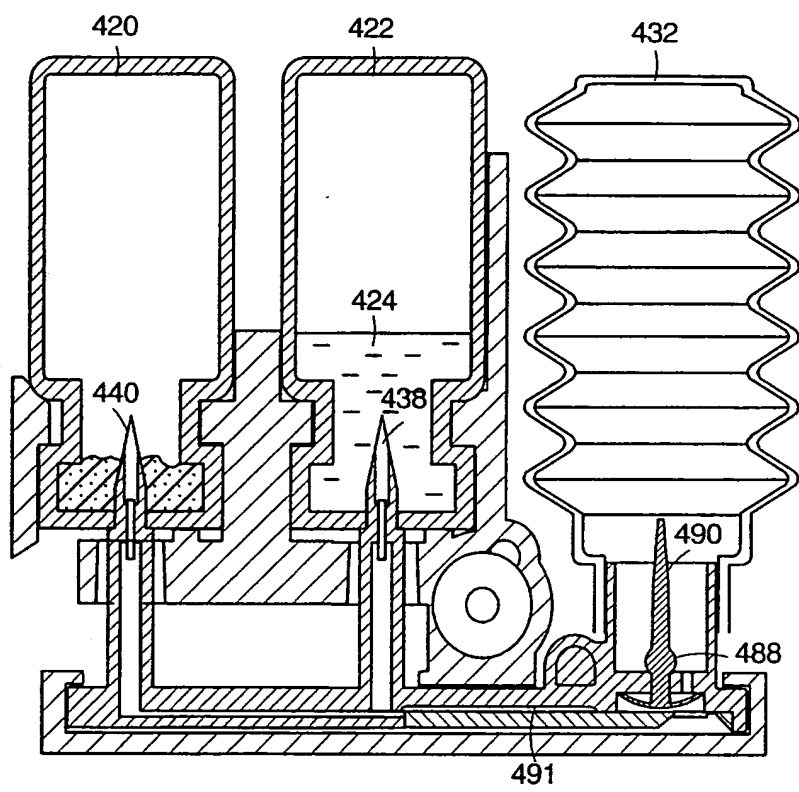


Figure 19E

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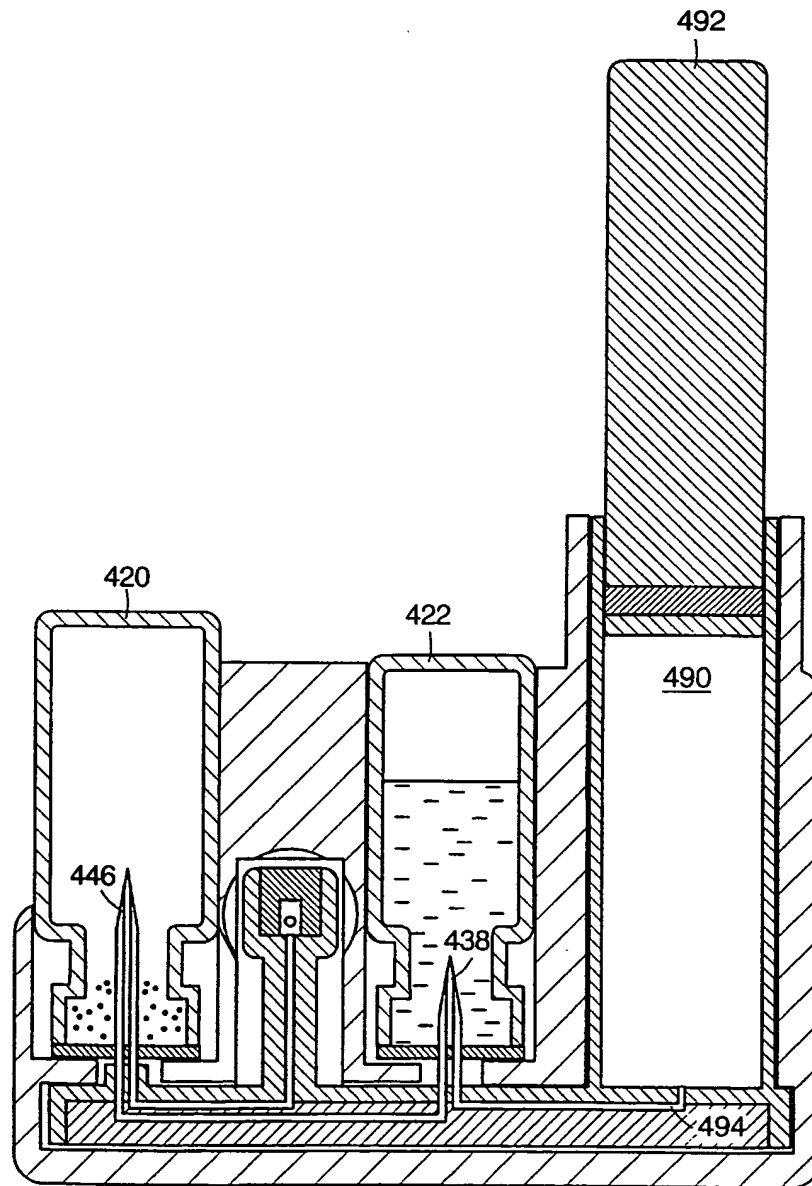


Figure 19F

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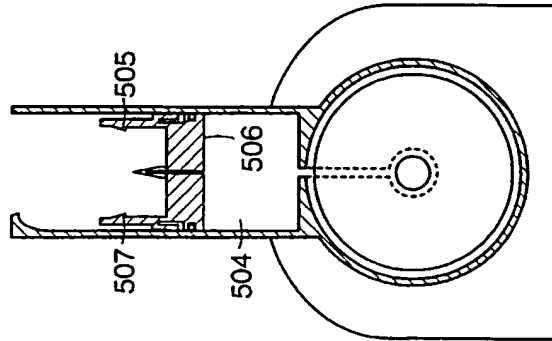
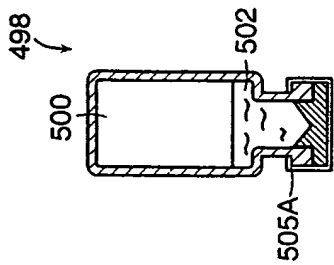


Figure 20A-1

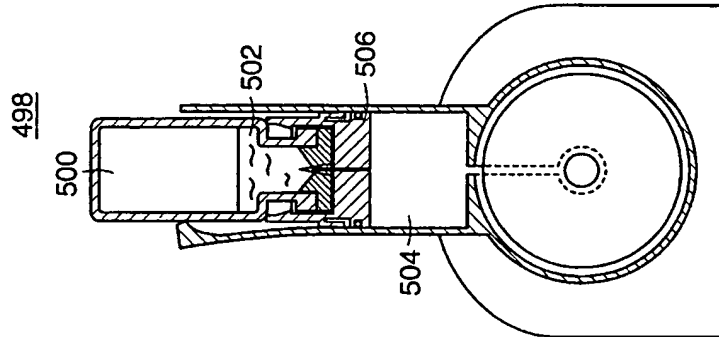


Figure 20A-2

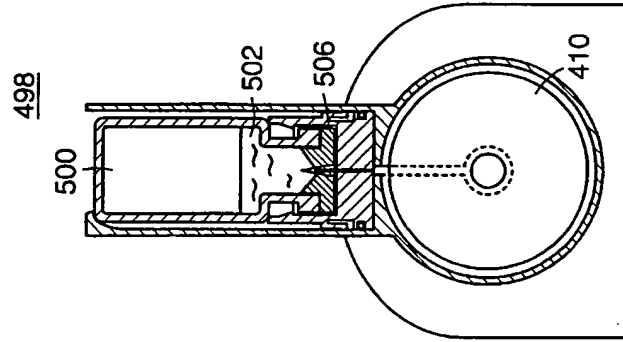


Figure 20A-3

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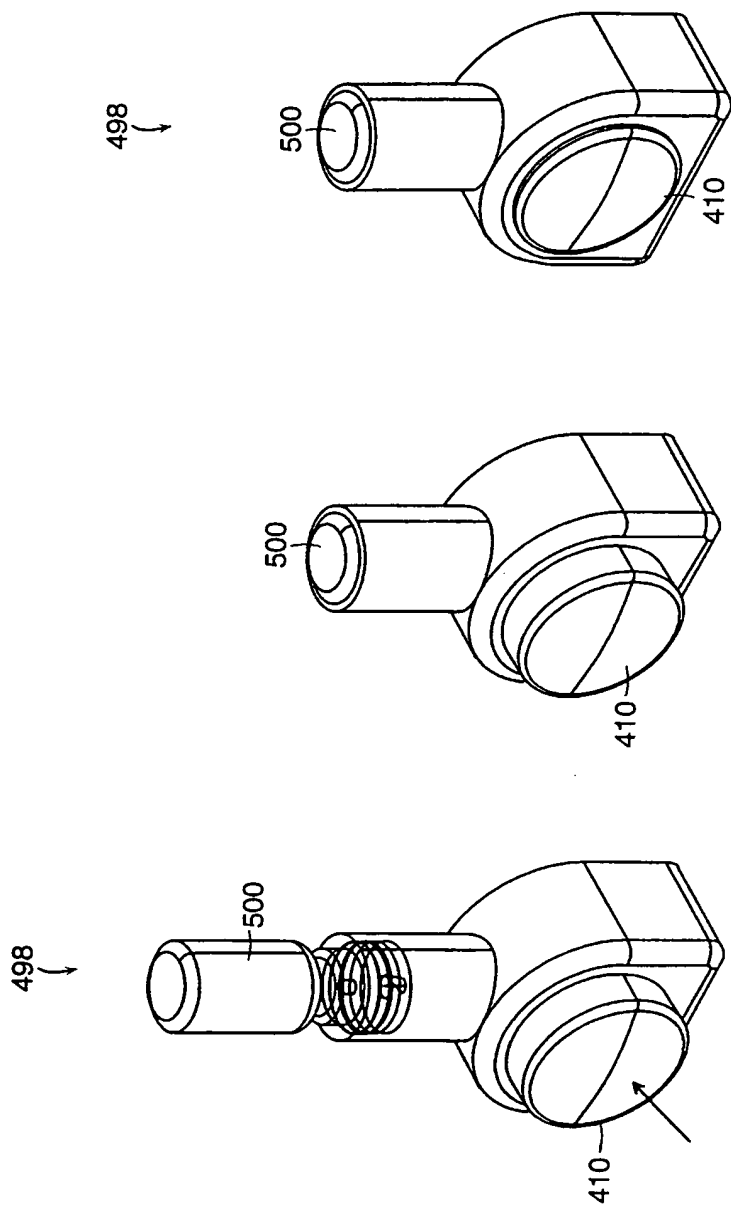


Figure 20B-3

Figure 20B-2

Figure 20B-1

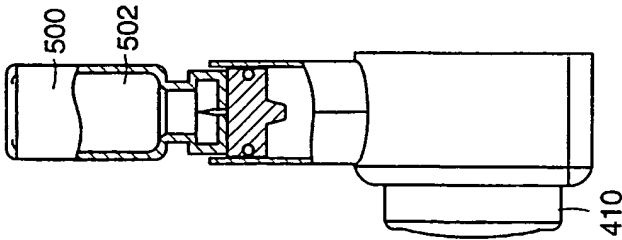


Figure 20C-1

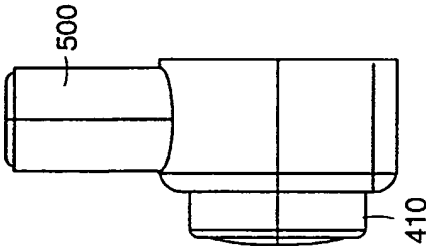


Figure 20C-2

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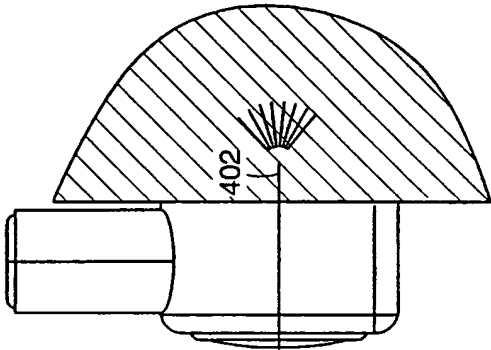


Figure 20C-3

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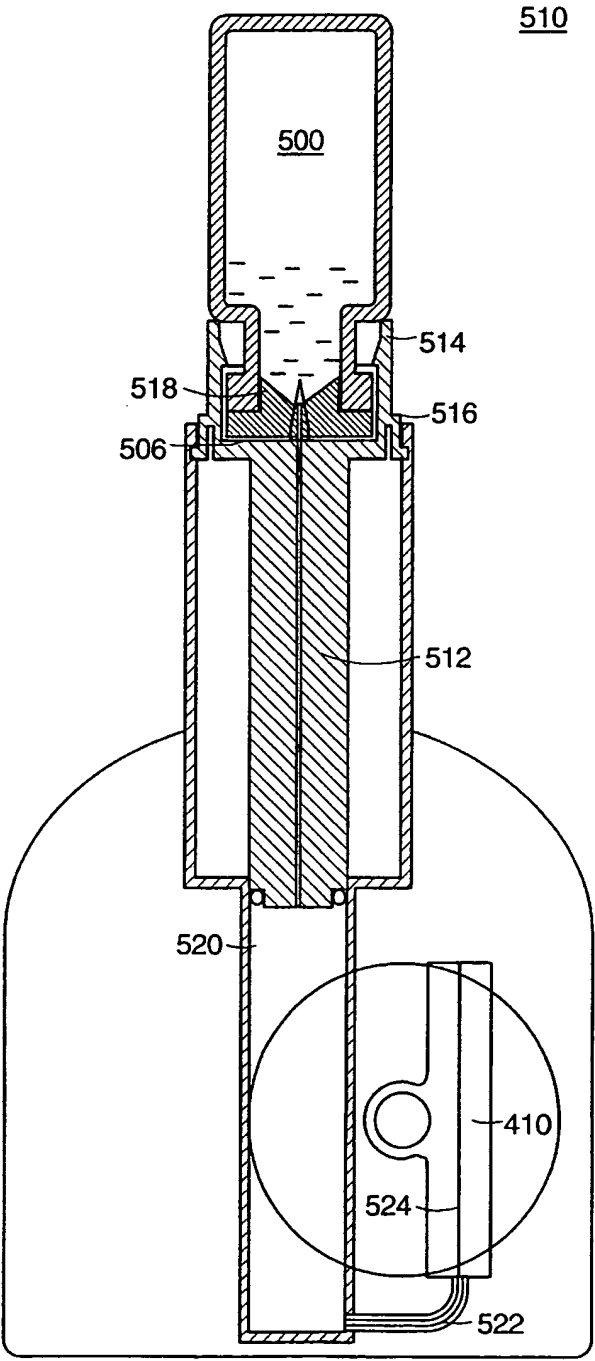


Figure 21



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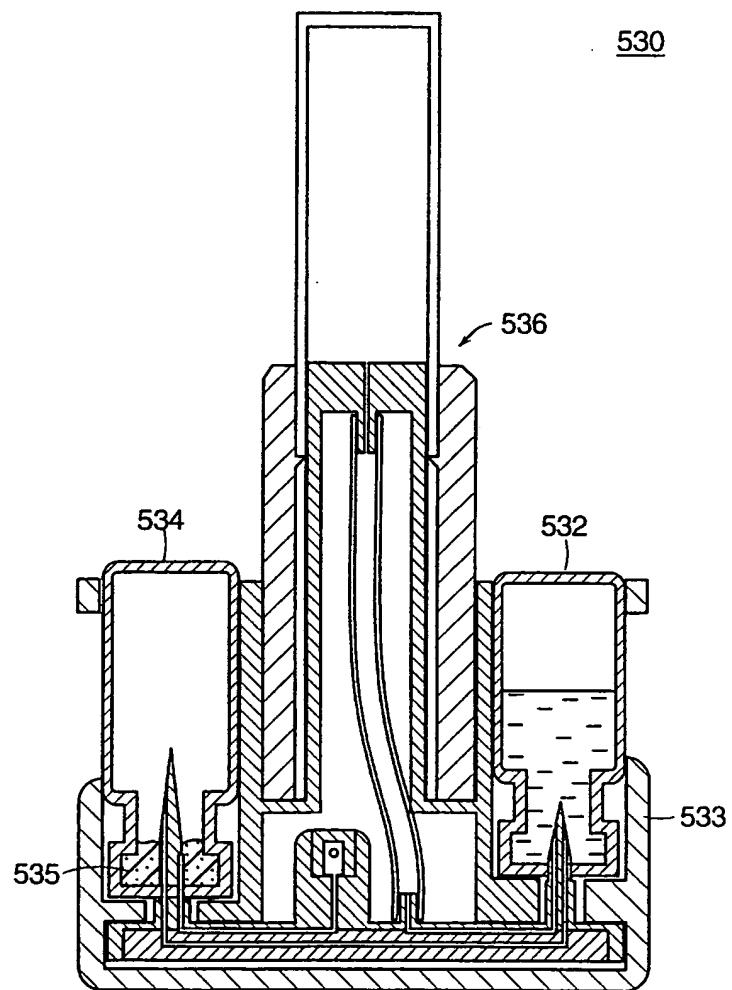


Figure 22A

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530  
↓

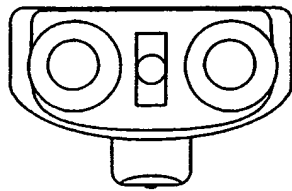


Figure 22B

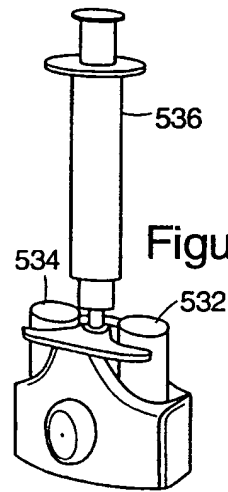


Figure 22C

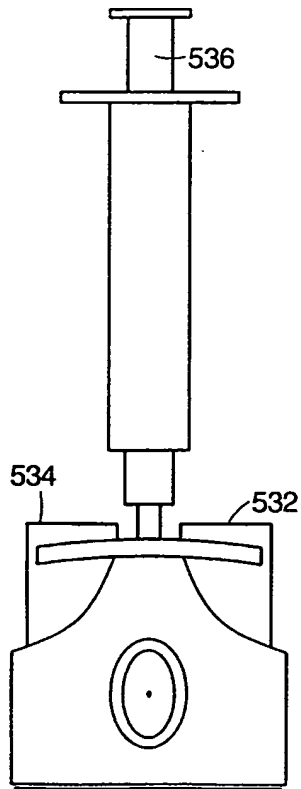


Figure 22D

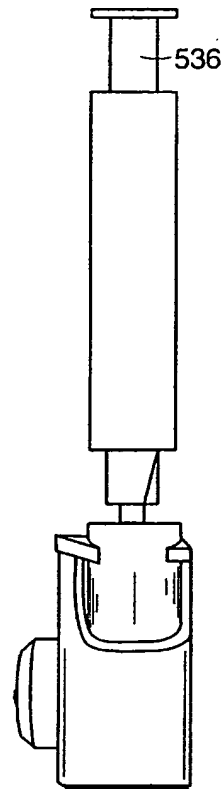


Figure 22E

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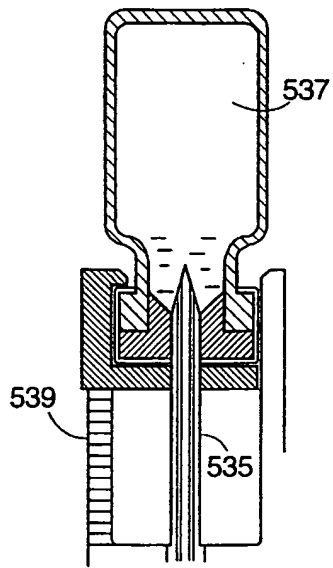


Figure 23A

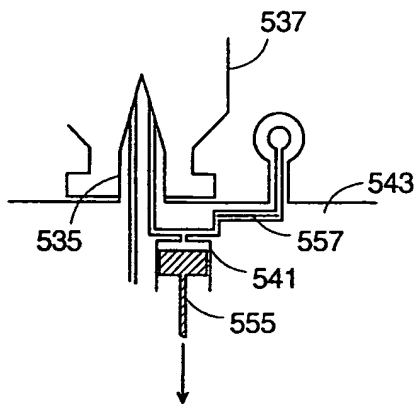


Figure 23B

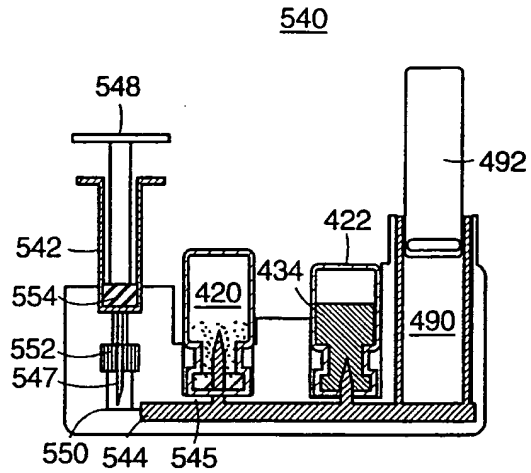


Figure 24A

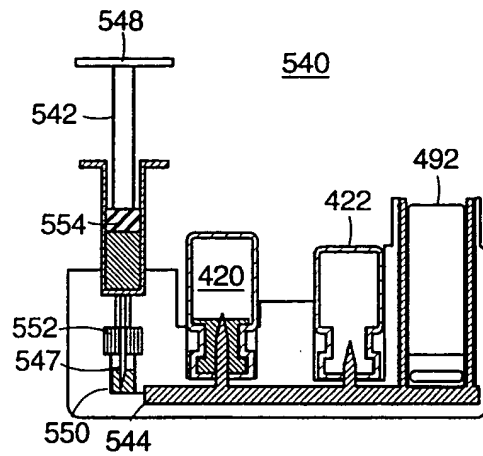


Figure 24B

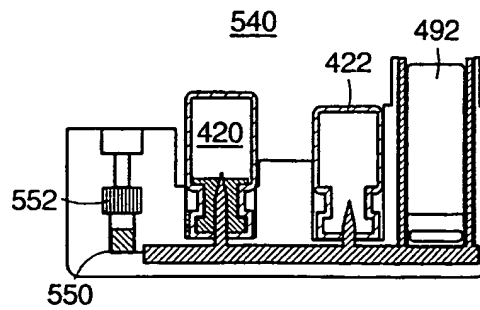


Figure 24C

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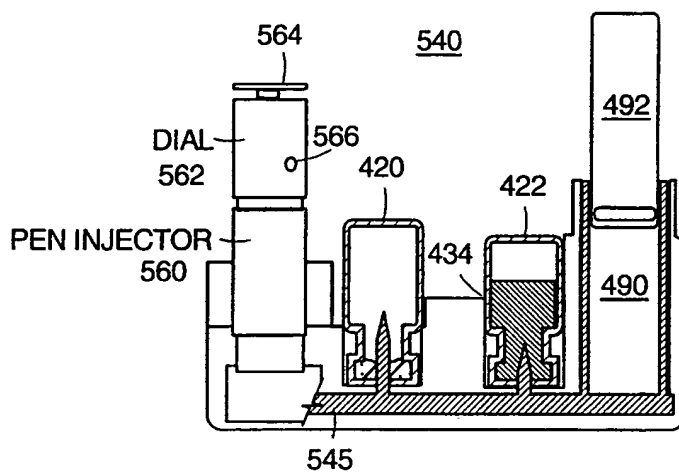


Figure 25

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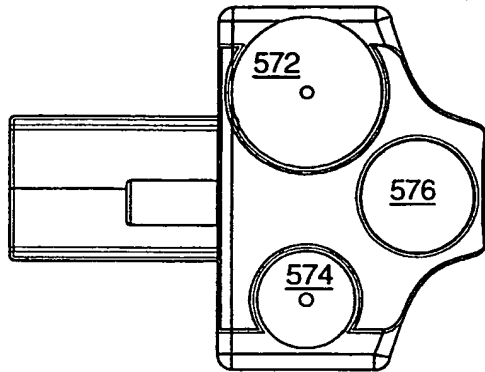


Figure 26A

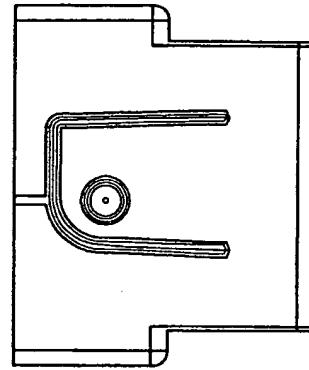


Figure 26B

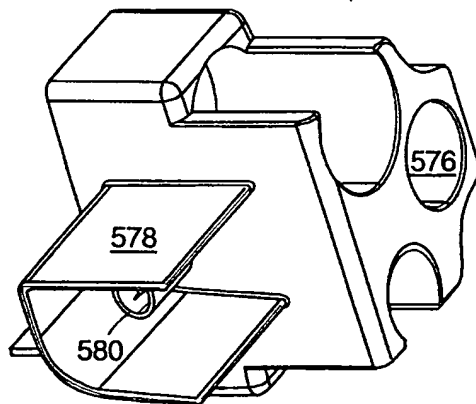


Figure 26C

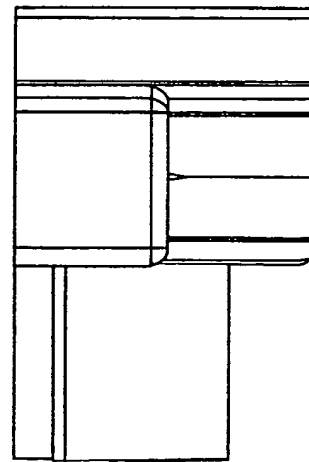


Figure 26D

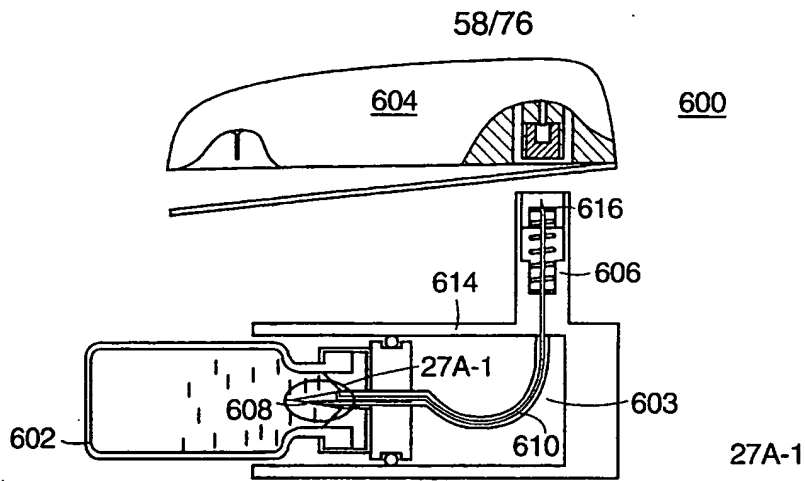


Figure 27A

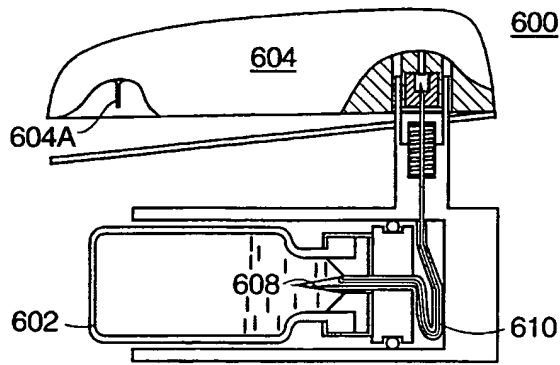


Figure 27B

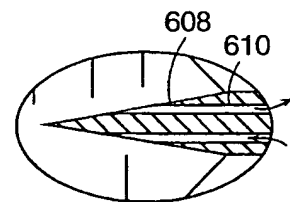


Figure 27A-1

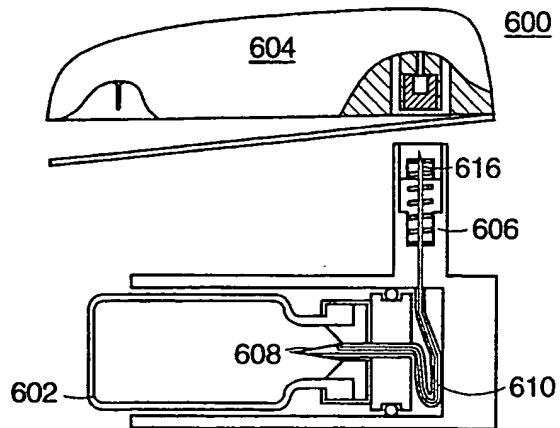


Figure 27C

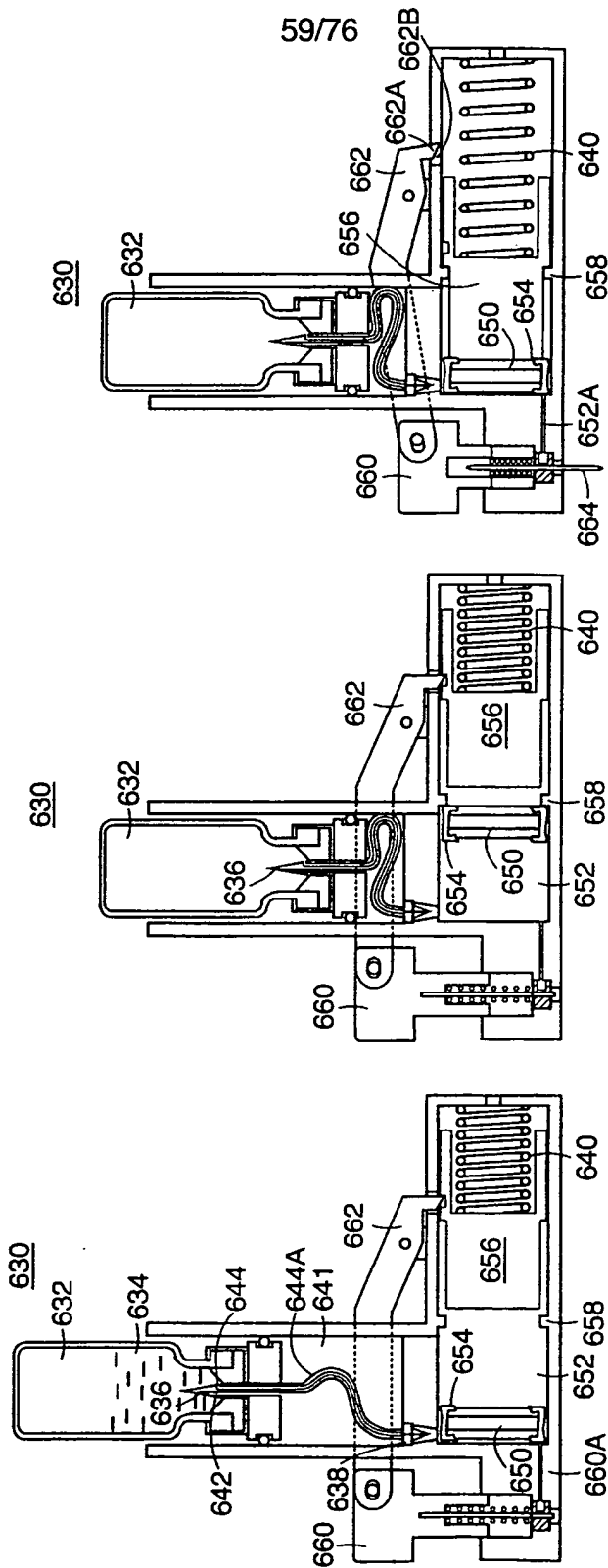


Figure 28C

Figure 28B

Figure 28A

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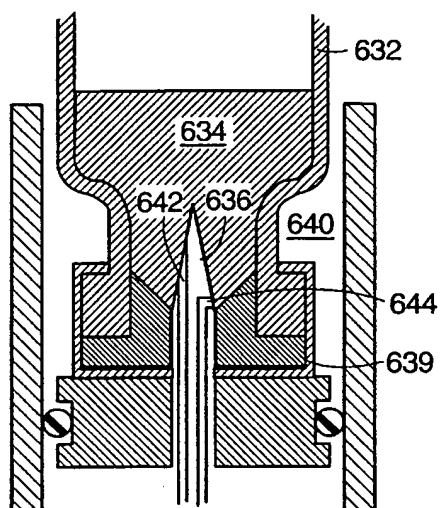


Figure 28D



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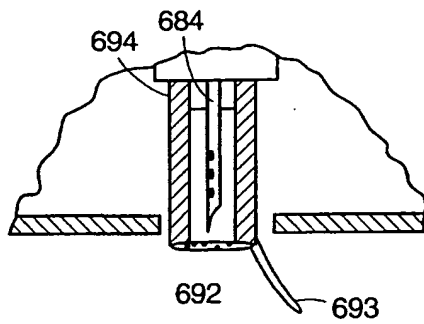


Figure 29A-1

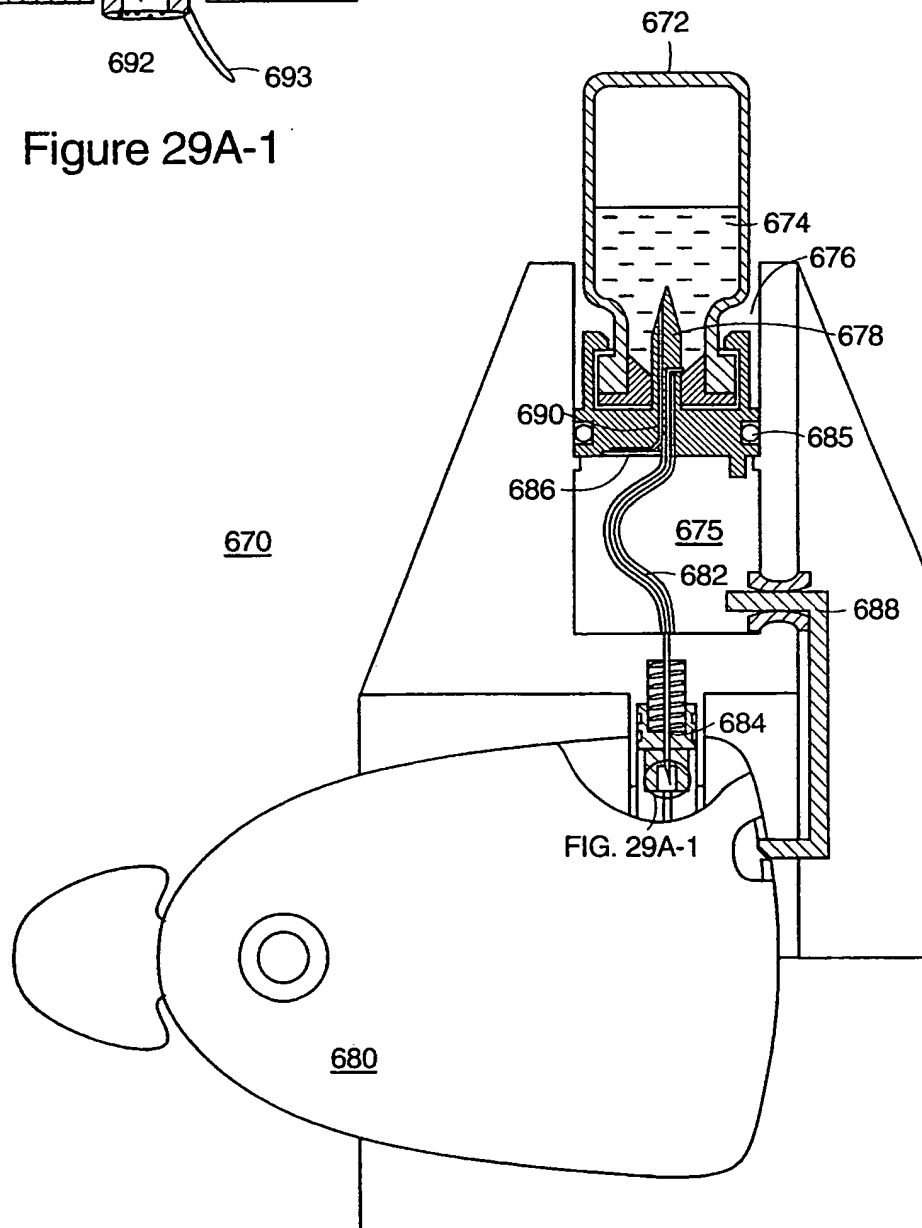


Figure 29A

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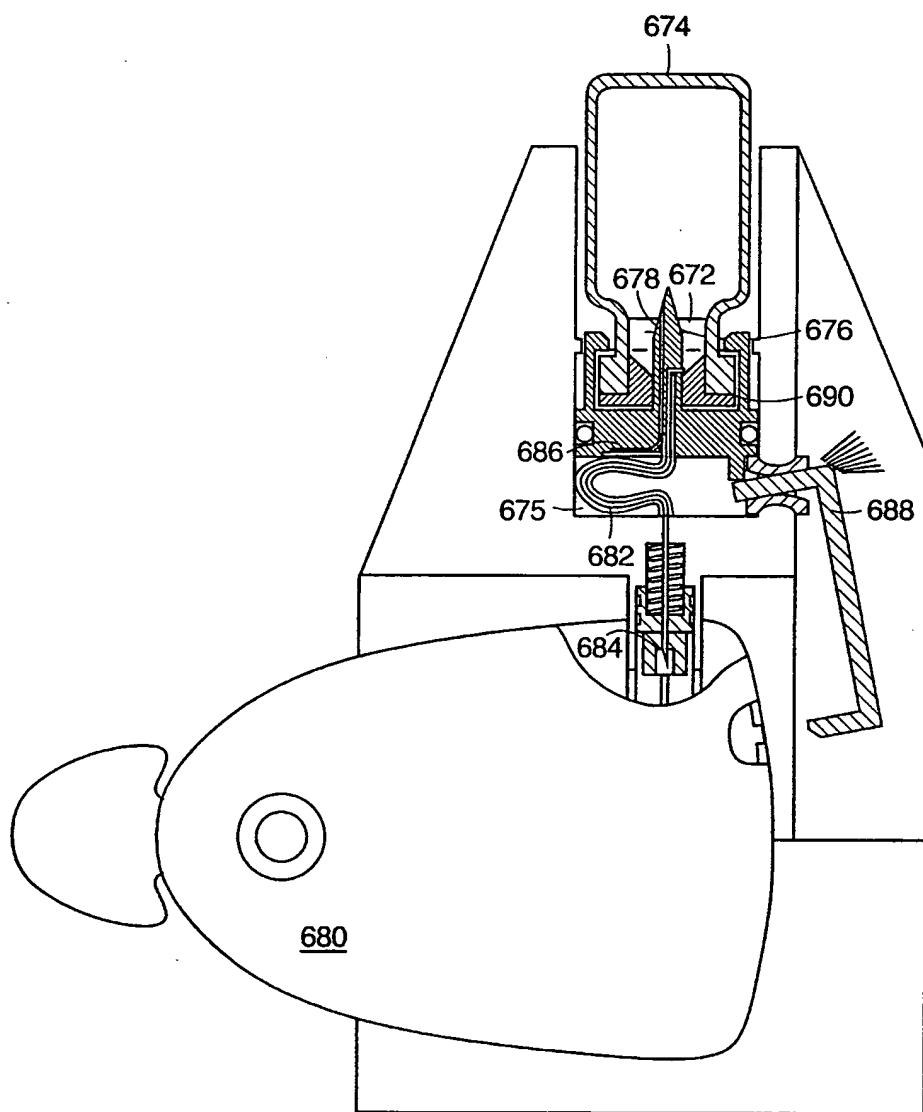


Figure 29B

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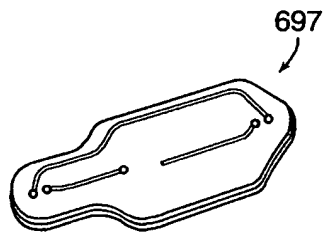


Figure 30B

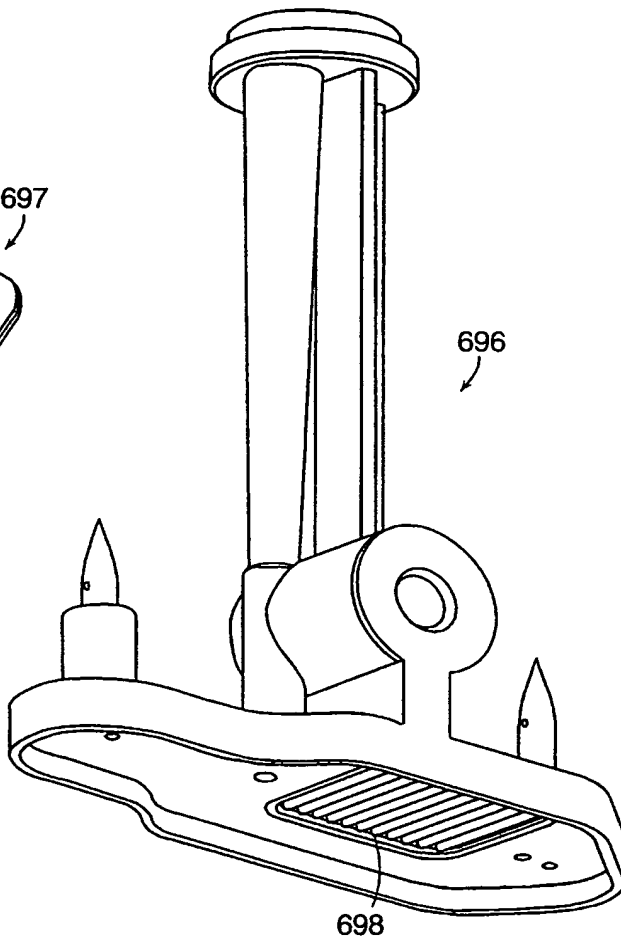
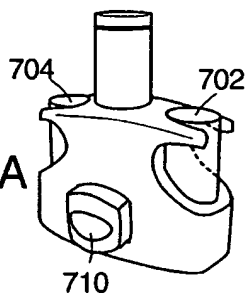


Figure 30A

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Figure 31A



700

Figure 31B

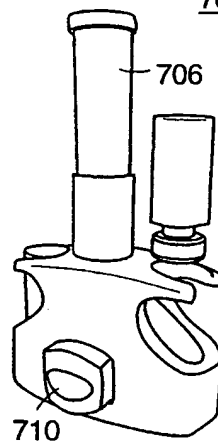


Figure 31C

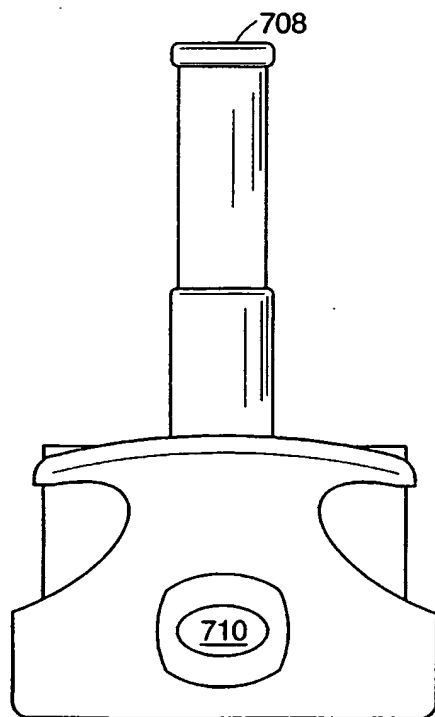
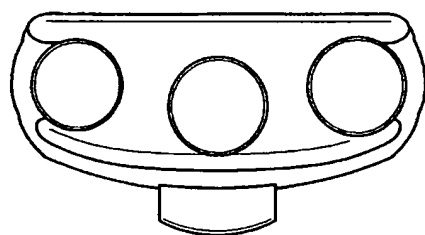


Figure 31D

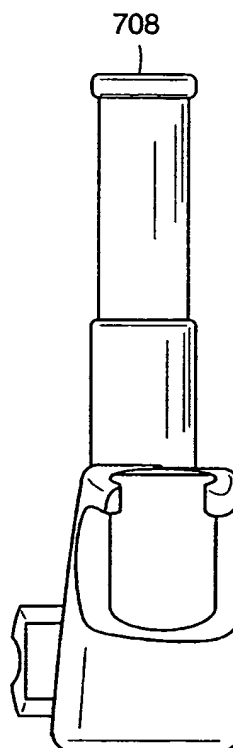


Figure 31E

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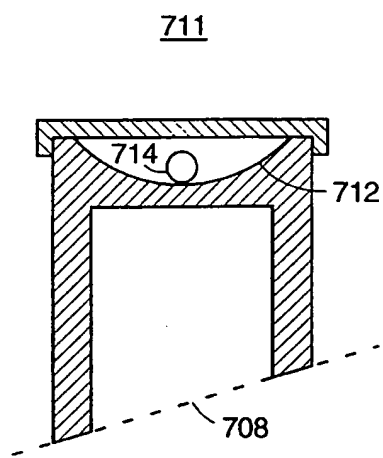


Figure 31F

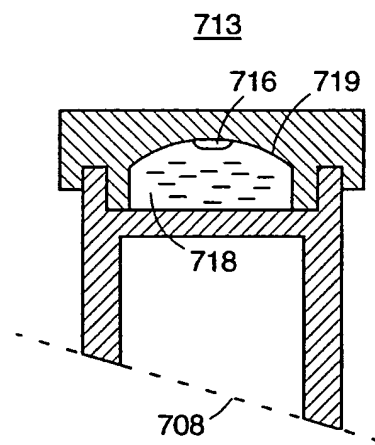


Figure 31G

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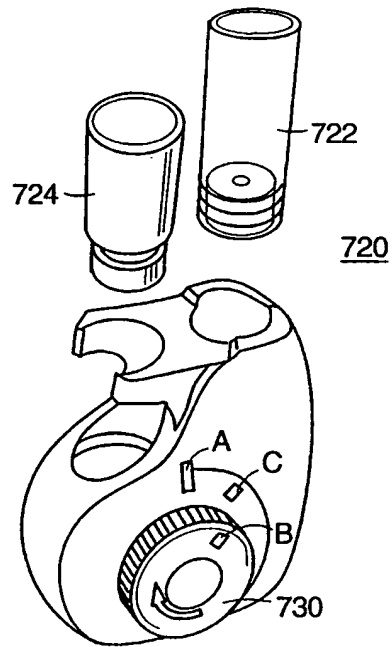


Figure 32A

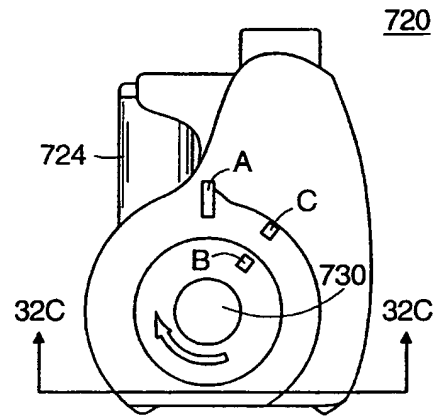


Figure 32B

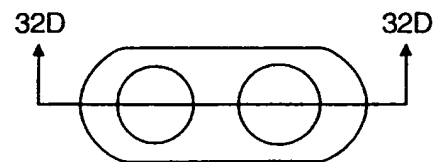


Figure 32C

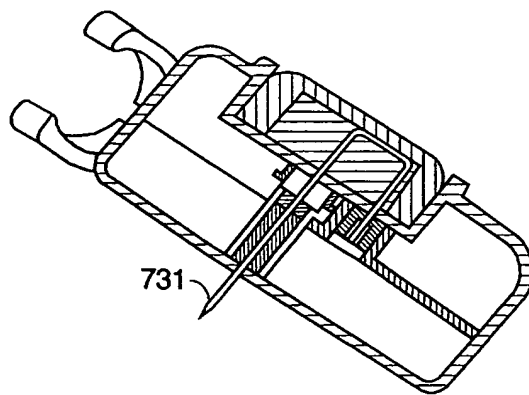


Figure 32D

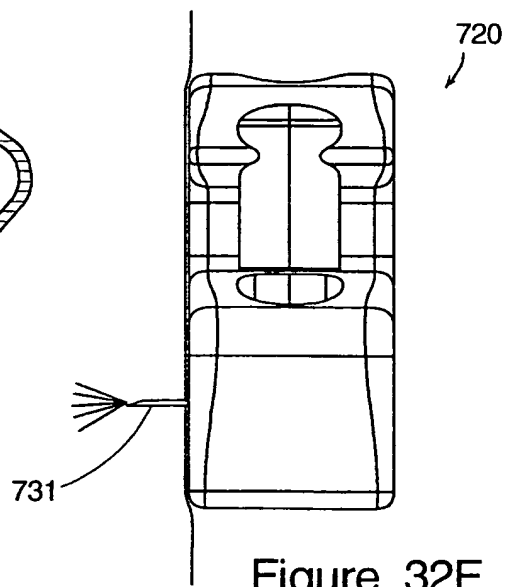


Figure 32E

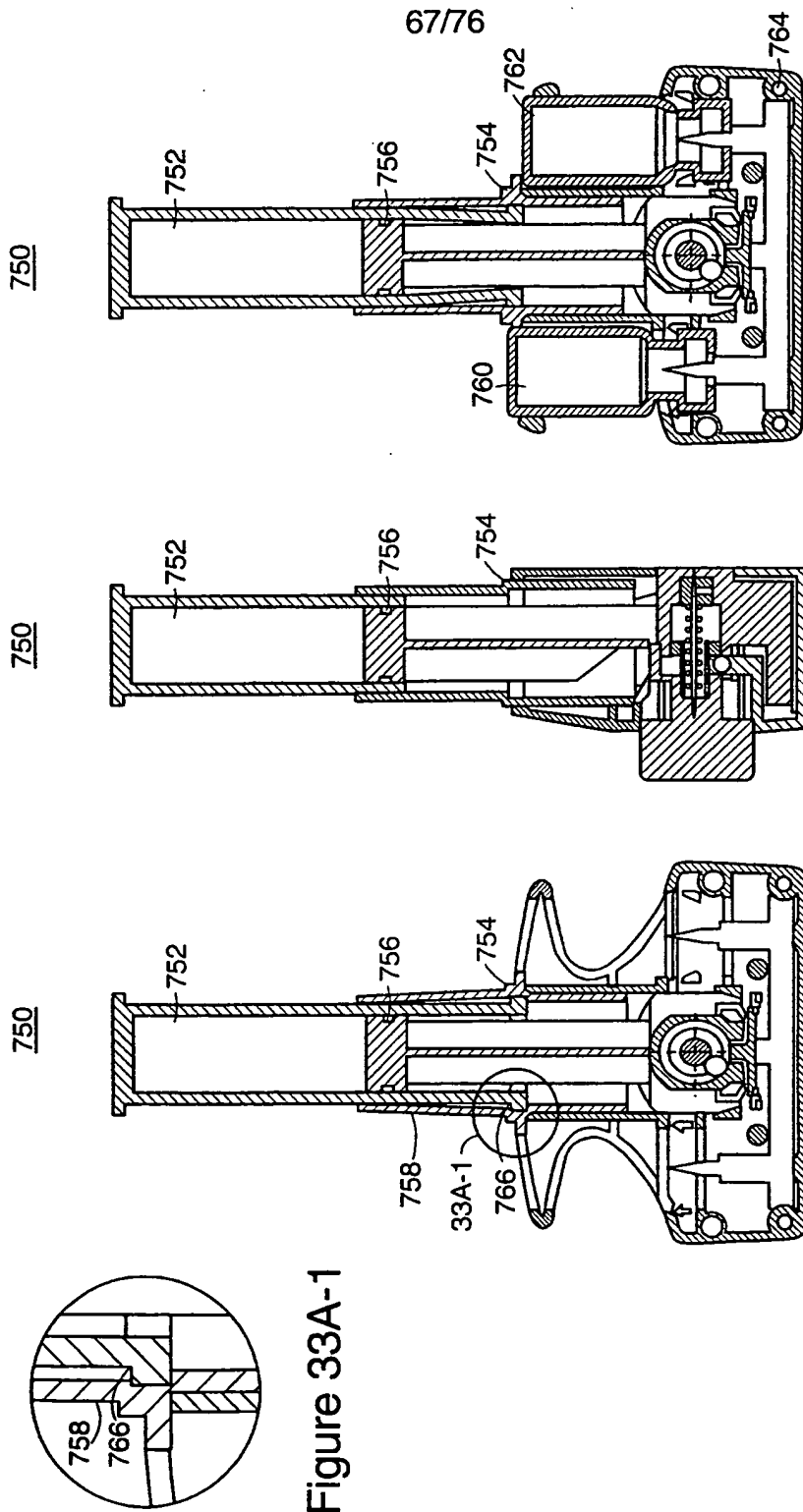


Figure 33A-1

Figure 33C

Figure 33B

Figure 33A

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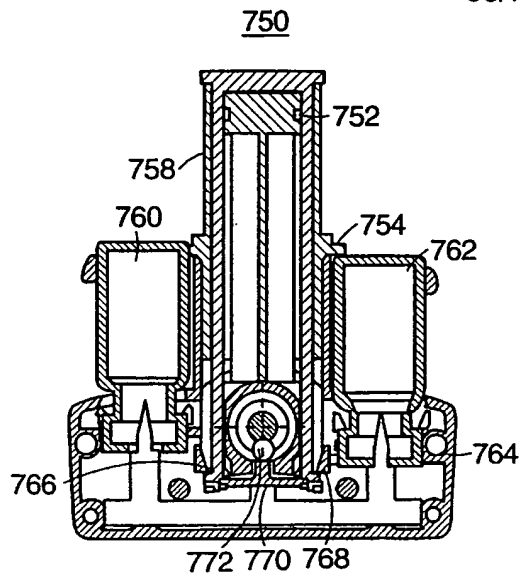


Figure 33D

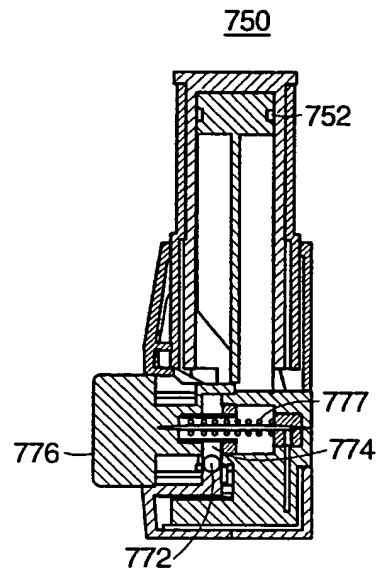


Figure 33E

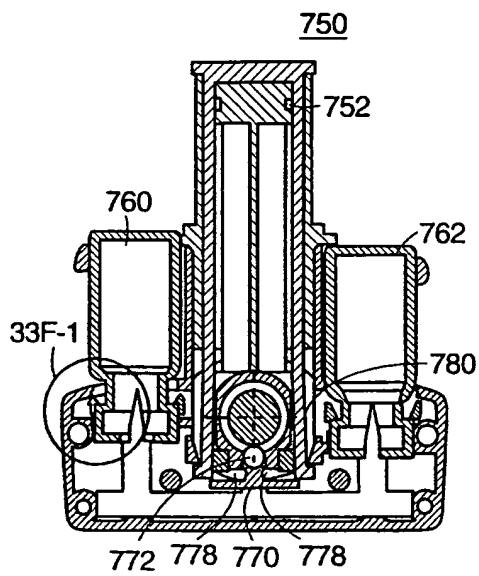


Figure 33F

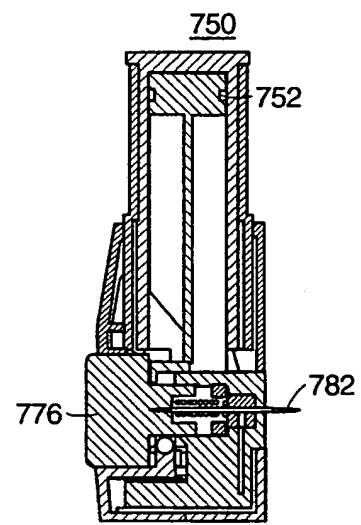


Figure 33G

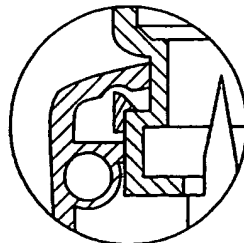


Figure 33F-1



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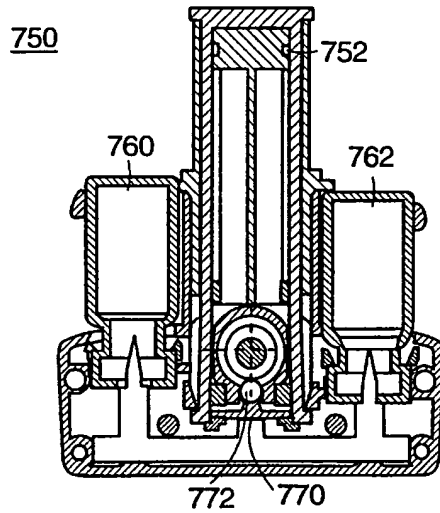


Figure 33H

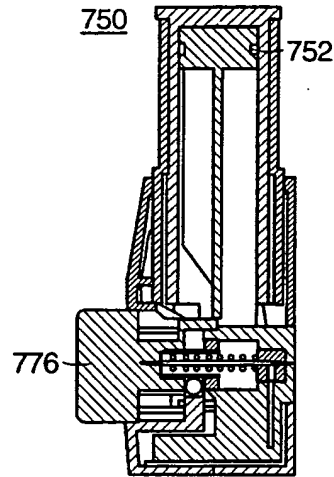


Figure 33I

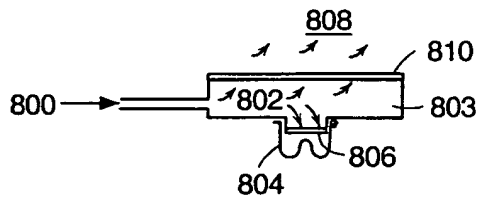


Figure 34A

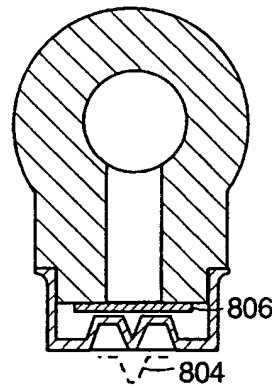


Figure 34C

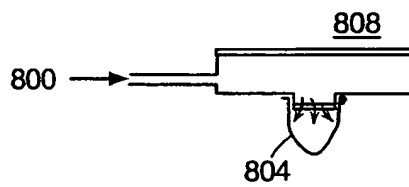


Figure 34B

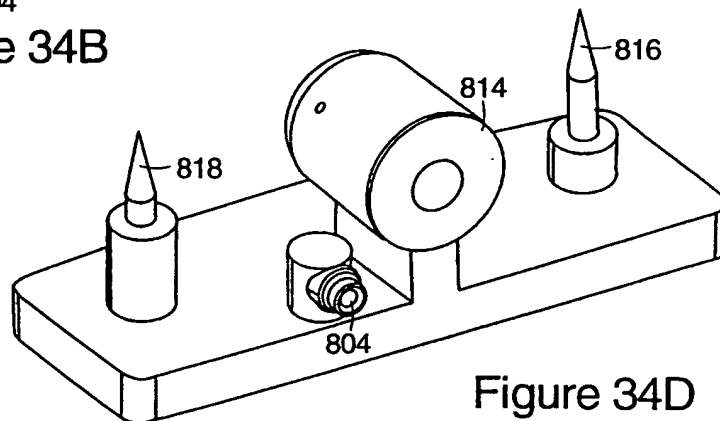


Figure 34D

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TYPICAL INJECTION PROFILE  
DELIVERY FROM HIGH VOLUME VIAL  
DELIVERY PROFILE (SIMULATION) - NO ADDITIONAL AIR.

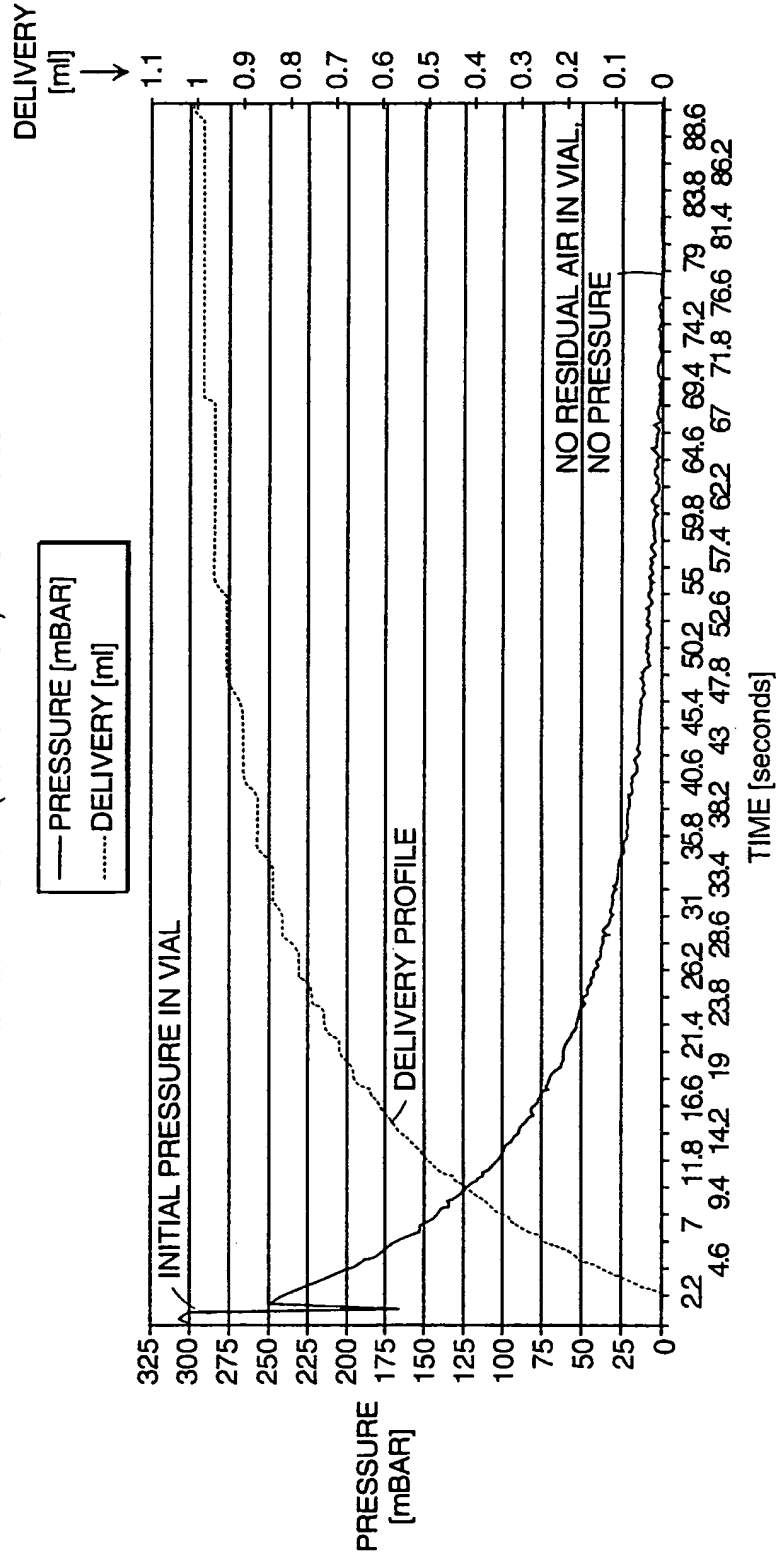


Figure 35

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TYPICAL INJECTION PROFILE  
DELIVERY FROM HIGH VOLUME VIAL

DELIVERY DURATION & DELIVERY PRESSURE / AIR VOLUME (SIMULATION CONFIGURATION)

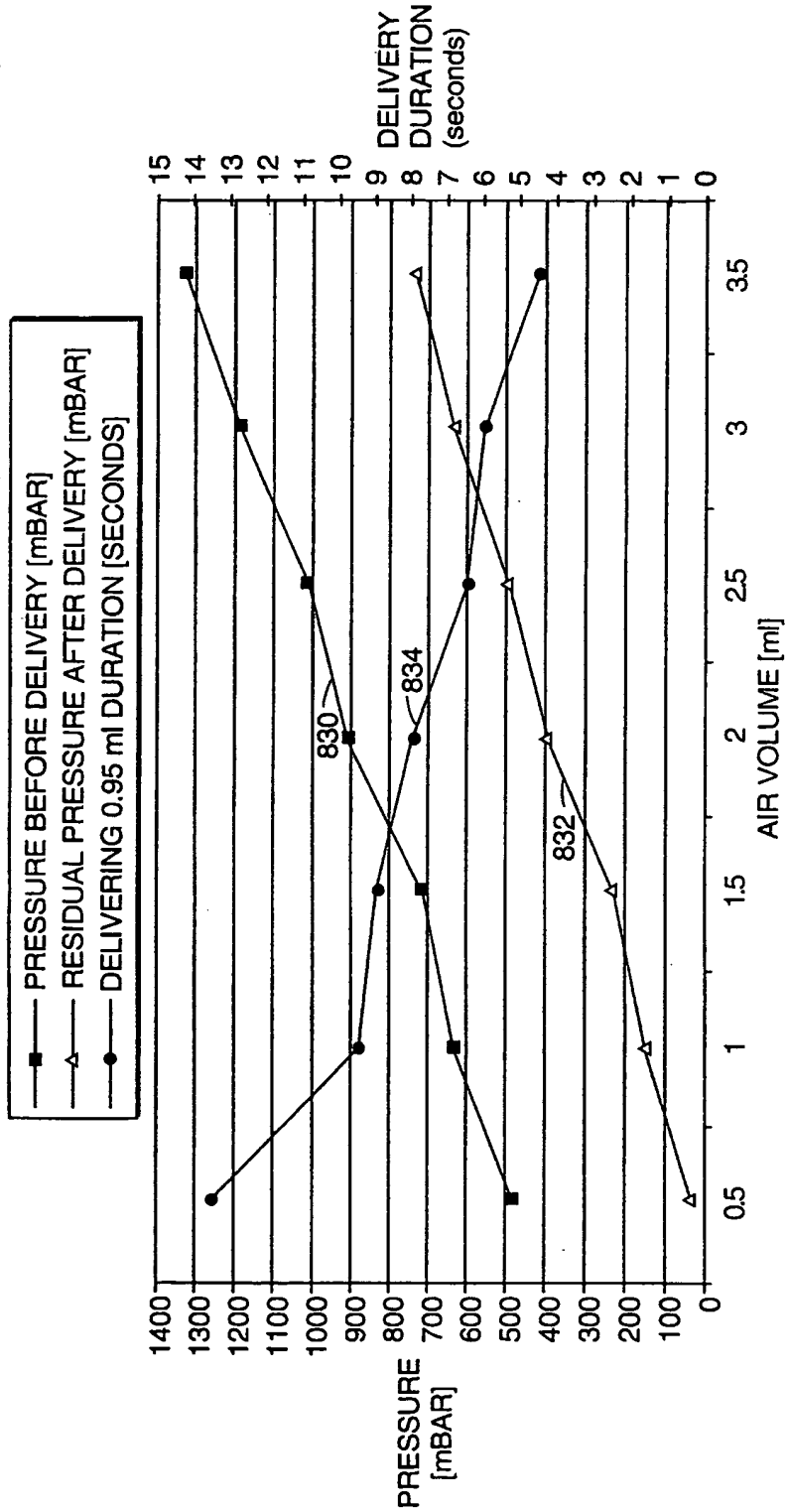


Figure 36

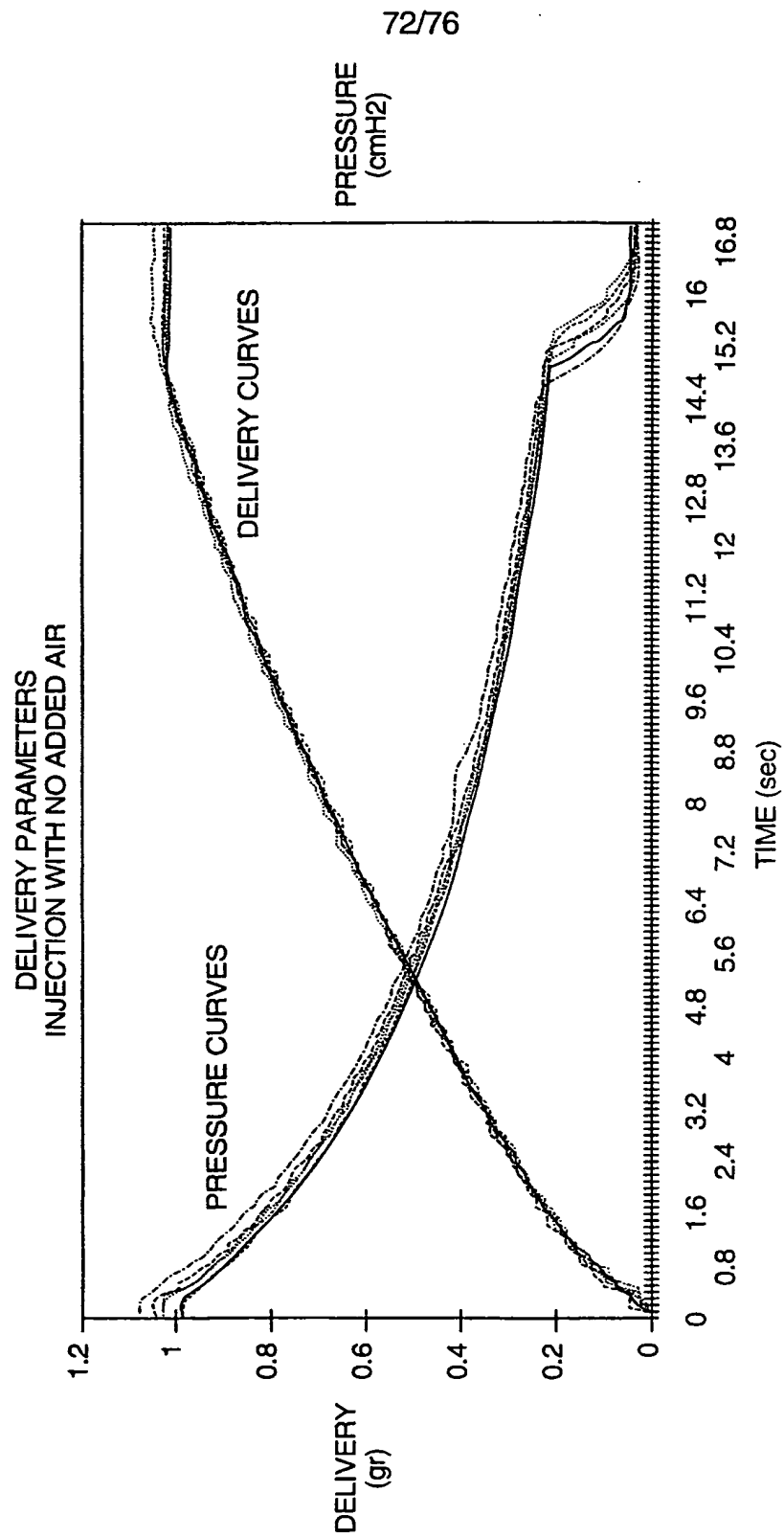


Figure 37

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AIR PRESSURE GRADIENT ON HYDROPHILIC MEMBRANE

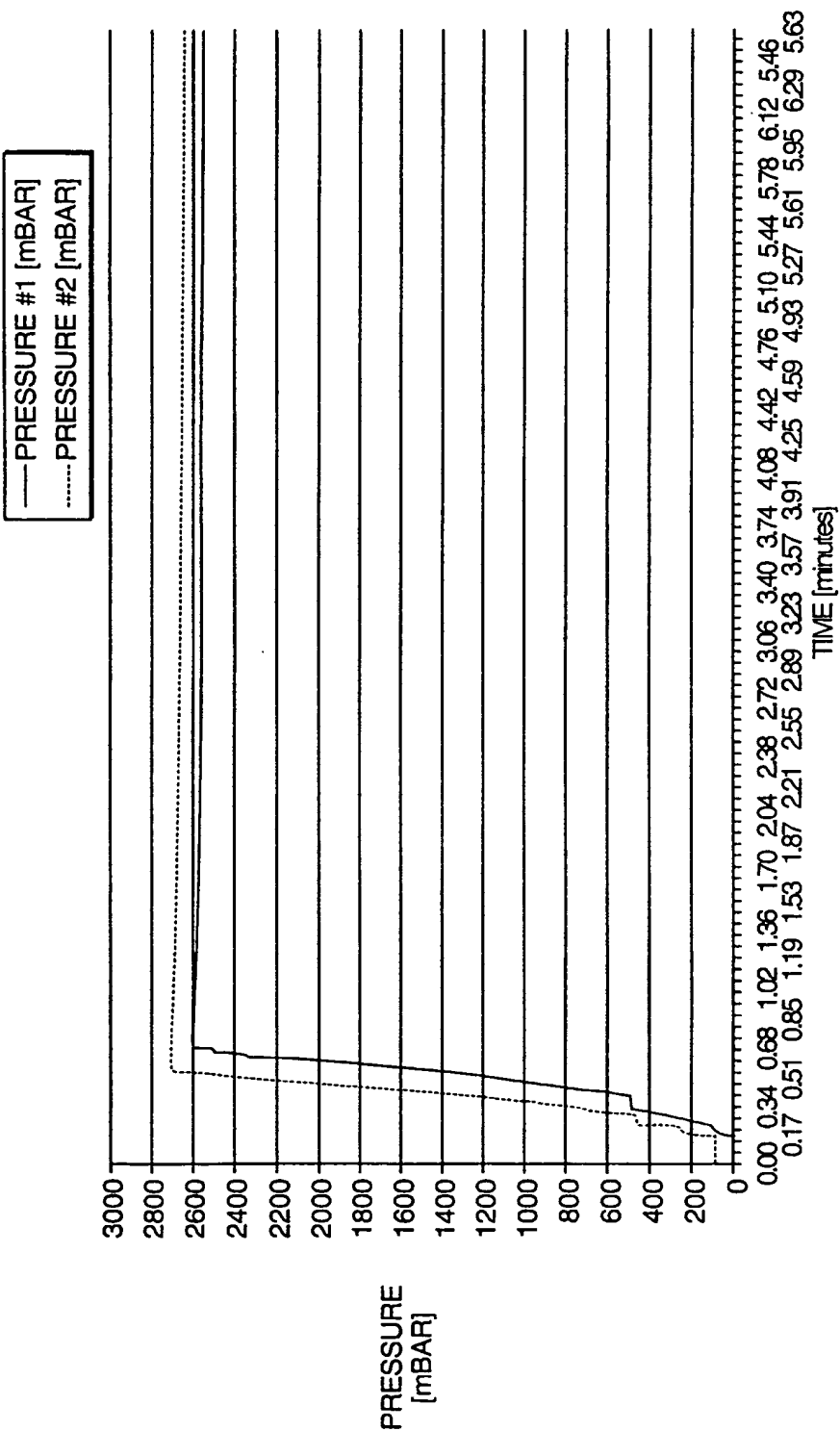


Figure 38

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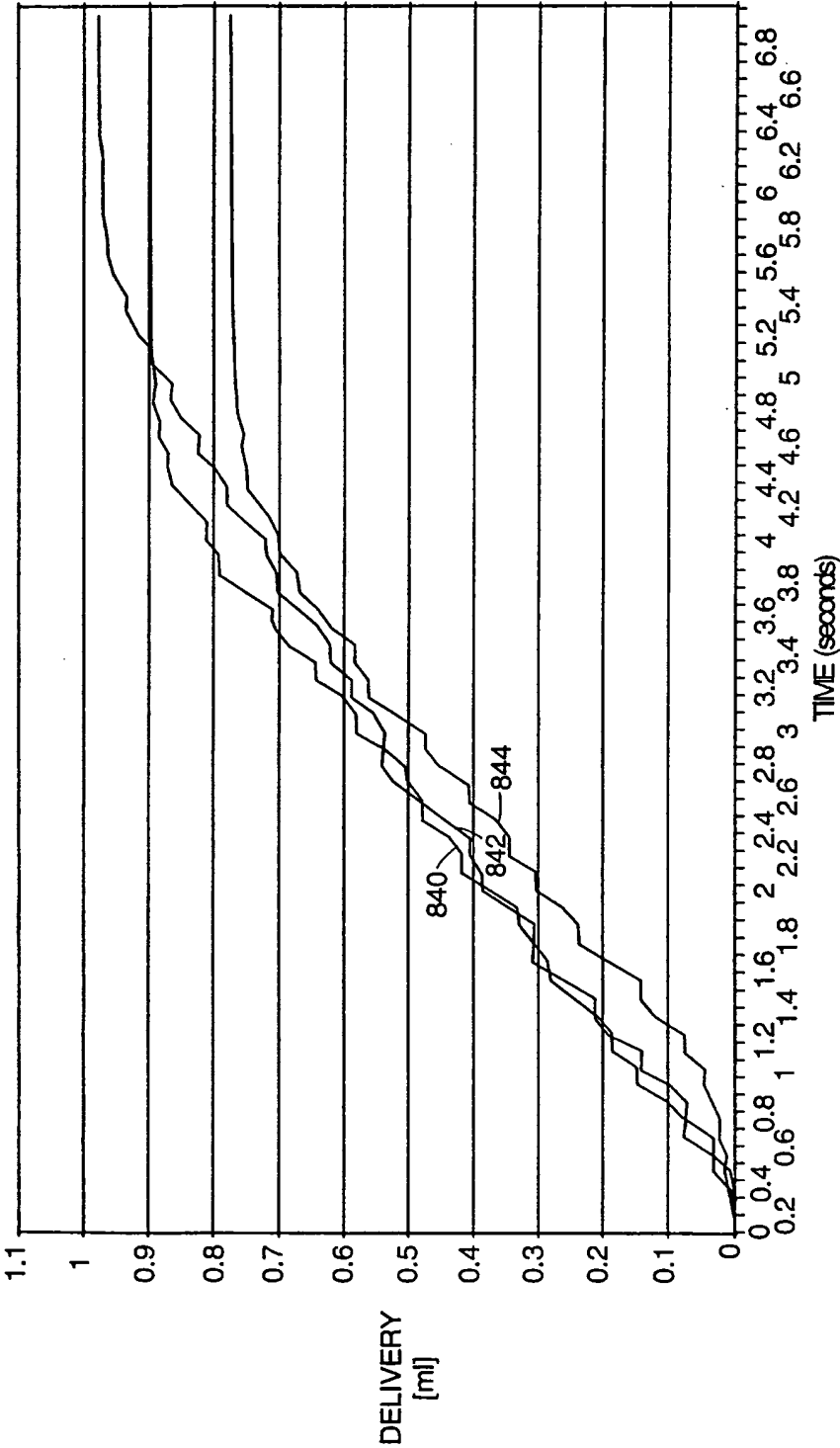


Figure 39

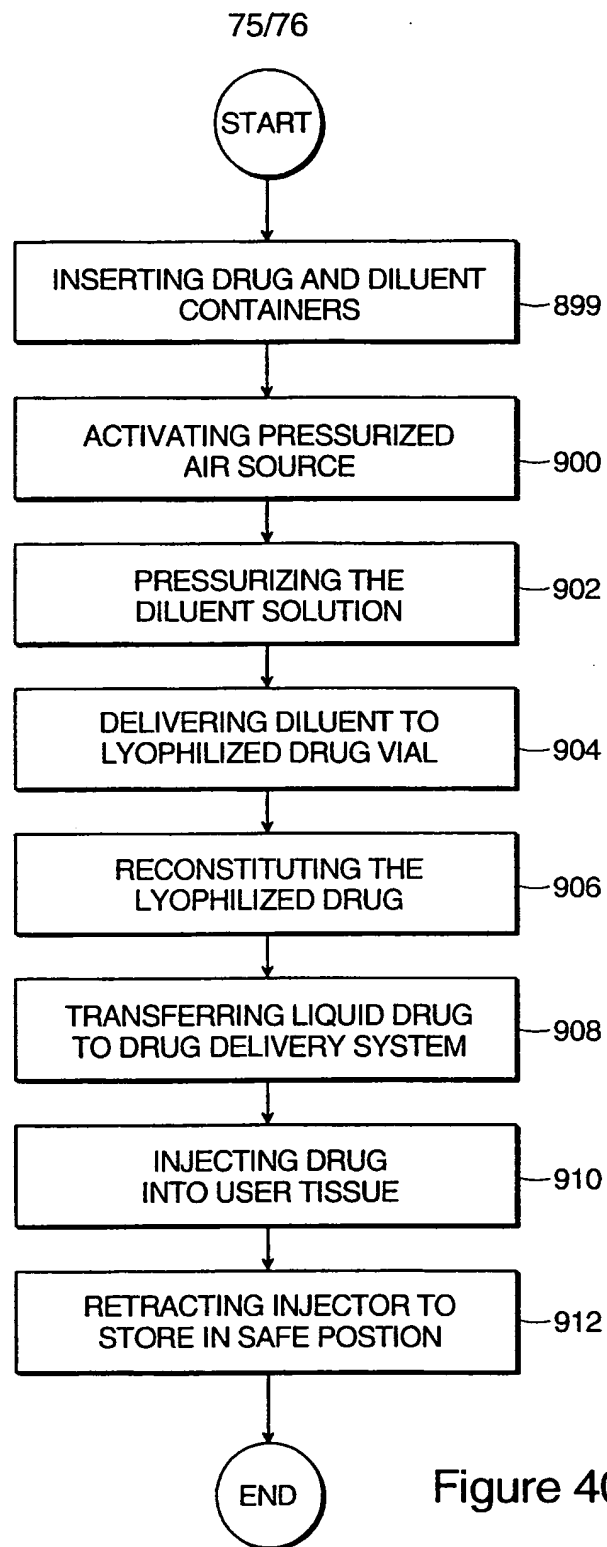


Figure 40

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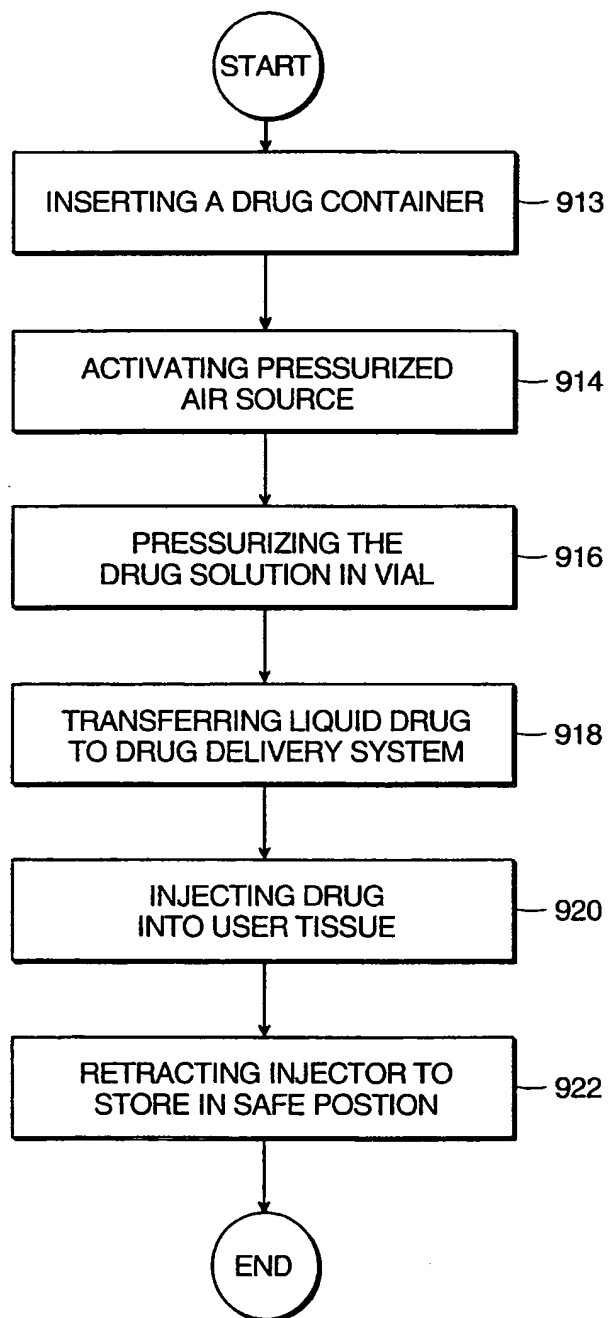


Figure 41



# INTERNATIONAL SEARCH REPORT

International Application No  
PCT/US 99/26751

<b>A. CLASSIFICATION OF SUBJECT MATTER</b> IPC 7    A61M5/24    A61M5/19    A61M5/178		
According to International Patent Classification (IPC) or to both national classification and IPC		
<b>B. FIELDS SEARCHED</b> Minimum documentation searched (classification system followed by classification symbols) IPC 7    A61M		
Documentation searched other than minimum documentation to the extent that such documents are included in the fields searched		
Electronic data base consulted during the international search (name of data base and, where practical, search terms used)		
<b>C. DOCUMENTS CONSIDERED TO BE RELEVANT</b>		
Category *	Citation of document, with indication, where appropriate, of the relevant passages	Relevant to claim No.
X	US 4 755 169 A (SARNOFF STANLEY J ET AL) 5 July 1988 (1988-07-05)  column 7, line 12 -column 9, line 20; figures	1,2, 4-12, 18-30
X	US 4 915 689 A (THEEUWES FELIX) 10 April 1990 (1990-04-10)  see figures 2 and 8 and their related description	1,2,4,5, 7,8, 11-14, 19,20
X	US 5 329 976 A (HABER TERRY M ET AL) 19 July 1994 (1994-07-19)  column 8, line 32 -column 10, line 48; figures	1,2, 4-13, 18-30
-/-		
<input checked="" type="checkbox"/> Further documents are listed in the continuation of box C.		
<input checked="" type="checkbox"/> Patent family members are listed in annex.		
<b>* Special categories of cited documents :</b>  <div style="display: flex; justify-content: space-between;"> <div style="width: 45%;"> <p>"A" document defining the general state of the art which is not considered to be of particular relevance</p> <p>"E" earlier document but published on or after the International filing date</p> <p>"L" document which may throw doubts on priority claim(s) or which is cited to establish the publication date of another citation or other special reason (as specified)</p> <p>"O" document referring to an oral disclosure, use, exhibition or other means</p> <p>"P" document published prior to the international filing date but later than the priority date claimed</p> </div> <div style="width: 45%;"> <p>"T" later document published after the International filing date or priority date and not in conflict with the application but cited to understand the principle or theory underlying the invention</p> <p>"X" document of particular relevance; the claimed invention cannot be considered novel or cannot be considered to involve an inventive step when the document is taken alone</p> <p>"Y" document of particular relevance; the claimed invention cannot be considered to involve an inventive step when the document is combined with one or more other such documents, such combination being obvious to a person skilled in the art.</p> <p>"&amp;" document member of the same patent family</p> </div> </div>		
Date of the actual completion of the international search  <div style="text-align: center; font-size: large;">20 March 2000</div>		Date of mailing of the international search report  <div style="text-align: center; font-size: large;">28/03/2000</div>
Name and mailing address of the ISA European Patent Office, P.B. 5818 Patentlaan 2 NL - 2280 HV Rijswijk Tel. (+31-70) 340-2040. Tx. 31 651 epo nl Fax: (+31-70) 340-3016		Authorized officer  <div style="text-align: center; font-size: large;">Clarkson, P</div>

# INTERNATIONAL SEARCH REPORT

International Application No  
PCT/US 99/26751

C.(Continuation) DOCUMENTS CONSIDERED TO BE RELEVANT		
Category *	Citation of document, with indication, where appropriate, of the relevant passages	Relevant to claim No.
X	EP 0 252 892 A (HAESSLE AB) 13 January 1988 (1988-01-13)  column 1, line 32 -column 2, line 13; figures ----	1,2,5,7, 8,12,15, 19,20
X	US 5 531 683 A (THOMPSON THOMAS N ET AL) 2 July 1996 (1996-07-02)  column 13, line 47 -column 16, line 29; figures 18-24 ----	1,4-9, 12,15, 18-29,32
X	US 4 915 688 A (BISCHOF DECEASED REINHARD ET AL) 10 April 1990 (1990-04-10) the whole document ----	1,2,7,8
A	WO 97 10012 A (ELAN MED TECH ;GROSS JOSEPH (IE)) 20 March 1997 (1997-03-20) the whole document ----	1-34
A	US 4 850 978 A (DUDAR THOMAS E ET AL) 25 July 1989 (1989-07-25) the whole document ----	1-34
A	US 5 707 365 A (SMEDLEY WILLIAM H ET AL) 13 January 1998 (1998-01-13) the whole document ----	1-34
A	US 5 147 323 A (SMEDLEY WILLIAM H ET AL) 15 September 1992 (1992-09-15) the whole document -----	1-34

# INTERNATIONAL SEARCH REPORT

International application No.

PCT/US 99/ 26751

## Box I Observations where certain claims were found unsearchable (Continuation of Item 1 of first sheet)

This International Search Report has not been established in respect of certain claims under Article 17(2)(a) for the following reasons:

1. ☐ Claims Nos.:  
because they relate to subject matter not required to be searched by this Authority, namely:
2. ☒ Claims Nos.: 35-134  
because they relate to parts of the International Application that do not comply with the prescribed requirements to such an extent that no meaningful International Search can be carried out, specifically:  
see FURTHER INFORMATION sheet PCT/ISA/210
3. ☐ Claims Nos.:  
because they are dependent claims and are not drafted in accordance with the second and third sentences of Rule 6.4(a).

## Box II Observations where unity of invention is lacking (Continuation of Item 2 of first sheet)

This International Searching Authority found multiple inventions in this international application, as follows:

1. ☐ As all required additional search fees were timely paid by the applicant, this International Search Report covers all searchable claims.
2. ☐ As all searchable claims could be searched without effort justifying an additional fee, this Authority did not invite payment of any additional fee.
3. ☐ As only some of the required additional search fees were timely paid by the applicant, this International Search Report covers only those claims for which fees were paid, specifically claims Nos.:
4. ☐ No required additional search fees were timely paid by the applicant. Consequently, this International Search Report is restricted to the invention first mentioned in the claims; it is covered by claims Nos.:

Remark on Protest

- ☐ The additional search fees were accompanied by the applicant's protest.
- ☐ No protest accompanied the payment of additional search fees.

**FURTHER INFORMATION CONTINUED FROM PCT/ISA/ 210**

**Continuation of Box 1.2**

**Claims Nos.: 25-134**

In a view of the large number and also the wording of the claims presently on file, which render it difficult, if not impossible, to determine the matter for which protection is sought, the present application fails to comply with the clarity and conciseness requirements of Article 6 PCT (see also Rule 6.1(a)PCT) to such an extent that the meaningful search is impossible. Consequently, the search report has been drawn up for those parts of the application which do appear to be clear (and concise), namely claims 1 to 34.

The applicant's attention is drawn to the fact that claims, or parts of claims relating to inventions in respect of which no international search report has been established need not be the subject of an international preliminary examination (Rule 66.1(e) PCT). The applicant is advised that the EPO policy when acting as an International Preliminary Examination Authority is normally not to carry out a preliminary examination on matter which has not been searched. This is the case irrespective of whether or not the claims are amended following receipt of the search report or during Chapter II procedure.

FURTHER INFORMATION CONTINUED FROM PCT/ISA/ 210

Continuation of Box I.2

Claims Nos.: 35-134

In view of the large number and also the wording of the claims presently on file, which render it difficult, if not impossible, to determine the matter for which protection is sought, the present application fails to comply with the clarity and conciseness requirements of Article 6 PCT (see also Rule 6.1(a) PCT) to such an extent that a meaningful search is impossible. Consequently, the search report has been drawn up for those parts of the application which do appear to be clear (and concise), namely claims 1 to 34.

The applicant's attention is drawn to the fact that claims, or parts of claims, relating to inventions in respect of which no international search report has been established need not be the subject of an international preliminary examination (Rule 66.1(e) PCT). The applicant is advised that the EPO policy when acting as an International Preliminary Examining Authority is normally not to carry out a preliminary examination on matter which has not been searched. This is the case irrespective of whether or not the claims are amended following receipt of the search report or during any Chapter II procedure.

# INTERNATIONAL SEARCH REPORT

Information on patent family members

International Application No

PCT/US 99/26751

Patent document cited in search report	Publication date	Patent family member(s)	Publication date
US 4755169 A	05-07-1988	US 4689042 A AT 91634 T AU 579301 B AU 6140886 A CA 1263576 A DD 245817 A DE 3688736 A DE 3688736 T EP 0229820 A ES 555096 D ES 8707865 A GR 861290 A IL 78813 A IL 97942 A JP 62502876 T KR 9406107 B NZ 216166 A PT 82618 A,B WO 8606967 A	25-08-1987 15-08-1993 17-11-1988 24-12-1986 05-12-1989 20-05-1987 26-08-1993 28-10-1993 29-07-1987 01-09-1987 16-11-1987 16-09-1986 04-04-1993 21-02-1993 19-11-1987 06-07-1994 29-08-1989 28-11-1986 04-12-1986
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# INTERNATIONAL SEARCH REPORT

Information on patent family members

International Application No

PCT/US 99/26751

Patent document cited in search report	Publication date	Patent family member(s)	Publication date
US 5531683 A		AU 6770694 A WO 9528201 A	10-11-1995 26-10-1995
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